

Flux Ratios and Channel Structures

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Dedicated to the memory of Professor George R. Sell

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Abstract We investigate Ussing's unidirectional fluxes and flux ratios of charged tracers motivated particularly by the insightful proposal of Hodgkin and Keynes on a relation between flux ratios and channel structure. Our study is based on analysis of quasi-one-dimensional Poisson-Nernst-Planck type models for ionic flows through membrane channels. This class of models includes the Poisson equation that determines the electrical potential from the charges present and is in that sense consistent. Ussing's flux ratios generally depend on all physical parameters involved in ionic flows, particularly, on bulk conditions and channel structures. Certain setups of ion channel experiments result in flux ratios that are universal in the sense that their values depend on bulk conditions but not on channel structures; other setups lead to flux ratios that are specific in the sense that their values depend on channel structures too. Universal flux ratios could serve some purposes better than specific flux ratios in some circumstances and worse in other circumstances. We focus on two treatments of tracer flux measurements that serve as estimators of important properties of ion channels. The first estimator determines the flux of the main ion species from measurements of the flux of its tracer. Our analysis suggests a better experimental design so that the flux ratio of the tracer flux and the main ion flux is universal. The second treatment of tracer fluxes concerns ratios of fluxes and experimental setups that try to determine some properties of channel structure. We analyze the two widely used experimental designs of estimating flux ratios and

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show that the most widely used method depends on the spatial distribution of permanent charge so this flux ratio is specific and thus allows estimation of (some of) the properties of that permanent charge, even with ideal ionic solutions. The work presented in this paper is a first step showing how measurements of fluxes and flux ratios can give important insights into channel structure and function.

Keywords Unidirectional flux · Flux ratio · Channel structures

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1 Introduction

Challenges in study of ion channel functions The atomic structure of the channel protein is important for functions of ion channels (see, e.g., [9, 10, 16–18, 22, 27, 30, 36, 37, 43, 44, 60, 61, 64,71,74,79–81]). The atomic structure determines the class of mechanisms of ion channel functions, in an important but qualitative sense, and provides the basis for describing correlations in continuum models, increasing the resolution and realism of these models in significant ways. The structures being discussed are determined from crystals, with somewhat perturbed locations of atoms and forces (or they would not crystallize), in solutions remote from the physiological solutions in which the channels function, without gradients of electrical or chemical potential essential for channel function, and often at temperatures around 100 K. The disorder of crystals is much less at 100 K than at the biological temperatures (300 K, more or less) where they were evolved to function. Entropic terms important at 300 K are much less visible at 100 K. Changes in entropy with temperature can change the qualitative properties of materials. Semiconductors are insulators at low temperatures when their entropy is small but conductors at higher temperatures where entropy is larger. The structural approach does not deal at all with experimental measurements of current (that are the biological function of most channels). Current versus voltage or concentration curves are not found in papers using the qualitative approach to selectivity. For example, a recent summary [65] in a leading journal includes neither current voltage relations, nor equations. Qualitative study is of great importance but it must not be confused with attempts at quantitative models. It is difficult to compare or improve qualitative models because they do not provide a basis for comparison. Qualitative models omit the specific fits to experimental data that allow one model to be compared to another. Quantitative models are needed to provide such comparisons.

The quantitative treatment of ion channel functions and structures taken in this paper (reviewed in [11–14,19,20,23–26,31,33–35,47,48,53,66,68,69], etc.) differs from the usual classical treatment in several important respects. Most importantly the quantitative approach used here includes structure. Classical treatments omit most structural information including the structure of electrical charge (permanent and polarization) that underlies so much of protein function and is canonized with the classical biochemical classification of amino acid side chains, as acid (negative permanent charge), basic (positive permanent charge), nonpolar (small dielectric coefficient) or polar (large dielectric coefficient). The quantitative approach based on continuum models treats ion channel functions as expressions of the current flow through a channel under a variety of conditions, namely different membrane potentials, different concentrations and compositions of ionic solutions, and different mutations. The quantities from computations/analyses of models can be compared directly with experimental measurements of current. The quantitative models are dramatically reduced in



complexity compared to structures or simulations of structures in atomic detail, but they are precise. Such is the nature of most physical models of condensed phases. It is obviously impossible to include all the interactions of the tremendous number of particles involved. Both qualitative and quantitative approaches are needed and complement each other.

It is convenient to treat ion channels as electric nano-devices with well defined reasonably robust input output relations and easily predicted interactions with their surroundings. The quantitative treatments of ion channel functions are extremely important due to nanoscale, multi-scales, nonlocal interaction, limitations of experimental measurements, measurable characteristic quantities of ionic flows versus characteristics of channel structures.

Importances of a mathematical theory and numerics The challenges in understanding ion channel functions and structures strongly suggest the importance of mathematical analysis and numerical simulations as complementary tools to the physiological theory and experiments. A sound mathematical theory provides direct relations between the outputs and the inputs, at least for the simplified settings used in actual biological experiments. Once tested experimentally, the theory can make predictions and guide numerical designs for simulations and actual experiments.

The enormous literature on channels and transporters from 1947 to say 1990 used measurements of fluxes, fluxes of radioactive isotopes, and their ratios as a main tool. The purpose of this paper is to define such fluxes in precise mathematical language so modern theories can be compared with those thousands of papers. Modern theories compute potentials from distributions of charge and have the advantage of being compatible with the Maxwell description of electrodynamics. Modern measurements are mostly of the structure and fluxes of channels and transporters. We believe measurements of structures, and fluxes, must be combined with electrodynamics to understand how channels and transporters work. We begin this process here by taking one precisely defined class of models (PNP type) and defining and computing the fluxes and flux ratios measured with such effort in so many laboratories for so many years. Transporters and channels have been studied in thousands of papers because they control most biological functions and are directly involved in a wide range of diseases. Our approach will identify the issues involved and pave the way for computations of fluxes and flux ratios in the substantial sequence of models that seek to remove the obvious limitations of classical PNP. It is the purpose of this paper to examine the Poisson-Nernst-Planck theory to see if the consistency of these models is significant. It turns out the consistency of the PNP type models is crucial.

1.1 Important Previous Works on Flux Ratios

The arguably most important quantity for ion channel functions is the *total current*, which is nowadays routinely measured based on an *electric property* of ionic flows. The total current is a combination of *individual fluxes* of all ion species in the steady state where, in particular, displacement current $(\varepsilon_0 \partial E/\partial t)$ where E is the electric field) is zero, and provides crucial information on ion channel properties such as permeation and selectivity. Of course, the fluxes of individual ion species will provide more information. While individual fluxes are (additive) components of the total current, they cannot be decomposed from measurements of the total current using just electrical measurements. The *flux ratio* is needed as well, together with the flux measurements based on radioactive properties.

Ussing's work on flux ratios Ussing, a physiologist, considered fluxes soon after the second world war, when radioactive isotopes of sodium first became available. At that time the role of proteins in membranes was not known so of course his analysis could not include effects



of the structure of proteins let alone their spatial distribution of charge. Indeed, the modern idea of protein structure was then just a dream in the mind of a few young workers mostly at Cambridge (UK and USA). In [78], based on an insightful observation from the Nernst–Planck equation (without using Poisson equation for electric potential explicitly), Ussing introduced and studied the *flux ratio* between the influx $J^{[i]}$ (the inward unidirectional flux from outside x = 0 to inside x = 1 of a channel measured at x = 1) and the efflux $J^{[o]}$ (the outward unidirectional flux measured at x = 0) of the same ion species. Note that the channel length is normalized to 1 (see (5.2) for a normalization). Ussing's formula (equation (8) in [78]) is recast below

$$\frac{J^{[i]}}{J^{[o]}} = \frac{f(0)}{f(1)} \cdot \frac{c(0)}{c(1)} e^{\frac{e_0}{k_B T} z V_0} = \frac{c(0)}{c(1)} e^{\frac{e_0}{k_B T} z V_0 + \frac{1}{k_B T} \mu^{e_X}(0) - \frac{1}{k_B T} \mu^{e_X}(1)}},$$
(1.1)

where the quantity e_0 is the (positive) elementary charge, k_B is the Boltzmann constant and T is the absolute temperature, z is the valence (number of charges per ion) of the ion species, c(0) and c(1) are the concentrations of the ion species at left boundary x=0 and the right boundary x=1, respectively, $\mu^{ex}(0)$ and $\mu^{ex}(1)$ are the respective excess components (so $f(0)=e^{\frac{1}{k_BT}\mu^{ex}(0)}$ and $f(1)=e^{\frac{1}{k_BT}\mu^{ex}(1)}$ are the respective activity coefficients), V_0 is the transmembrane electic potential—the difference between the electric potential at x=0 and that at x=1.

An apparent advantage of flux ratios over individual fluxes is that its dependence on physical parameters involved in ionic flow is much simpler. As far as we know, physical scientists had not anticipated the importance and subtleness of the ratio of unidirectional fluxes despite the large physical literature on Nernst–Planck equations. Physiologists seem to have been the first to recognize the physical importance of flux ratios. This essentially abstract, physical and mathematical estimator was used universally to distinguish transporters from channels in thousands of experimental papers from 1949 to 1990 or so. The estimator proved to be quite robust in classical models that assumed electric potentials independent of the distribution of charge [5,6,62,63].

Note that formula (1.1) provides a direct relation between the flux ratio with the data at two points x=0 and x=1. On the other hand, the activity coefficients f(0) and f(1) (or equivalently, the excess components $\mu^{ex}(0)$ and $\mu^{ex}(1)$) cannot be determined by the data $(V_0, c(0), c(1))$ alone. Multicomponent systems like ionic solutions are complex fluids in which 'everything depends on everything else', as shown directly in the thousands of experimental measurements of activity coefficients in different solutions. The electrical potential is a global quantity depending on (for example) boundary conditions far away. The concentrations (more generally the chemical potentials) can depend on the shape of the structure confining them and on the electrical potential as well as on the interactions with ions of different type and variable concentration.

Teorell [76], and Hodgkin and Huxley [40] used the 'independence principle' that states, with a constant potential difference across the membrane, the chance of any individual ion crossing the membrane in a given time interval is not affected by the other ions that are present, to derive the flux ratio formula below

$$\frac{J^{[i]}}{J^{[o]}} = \frac{c(0)}{c(1)} e^{z\zeta_0 V_0},\tag{1.2}$$

where $\zeta_0 = \frac{e_0}{k_B T}$. The independence principle is useful, we now know, for highly selective channels that function independently in membranes (like the sodium and potassium channels studied by Hodgkin and Huxley). The independence principle does not apply to less selective



channels (of which there are many, including the acetylcholine activated channel studied extensively by Katz, a collaborator of Hodgkin and Huxley) or to crowded bulk solutions. ¹

Formula (1.2) is simpler than (1.1). In particular, the right-hand side of formula (1.2) involves only the data (V_0 , c(0), c(1)) at the boundary points. But formula (1.2) requires the independence hypothesis, and hence, could only be used to compare with experimental measurements of flux ratios as a TEST for independence hypotheses.

Work of Hodgkin and Keynes In [45], Hodgkin and Keynes pointed out that "Examples of mechanisms to which such an independence relation should apply are those involving combination with carries where only a small proportion of the carrier is combined, or systems involving diffusion where the ions are present at fairly low concentrations throughout the membrane, and have no tendency to concentrate in narrow channels." In comparing their experimentally measured flux ratio from potassium channels with that from formula (1.2) for a broad range of experimental designs, they found the deviation between these two flux ratios could be significant and concluded that independence hypotheses do not hold for ion channels in general. It is a fascinating fact that flux ratios for sodium channels (which were of great interest to Hodgkin and coworkers) have very different properties from potassium channels and do NOT show the interactions so characteristic of potassium channels. In fact sodium channels follow the independence principle [7,72] nearly exactly, while potassium channels do not. Perhaps sodium channels function at very low occupancy and so only one ion is in the channel at a time and that ion cannot interact with neighbors even though the channel is narrow [7,15,72].

In the same paper [45], based on a fitting function to the experimental data, Hodgkin and Keynes introduced the *flux ratio exponent n'* through the relation

$$\frac{J^{[i]}}{J^{[o]}} = \left(\frac{c(0)}{c(1)}e^{z\zeta_0 V_0}\right)^{n'}.$$
 (1.3)

They argued that the flux ratio exponent n' estimates the average number of sites occupied by ions in the membrane. There is an enormous biological, physical, chemical and mathematical literature building on the original work of Hodgkin and Keynes on single file diffusion because nearly one dimensional systems are found in ion channels, zeolites, and throughout the physical and biological world (see, e.g., [8,52] and references therein). Hille summarizes the biological situation in Table 15.1 in [36].

In practice, one could determine the flux ratio exponent n' easily: by computing the value $\frac{c(0)}{c(1)}e^{z\xi_0V_0}$ from experimental designs of boundary conditions and experimentally measuring the flux ratio $J^{[i]}/J^{[o]}$, and then using the relation (1.3). This procedure of determining the flux ratio exponent n' has been used in thousands of experimental papers.

The treatment of Hodgkin and Keynes, and its users following Hille [36] more than anyone else, involved electric fields that did not depend on the charge of the protein. Proteins are highly charged and the structure of their charges is an important determinant of their function: the location of acid and base groups and polar and nonpolar amino acids is a structural feature of the greatest importance. Charge changes electric fields in all models of electrodynamics (e.g., Maxwell equations) so the question arises whether the Hodgkin–Keynes–Hille interpretation of the flux ratio exponent is correct. The interpretation of n'

¹ The independence principle played a large part in the early thinking of Hodgkin, Huxley, and Katz [38−44] and was widely used by physiologists and biochemists to describe bulk solutions perhaps for that reason. Hodgkin was unaware of the evidence (personal communications ALH to RSE) that the Kohlraush principle of independent migration (∼1880) had been disproven by measurements showing that properties of dilute sodium chloride solutions depended on the square root of concentration (because of the screening of the ionic atmosphere approximated by Debye-Hückel theory).



by Hodgkin and Keynes [45] was a startling insight and was widely thought to be a general property of channels resulting from their narrow structure (see Hille [36]) even though sodium channels in fact turn out to have independent fluxes similar to those in bulk solutions. The question is how much can we rely on the conclusions of this experimental work interpreted by using a theory assuming an electric field independent of protein structure and charge?

To understand the flux ratio of Hodgkin-Keynes-Hille, we need a theory that includes the channel structure, mainly its permanent charges. Analysis could determine how the crucial property of the flux ratio varies with conditions. The simplest treatment of channels in which the electric field is computed from charge is probably the classical Poisson-Nernst-Planck theory (see, e.g., [1-4,28,29,55,56,59,70]). The classical PNP is just a beginning since it ignores correlations produced by the crowding of ions of finite size, although it does include long range correlations produced by charge through the Poisson equation. We study flux ratios of the PNP type that also includes ion-to-ion correlations due to ion sizes, trying to present a formulation that can easily accommodate generalizations that include more correlations. Universal flux ratios and specific flux ratios It seems that formula (1.1) suggests that flux ratios depend on bulk conditions only. It is not the case in general. First of all, Ussing's design that leads to his formula (1.1) is special in the sense that the two unidirectional fluxes are produced in one experiment (essentially the same setup as in the two-isotope-setup discussed in Sect. 4.2). Still, in this case, the excess potentials $\mu^{ex}(0)$ and $\mu^{ex}(1)$ at x=0 and x=1are involved in the formula. The excess potentials $\mu^{ex}(0)$ and $\mu^{ex}(1)$ generally also depend on the channel structure except when we use *local* models (see Hypothesis 2.2) for excess potentials. Other experiment designs will lead to flux ratios that depend on channel structures even when local models are used for excess potentials, in fact, even if the classical PNP model is used where the excess potentials are totally ignored.

It is reasonable and important to classify types of flux ratios due to different experiment designs, relative to the channel structure, into two types: *universal* and *specific*. More precisely, if the flux ratio from a certain experimental design is dependent only on properties of bulk solutions (boundary conditions), particularly, not on the channel structure, the flux ratio is called *universal* (see part (i) and Setup 2 in part (ii) of Sect. 1.2 for examples of universal flux ratios); if the flux ratio depends on the channel structure too, then it is *specific* (see Setup 1 in part (ii) of Sect. 1.2 for an example of specific flux ratios).

We emphasize that it is the detail of an experimental design that dictates the type of flux ratios. For the same channel, some experimental designs could lead to *universal* flux ratios (see Corollary 3.2 and particularly Remark 3.3); some experimental designs could lead to *specific* flux ratios (see Corollary 4.2).

We point out that this classification is rough but helpful. The flux ratio in formula (1.1) is, strictly speaking, specific. But, for reasonably dilute bulk solutions, local model for excess potentials are good enough so the flux ratio is nearly universal. Also, the terminology could be misunderstood to mean that the universal flux ratios are useless. Indeed, universal flux ratios are not directly useful for detecting channel structures. But universal flux ratios are helpful in understanding other channel properties (see the discussion of treatment (i) of flux ratios in Sect. 1.2).

1.2 Experiments on Flux Ratios and Poisson–Nernst–Planck Theory

Motivated by the works of Ussing, and of Hodgkin and Keynes, flux ratios have been used in many studies of various properties of ion channels. Two major applications will be briefly described below and will be carefully analyzed based on PNP type models in the main part of this paper.



(i) Flux ratios of a main ion species and its tracer One application of flux ratios is to determine the flux of a main ion species by measuring the flux of its tracer (a radioactive isotope). Roughly speaking, one adds a small amount of a radioactive isotope of the main ion species and measures the flux of the isotope from its radioactive property, namely the number of disintegrations per unit time (detected by the radiation products of the disintegration such as gamma rays), and then estimates the flux of the main ion species by determining the flux ratio—proportionality constant—between the flux of the tracer and that of the main ion species. In view of Ussing's work, the proportionality constant can be well approximated and easily determined from the boundary conditions alone (see Corollary 3.2).

An ideal experimental design for this purpose uses a *universal* flux ratio so that the proportionality constant can be *precisely* and *easily* determined, independent of the often unknown channel structure. Based on analysis of PNP type models, we discover an experimental design (proposed in Remark 3.3) so that, *if the design can be practically implemented*, the resulting flux ratio is indeed universal.

(ii) Flux ratios versus channel structures Another setup for flux ratios is motivated by the work of Hodgkin and Keynes [45] discussed above. These setups are designed so the estimated flux ratios are NOT universal. Rather these flux ratios suppose to depend on the characteristics of the channel, which would allow one to extract information on channel structure—permanent charge, in principle. We consider two different experimental setups (see Sect. 4) that produce estimates of flux ratios. One setup, the one-isotope-setup (Setup 1), uses one isotope in two experiments, and the other, the two-isotope-setup (Setup 2), uses two isotopes in the same experiment (essentially the same setup Ussing used in deriving formula (1.1)). With the specific setups described in Sect. 4, it will be clear that the two flux ratios from the two setups are nearly, but not quite equal (numerically).

Analysis of PNP type models indicates that the issue of experimental setups in this application of flux ratios is subtle. In Sect. 4, we analyze the flux ratios from the two different setups based on PNP type models with *local* excess potential models. Our analysis shows that the two different setups make a significant qualitative difference—the flux ratio from the one-isotope-setup (Setup 1) is specific so the flux ratio depends on the permanent charge, even with ideal ionic solutions; the flux ratio from the two-isotope-setup (Setup 2), for PNP type with local excess potential models, is universal, totally independent of the permanent charge.

The ultimately important issue is the relation between the flux ratio and the channel structure. As mentioned above, for the two-isotope-setup (Setup 2), the PNP model with local excess potential does not provide any relation between the flux ratio and the channel structure. But, for the one-isotope-setup (Setup 1), PNP with local excess potentials, even PNP with only ideal electrochemical potentials, does provide such a relation although not in an explicit form yet. To further examine the relevance of the flux ratio from the one-isotope-setup (Setup 1) to channel structures, we consider the case where the permanent charge is small relative to the characteristic concentration and a local hardsphere is included in the electrochemical potential. An approximation formula of the flux ratio is obtained with the leading terms explicitly expressed in terms of boundary conditions and the assumed channel structure. This formula allows one to analyze the relation between the flux ratio and the permanent charge in this simple case. We emphasize that our work in this paper is only the starting point of our investigation so the results are far from a complete theory on relationship between the flux ratio and the channel structure. Indeed, one of the reasons for this paper is to pose this important biological language in precise mathematical form so more complete theories can be developed and applied.



A comment on the sign of unidirectional flux In formulas (1.1), (1.2) and (1.3), $J^{[i]}$ and $J^{[o]}$ are both defined as positive quantities, although they flow in opposite directions. In the following, we will fix one spatial orientation in our formulas for all fluxes. Thus $J^{[i]}$ is positive and $J^{[o]}$ is negative. This produces a minus sign in our formulas for flux ratio $J^{[i]}/J^{[o]}$.

Organization of the paper In Sect. 2, a quasi-one-dimensional PNP type model for ionic flow is reviewed and our assumption on the excess potentials is introduced.

In Sect. 3, a formula (3.1) for individual fluxes is provided. We then examine the proportionality between the flux of the main ion species and the unidirectional flux of a tracer. A formula (3.7) for the *proportionality constant* is derived and, based on the formula, we propose an extremely useful experimental design in Remark 3.3 from which this flux ratio is universal—the ideal situation for the purpose of determining the proportionality constant.

In Sect. 4, we discuss two widely used experimental setups for measuring unidirectional fluxes and their flux ratios of unidirectional fluxes, and their differences are discussed. For PNP type models with local excess potentials, the analysis indicates that the flux ratio from the two-isotope-setup (Setup 2) is universal and does not provide any information on channel structures but the flux ratio estimated from the one-isotope setup (Setup 1) is specific and contain information of channel structure.

In Sect. 5, we consider a special case for the one-isotope-setup (Setup 1) to illustrate that the flux ratio is indeed *specific*, in a concrete way. The permanent charge is described in (5.1) and is assumed to be small relative to the characteristic concentration, a local hard-sphere approximation for excess potential is specified in (5.5), and, particularly, the dimensionless quantity ε defined in (5.2) is assumed to be small. We only examine the zeroth order (in ε) term of this specific flux ratio. (For convenience, we refer to this zeroth order (in ε) term of the flux ratio simply as the flux ratio.) Then approximation formulas (5.14) and (5.18) for the flux ratios are derived for the one-isotope-setup (Setup 1) with different boundary electroneutrality conditions. The approximate formulas for the flux ratios are expressed explicitly in terms of boundary conditions and the prescribed permanent charge distribution. Section 6 contains a summary of our results and further discussions on our work.

The derivation of formulas (5.14) and (5.18) for the one-isotope-setup (Setup 1) is provided in "Appendix" (Sect. 7). Section 7.1 gives a reformulation of the flux ratio formula for the special case considered in Sect. 5. Formula (5.14) for electroneutrality boundary conditions among all three ion species is derived in two parts: Sect. 7.2.1 handles the contribution to the flux ratio from (small) permanent charge and Sect. 7.2.2 treats the contribution of ion sizes with a local hard-sphere potential. Formula (5.18) for electroneutrality boundary conditions among only the main ion species and the counter ion species is derived based on the derivation of formula (5.14) with necessary modifications indicated.

2 PNP Type Models and Electrochemical Potentials

2.1 The Boundary Value Problem

The following quasi-one-dimensional PNP type model was suggested by Nonner and Eisenberg [67] (see [57] for a justification from the three-dimensional PNP for a special case):

$$\frac{1}{h(x)} \frac{d}{dx} \left(\varepsilon_r(x) \varepsilon_0 h(x) \frac{d}{dx} \phi \right) = -e_0 \left(\sum_{s=1}^n z_s c_s + Q(x) \right),$$

$$\frac{d}{dx} J_k = 0, \quad -J_k = \frac{1}{k_B T} D_k(x) h(x) c_k \frac{d}{dx} \mu_k, \quad k = 1, 2, \dots, n$$
(2.1)



where ϕ is the electric potential, k_B is the Boltzmann constant, T is the absolute temperature, e_0 is the elementary charge, $\varepsilon_r(x)$ is the relative dielectric coefficient, ε_0 is the dielectric constant of vacuum; h(x) is the cross-section area over the longitude coordinate x of the channel, Q(x) is the permanent charge; for the kth ion species, c_k is the concentration, z_k is the valence, J_k is the flux density across each cross-section of the channel, $D_k(x)$ is the diffusion coefficient, μ_k is the electrochemical potential (that depends on ϕ and $\{c_j\}$ in general).

The boundary conditions are, for k = 1, 2, ..., n,

$$\phi(0) = V_0, \quad c_k(0) = L_k; \quad \phi(1) = 0, \quad c_k(1) = R_k.$$
 (2.2)

The concentrations of ions manipulated in experiments are represented by the set of boundary values of concentrations L_k 's on the left side and R_k 's on the right side. We remark that the channel has been normalized from x = 0 to x = 1 by a scaling of its longitude variable (see (5.2) for the full dimensionless rescaling).

2.2 Electrochemical Potential

The electrochemical potential $\mu_k = \mu_k^{id} + \mu_k^{ex}$, consisting of the ideal component μ_k^{id} and the excess component μ_k^{ex} , is the most important variable in a model of ions in solutions or channels. The ideal component

$$\mu_k^{id} = k_B T \ln \frac{c_k}{c_0} + z_k e_0 \phi, \tag{2.3}$$

where c_0 is a characteristic concentration, reflects the contribution of ions as point-charges. For nearly infinite dilute ion solutions, the ideal component μ_k^{id} is a good approximation of the electrochemical potential μ_k .

The excess component μ_k^{ex} measures the deviation of the electrochemical potential from the ideal component, in particular, it accounts for ion size effects and presumably channel size in turn. This description of nonideal properties uses the excess component μ_k^{ex} as an additive component to the ideal component. Another equivalent description of nonideal properties is in terms of activity coefficient (discussed below) as multiplication factor to the one associated with the ideal component. The nonideal property of kth ion species depends, in principle, on everything involved such as the temperature, the medium (water), ion-ion interactions due to ion sizes, the concentrations of all ion species of the mixture, etc. Models of μ_k^{ex} are not fully understood and developed. There are various explicit approximations of μ_k^{ex} that are particularly important in models of ionic solutions in and around biological cells. These are all derived from seawater, and so are quite concentrated mixtures (\approx 0.2 M) and so have substantial and important excess components. Indeed, animal cells depend on the difference between potassium and sodium: without that difference they cannot survive, and potassium and sodium ions differ only because of their excess properties due to their different sizes.

The *activity* a_k is another standard characteristic of the electrochemical potential of kth ion species and describes nonideal properties through its *activity coefficient* f_k as a multiplicative factor to the one associated with the ideal component (up to a reference potential). The activity a_k is dimensionless and is defined by

$$a_k = e^{\frac{1}{k_B T}(\mu_k - \mu_k^0)} = e^{\frac{1}{k_B T}\mu_k^{ex}} e^{\frac{1}{k_B T}(\mu_k^{id} - \mu_k^0)}, \tag{2.4}$$



where, in general, μ_k^0 can be any reference potential and, in this sense, the activity a_k is a relative term. The *activity coefficient* f_k is the pre-factor in the last expression in (2.4)

$$f_k = e^{\frac{1}{k_B T} \mu_k^{ex}}. (2.5)$$

Note that $f_k=1$ for ideal ionic solutions. The deviation of f_k from 1 measures the nonideal nature of the ionic solution. The relation (2.5) is used to get the second expression of the flux ratio in (1.1). For a solute in solution, a standard convention is to take $\mu_k^0=\mu_k^{id}$. In this case, one has $a_k=f_k$. If we take $\mu_k^0=z_ke_0\phi$ (only the electric component of μ_k^{id}) and the characteristic concentration $c_0=\sum_j c_j$, then

$$a_k = f_k \frac{c_k}{c_0} = f_k x_k,$$

where x_k is the concentration fraction of kth ion species, is another form of activity. If we take $\mu_k^0 = 0$, then (2.4) can be rewritten as

$$a_k = f_k e^{\frac{1}{k_B T} \mu_k^{id}}$$
 or $\ln a_k = \ln f_k + \ln \frac{c_k}{c_0} + z_k \zeta_0 \phi$.

The latter is the equation (3) with $c_0 = 1$ in [78] used by Ussing to define the (electrochemical) activity a_k that includes the electrical potential ϕ as a part.

In the following, we will use the excess components μ_k^{ex} 's to characterize the nonideal nature of ionic solutions.

For all results in Sects. 3 and 4, we will make two assumptions about the electrochemical potentials adopted in the PNP type model (2.1).

Hypothesis 2.1 For a given fixed ionic mixture, if jth ion species and kth ion species have the same valence and diameter, then the excess potentials and diffusion coefficients for jth ion species and for kth ion species are the same; that is, if $z_j = z_k$ and $d_j = d_k$, then $\mu_j^{ex}(x) = \mu_k^{ex}(x)$ and $D_j(x) = D_k(x)$.

The validity of Hypothesis 2.1 in great generality was explicitly pointed out by Ussing in the last paragraph on page 45 of [78]. In our work, Hypothesis 2.1 will be applied to a main ion species and its isotopic tracer that have the same valence and diameter.

For a solution $(\phi(x), C(x), J)$ of the boundary value problem (BVP) (2.1) and (2.2), we will thus use the following notation for $\mu_k^{ex}(x)$ to indicate explicitly its dependence on (z_k, d_k) :

$$\mu_k^{ex}(x) = \mu_k^{ex}(x; z_k, d_k).$$
 (2.6)

Hypothesis 2.2 The excess potentials are taken to be *local* in the sense that, for kth ion species, its excess potential $\mu_k^{ex}(x; z_k, d_k)$ at location x depends pointwise on concentrations $C(x) = \{c_j(x) : j = 1, \ldots, n\}$ of all ion species of the ionic mixture but only at the location x; that is, $\mu_k^{ex}(x; z_k, d_k) = \mu_k^{ex}(C(x); z_k, d_k)$.

For a nonlocal model of the excess potential μ_k^{ex} , its value $\mu_k^{ex}(x)$ at x is often taken to be dependent on the values of C(y) for y in a neighborhood of x where the size of the neighborhood is typically about the maximum of $(d_j + d_k)/2$ for $j = 1, 2, \ldots, n$ and the Debye screening length at x.

The local nature of excess potentials assumed in Hypothesis 2.2 is an approximation and is often good enough. We will further comment on this hypothesis in Remark 2.3 and at other places that it is crucial.



In the following, we separate the *ideal gas component* from the electrical and nonideal terms to make our formulas more tidy and concise, that is, we introduce

$$p_k(x; z_k, d_k) = z_k \zeta_0 \phi(x) + \frac{1}{k_B T} \mu_k^{ex}(x; z_k, d_k), \tag{2.7}$$

where $\zeta_0 = e_0/k_BT$. Therefore, for kth ion species, $k_BTp_k(x; z_k, d_k)$ is the component beyond the ideal gas (non-charged) component $k_BT\ln(c_k(x)/c_0)$, that is, the total electrochemical potential $\mu_k(x)$ is

$$\mu_k(x) = k_B T \ln \frac{c_k(x)}{c_0} + k_B T p_k(x; z_k, d_k).$$

We also purposely include z_k and d_k in the expression $p_k(x; z_k, d_k)$ to remind the readers of Hypothesis 2.1; that is, for *j*th ion species and *k*th ion species, if $z_j = z_k$ and $d_j = d_k$, then $p_k(x; z_k, d_k) = p_j(x; z_j, d_j)$.

Remark 2.3 We claim that, for all the results in Sects. 3 and 4, the local assumption (2.2) on the excess potentials $\mu_k^{ex}(x; z_k, d_k)$'s can be relaxed under one general condition; that is, one needs $\mu_k^{ex}(x; z_k, d_k)$ to be *local* only outside the channel (near x=0 and x=1), in particular, nonlocal models for the excess potentials are allowed inside the channel, provided the corresponding BVP (2.1) and (2.2) is well-posed. This claim follows from the proofs of all the results in Sects. 3 and 4 without any change. On the other hand, when nonlocal models for excess potentials are used at inside and outside (particularly near x=0 and x=1) of the channel, the corresponding BVP (2.1) and (2.2) is known to be severely under determined, and it is not completely understood how to formulate "correct" boundary conditions for the BVP to be well-posed. In [75], an initial attempt for a correct formulation of boundary conditions that are natural to the biological setups is taken. Further studies would be necessary for a better understanding of the roles of nonlocal nature of the excess potentials.

3 Unidirectional Flux and Proportionality Constant

For the results in this section and in Sect. 4, we only assume that the BVP specified in Eq. (2.1) and the boundary condition (2.2) has a solution. It is not assumed that the solution of the BVP (2.1) and (2.2) is unique (of course, the results are referred to a given solution of the BVP (2.1) and (2.2)). We also do not assume electroneutrality boundary conditions so there might be boundary layers. Experimental designs often use "four electrode" arrangements to remedy possible boundary layers. In those arrangements, two 'working' electrodes (that carry current) are inserted far away from the channel so boundary conditions that may produce boundary layers do not reach the ends of the channel. Two other electrodes are inserted near the ends of channel and away from possible boundary layers and used to measure electric potential and concentrations.

3.1 An Important Formula for J_k and Unidirectional Flux

Proposition 3.1 below has been derived in classical channel models for ideal solutions where $p_k(x; z_k, d_k) = z_k \zeta_0 \phi(x)$ (see, e.g., [49]).

Proposition 3.1 Assume Hypotheses 2.1 and 2.2. If (ϕ, C, J) is a solution of the BVP (2.1) and (2.2), then

$$J_k = \left(L_k e^{p_k(0;z_k,d_k)} - R_k e^{p_k(1;z_k,d_k)}\right) \left(\int_0^1 \frac{e^{p_k(x;z_k,d_k)}}{D_k(x)h(x)} dx\right)^{-1},\tag{3.1}$$

where $p_k(x; z_k, d_k)$ is defined in (2.7).

In particular, if, at the boundaries (outside the channel), we do not include the excess component, this is, if we take $\mu_k(0) = \mu_k^{id}(0)$ and $\mu_k(1) = \mu_k^{id}(1)$, then

$$J_k = \left(L_k e^{z_k \zeta_0 V_0} - R_k\right) \left(\int_0^1 \frac{e^{p_k(x; z_k, d_k)}}{D_k(x) h(x)} dx\right)^{-1}.$$
 (3.2)

Proof It follows from Nernst–Planck equations in (2.1) that

$$-J_k = D_k(x)h(x)e^{-p_k(x;z_k,d_k)} \left(c_k e^{p_k(x;z_k,d_k)}\right)'.$$
(3.3)

Divide the three factors on the right-hand side of (3.3) and integrate to get

$$-J_k \int_0^1 \frac{e^{p_k(x;z_k,d_k)}}{D_k(x)h(x)} dx = \int_0^1 \left(c_k e^{p_k(x;z_k,d_k)} \right)' dx$$
$$= c_k(1)e^{p_k(1;z_k,d_k)} - c_k(0)e^{p_k(0;z_k,d_k)}.$$

The formula (3.1) for J_k then follows from the boundary conditions (2.2).

When taking $\mu_k(0) = \mu_k^{id}(0)$ and $\mu_k(1) = \mu_k^{id}(1)$, one has $p_k(0; z_k, d_k) = z_k \zeta_0 V_0$ and $p_k(1; z_k, d_k) = 0$. Formula (3.2) then follows from formula (3.1).

Formula (3.3) is the same as Ussing's formula (5) in [78], from which Ussing derived his formula (1.1). The extra step leading to formula (3.1) proves to be useful at several occasions, for example, for obtaining formulas (3.7) and (4.3) below which are not direct consequences of Ussing's formula (1.1).

Formula (3.1) for J_k has the advantage that the only unknown quantity on the right-hand side is the function $p_k(x; z_k, d_k)$ which, from Hypothesis 2.1, is the SAME for ion species with the SAME (z_k, d_k) such as for an ion species and its isotopes.

We end this part by illustrating an immediate use of formula (3.1): a definition of *unidirectional fluxes*. This has been demonstrated for ideal ionic solutions in [49].

Formula (3.1) can be rewritten as follows to give a decomposition of J_k as the sum of two unidirectional fluxes $J_k = J_k^{[i]} + J_k^{[o]}$ where

$$J_{k}^{[i]} = L_{k}e^{p_{k}(0;z_{k},d_{k})} \left(\int_{0}^{1} \frac{e^{p_{k}(x;z_{k},d_{k})}}{D_{k}(x)h(x)} dx \right)^{-1},$$

$$J_{k}^{[o]} = -R_{k}e^{p_{k}(1;z_{k},d_{k})} \left(\int_{0}^{1} \frac{e^{p_{k}(x;z_{k},d_{k})}}{D_{k}(x)h(x)} dx \right)^{-1}$$
(3.4)

are the so-called *influx* and *efflux* of kth ion species, respectively. (Note the minus sign in $J_k^{[o]}$ is due to the fact that we use the same spatial orientation of positive current for both fluxes.)

Formulas in (3.4) provide a mathematically meaningful definition of influx and efflux. It should be stressed that the unidirectional influx $J_k^{[i]}$ (respectively, efflux $J_k^{[o]}$) depends also on all other quantities in the boundary conditions as well as the permanent charge of the problem through the global profile of $p_k(x; z_k, d_k)$. The ratio between these two unidirectional fluxes

$$\frac{J_k^{[i]}}{J_k^{[o]}} = -\frac{L_k e^{p_k(0; z_k, d_k)}}{R_k e^{p_k(1; z_k, d_k)}}$$

agrees with Ussing's formula (1.1). When local excess potentials are used, the above ratio is independent of channel structures, and hence, the flux ratio is 'approximately' universal. This formula, under the hypothesis that, near x = 0 and x = 1, ionic solutions are dilute



enough, would reduce to formula (1.2); in particular, the flux ratio is *universal*, independent of channel structures

3.2 Proportionality Between Flux of Main Ions and that of Its Tracer

While most experiments today measure the total current, it is important to measure the fluxes of individual ions—the components of the current—and such flux measurements were the basis of hundreds if not thousands of classical papers and almost all work on vesicle preparations widely used by molecular biologists. (The references [36,37,77] are good entry points to the classical literature.) For example, for Na+Cl- solutions, one can add a tiny amount of a radioactive isotope of sodium denoted by T_{Na} . The flux of T_{Na} can be measured by its radioactivity. The isotope T_{Na} has exactly the same electrical and chemical properties as the main ion species (the NON-radioactive Na) so one expects their fluxes are proportional to each other in a simple manner. Determining the proportionality constant would provide a measurement of the flux of the main ion species by measuring the tracer flux of radioactive T_{Na} . A general analysis of the proportionality constant or 'specific activity' (the favorite name of experimentalists) is not possible, of course, because the 'constant' varies with experimental setup. Experimental setups leading to universal flux ratios are preferred.

Since the value of the proportionality constant is different in different setups, we will consider one experimental setup that is widely used in the experimental literature and propose, in Remark 3.3, a specific experimental setup that has a substantial advantage.

For simplicity, we consider three ion species in this subsection: the main ion species (for example, Na^+), its tracer (an isotope of Na^+), and the counter ion (for example, Cl^-). For the relative quantities, we use the following notation. We use the same *subscript* 1 for both the main ion species and its isotope to indicate that they have the same valence, etc., but use different *superscripts* [m] for the main ion species and [t] for the tracer to distinguish them. The symbols for the boundary concentrations are used in the similar way.

	Concentration	Valence	Flux
Main ion species	$c_1^{[m]}$	$z_1 > 0$	$J_1^{[m]}$
Tracer Counter ion	$egin{array}{c} c_1^{[t]} \ c_2 \end{array}$	$z_1 > 0$ $z_2 < 0$	$J_1^{[t]}\\J_2$

For the moment, we do not specify the boundary concentrations of the tracer but will do so afterwards. Thus, the BVP (2.1) and (2.2) for the main ion species, the tracer and the counter ion species becomes

$$\frac{1}{h(x)} \frac{d}{dx} \left(\varepsilon_r(x) \varepsilon_0 h(x) \frac{d}{dx} \phi \right) = -e_0 \left(z_1 \left(c_1^{[m]} + c_1^{[t]} \right) + z_2 c_2 + Q(x) \right),$$

$$\frac{d}{dx} J_1^{[m]} = \frac{d}{dx} J_1^{[t]} = \frac{d}{dx} J_2 = 0,$$

$$-J_1^{[m]} = \frac{1}{k_B T} D_1(x) h(x) c_1^{[m]} \frac{d}{dx} \mu_1^{[m]},$$

$$-J_1^{[t]} = \frac{1}{k_B T} D_1(x) h(x) c_1^{[t]} \frac{d}{dx} \mu_1^{[t]},$$

$$-J_2 = \frac{1}{k_B T} D_2(x) h(x) c_2 \frac{d}{dx} \mu_2$$
(3.5)



with boundary conditions,

$$\phi(0) = V_0, \quad c_1^{[m]}(0) = L_1^{[m]}, \quad c_1^{[t]}(0) = L_1^{[t]}, \quad c_2(0) = L_2;$$

$$\phi(1) = 0, \quad c_1^{[m]}(1) = R_1^{[m]}, \quad c_1^{[t]}(1) = R_1^{[t]}, \quad c_2(1) = R_2.$$
(3.6)

Recall that the main ion species and its tracer have the SAME valence, diameter and diffusion coefficient. The following result is then a direct consequence of Proposition 3.1, not a direct consequence of Ussing's formula (1.1).

Corollary 3.2 Assume Hypotheses 2.1 and 2.2. For BVP (3.5) and (3.6), the proportionality constant between the flux $J_1^{[t]}$ of the tracer and the flux $J_1^{[m]}$ of the main ion species is

$$\frac{J_1^{[t]}}{J_1^{[m]}} = \frac{L_1^{[t]} e^{p_1(0;z_1,d_1)} - R_1^{[t]} e^{p_1(1;z_1,d_1)}}{L_1^{[m]} e^{p_1(0;z_1,d_1)} - R_1^{[m]} e^{p_1(1;z_1,d_1)}}.$$
(3.7)

Furthermore, if we take $\mu_1(0) = \mu_1^{id}(0)$ and $\mu_1(1) = \mu_1^{id}(1)$, then

$$\frac{J_1^{[t]}}{J_1^{[m]}} = \frac{L_1^{[t]} e^{z_1 \zeta_0 V_0} - R_1^{[t]}}{L_1^{[m]} e^{z_1 \zeta_0 V_0} - R_1^{[m]}}.$$
(3.8)

Proof Since both the main ion species and the tracer have the same valence z_1 and diameter d_1 , and hence, the function $p_1(x; z_1, d_1)$ in (3.1) is the same for both of them. Also both the main ion species and the tracer have the same diffusion coefficient $D_1(x)$. Formula in Proposition 3.1 yields the formula for the quotient.

Note that, since excess potentials are approximated by local models, the proportionality constant or the flux ratio given by formula (3.7) is approximately universal.

We now apply the results to specific boundary concentrations of tracers widely used in experiments. It is arranged so that the radioactivity on one side of the channel is kept nearly zero (by flowing solution by the channel). If one takes $L_1^{[t]} > 0$ and $R_1^{[t]} = 0$, then (3.7) gives the proportionality constant

$$\frac{J_1^{[t]}}{J_1^{[m]}} = \frac{L_1^{[t]} e^{p_1(0;z_1,d_1)}}{L_1^{[m]} e^{p_1(0;z_1,d_1)} - R_1^{[m]} e^{p_1(1;z_1,d_1)}},$$

where $J_1^{[t]} = J_1^{[t,i]}$ is the inward unidirectional flux (influx) of the tracer. This flux ratio, with any local models for excess potentials in the solution outside the channel, is universal. Given boundary conditions, one still needs to estimate $p_1(0; z_1, d_1)$ and $p_1(1; z_1, d_1)$, which depend on specifics of local models for excess potentials, to determine the proportionality constant. If this experiment involves dilute ionic mixtures, then one can apply formula (3.8) to approximate the proportionality constant

$$\frac{J_1^{[t]}}{J_1^{[m]}} = \frac{L_1^{[t]} e^{z_1 \zeta_0 V_0}}{L_1^{[m]} e^{z_1 \zeta_0 V_0} - R_1^{[m]}}.$$

Finally in the remark below, we make an observation and propose a possible design of experiments for a simple and precise determination of a proportionality constant.

Remark 3.3 One experimental setup provides simple and exact results and so we recommend using it, where practicable. If one designs experiments so that

$$L_1^{[t]}/L_1^{[m]} = R_1^{[t]}/R_1^{[m]} = \sigma,$$
 (3.9)



then it follows from formula (3.7) that

$$\frac{J_1^{[t]}}{J_1^{[m]}} = \sigma \tag{3.10}$$

where $J_1^{[t]} = J_1^{[t,i]} + J_1^{[t,o]}$ is the total flux of the tracer and $J_1^{[m]}$ is the flux of the main ion species. Note that this simple relation is universal and remains true independent of specifics of local models for excess electrochemical components and even if nonlocal models are used as long as the boundary value problem is well-posed.

If one can design this experimentally and measure the total tracer flux $J_1^{[t]} = J_1^{[t,i]} + J_1^{[t,o]}$, then formula (3.10) gives us a beautiful result. It says that if the "specific activity" defined in Eq. (3.9) is the same in the left and right hand solutions, then the radioactive species does in fact trace the movement of nonradioactive species robustly essentially without error. We do not know whether or not this design has been discovered and used for tracer measurements and regretfully we do not know how to find the appropriate reference in the vast literature.

There is a further powerful and beautiful result of this simpler and accurate formula. Consider a setup with two tracers T_1 and T_2 , two isotopes of the main ion species with different radioactivity. One designs the boundary concentrations for tracers as follows:

for tracer
$$T_1$$
: $L_1^{[t_1]} > 0$ at $x = 0$ and $R_1^{[t_1]} = 0$ at $x = 1$; for tracer T_2 : $L_1^{[t_2]} = 0$ at $x = 0$ and $R_1^{[t_2]} > 0$ at $x = 1$.

If
$$L_1^{[t_1]}/L_1^{[m]} = \sigma$$
 and $R_1^{[t_2]}/R_1^{[m]} = \sigma$, then

$$J_1^{[m]} = \frac{1}{\sigma} \left(J_1^{[t_1,i]} + J_1^{[t_2,o]} \right)$$

where $J_1^{[t_1,i]}$ is the influx of tracer T_1 and $J_1^{[t_2,o]}$ is the efflux of tracer T_2 . Under these conditions, the tracer in fact traces the main ion flux exactly.

4 Flux Ratios from Two Setups

In this section, we move to a different but related topic; that is, we examine the flux ratios of two unidirectional fluxes of tracers in two setups corresponding to two different experimental designs for the purpose of detecting channel structures. Two issues are relevant: the first (the focus of this section) is whether or not each flux ratio is universal or specific and is able to provide any information on channel structures, and to compare their differences based on PNP type models with local excess potentials; the second is the detailed relation between the specific flux ratios and the channel structure. The latter will be examined by case studies in Sect. 5.

Since our PNP type models contain local excess potentials, our results apply for non-ideal ionic solutions and, as direct consequences, we also include relevant results for ideal ionic solutions.

4.1 Flux Ratio for the One-Isotope-Setup (Setup 1)

For this setup, one uses one main ion species, one tracer (an isotope of the main ion species), and one counter ion species. Two sets of experiments are performed.



In one experiment, the boundary conditions for the tracer are nonzero concentration $L_1^{[t,i]} > 0$ on left boundary x = 0 and zero concentration $R_1^{[t,i]} = 0$ on the right x = 1. This would produce an influx $J_1^{[t,i]}$ of the tracer.

In the other, the boundary conditions for the tracer are zero concentration $L_1^{[t,o]} = 0$ on left boundary x = 0 and nonzero concentration $R_1^{[t,o]} > 0$ on the right x = 1. This would produce an efflux $J_1^{[t,o]}$ of the tracer.

We will examine the flux ratio $J_1^{[t,i]}/J_1^{[t,o]}$ associated with these two experiments.

According to the two different experiments, two different sets of boundary conditions are as follows.

$$(\text{BVi}): \begin{cases} \phi^{[i]}(0) = V_0, & \phi^{[i]}(1) = 0, \\ c_1^{[m,i]}(0) = L_1^{[m,i]} > 0, \ c_1^{[m,i]}(1) = R_1^{[m,i]} > 0, \ \text{(main ions)} \\ c_1^{[t,i]}(0) = L_1^{[t,i]} > 0, \ c_1^{[t,i]}(1) = R_1^{[t,i]} = 0, \ \text{(tracer)} \\ c_2^{[i]}(0) = L_2^{[i]} > 0, \ c_2^{[i]}(1) = R_2^{[i]} > 0. \ \text{(counterions)} \end{cases}$$

(BVo):
$$\begin{cases} \phi_{2}^{[o]}(0) = L_{2} > 0, & c_{2}^{[o]}(1) = R_{2} > 0. & \text{(counterions)} \\ \phi_{2}^{[o]}(0) = V_{0}, & \phi_{2}^{[o]}(1) = 0, \\ c_{1}^{[m,o]}(0) = L_{1}^{[m,o]} > 0, c_{1}^{[m,o]}(1) = R_{1}^{[m,o]} > 0, & \text{(main ions)} \\ c_{1}^{[t,o]}(0) = L_{1}^{[t,o]} = 0, & c_{1}^{[t,o]}(1) = R_{1}^{[t,o]} > 0, & \text{(tracer)} \\ c_{2}^{[o]}(0) = L_{2}^{[o]} > 0, & c_{2}^{[o]}(1) = R_{2}^{[o]} > 0. & \text{(counterions)} \end{cases}$$

$$(4.2)$$

We will thus consider TWO boundary value problems: one has system (2.1) with the boundary conditions (BVi) in (4.1) and the other has system (2.1) with the boundary conditions (BVo) in (4.2). The key difference between these two boundary conditions concerns the tracer concentration: it is zero at x=1 for (BVi) and it is zero for (BVo) at x=0. For simplicity, the boundary condition for the electric potential ϕ will be kept the same for both BVPs. The boundary concentrations for the main ion species and those for the counter ion species could be different for the two BVPs for the purpose of detailed case studies in Sect. 5.

For the boundary condition (BVi) where $L_1^{[t,i]} > 0$ and $R_1^{[t,i]} = 0$, the absorbing boundary is at the *right* end x = 1 where the tracer concentration is zero and the tracer is inserted from the left end with concentration $L_1^{[t,i]} > 0$ at x = 0; in particular, the flux of the tracer is the influx $J_1^{[t,i]}$. The notation in the next table will be used.

BVi	Concentration	Valence	Flux
Main ion	$c_1^{[m,i]}$	$z_1 > 0$	$J_1^{[m,i]}$
Tracer	$c_1^{[t,i]}$	$z_1 > 0$	$J_1^{[t,i]}$
Counter ion	$c_2^{[i]}$	$z_2 < 0$	$J_2^{[i]}$

Similarly, for the boundary condition (BVo) where $L_1^{[t,o]} = 0$ and $R_1^{[t,o]} > 0$, the flux of the tracer is the efflux $J_1^{[t,o]}$. For this case, we use the notation in next table.

Concerning the flux ratio between $J_1^{[t,i]}$ and $J_1^{[t,o]}$, we have the following formula.

Theorem 4.1 Assume Hypotheses 2.1 and 2.2. For the one-isotope-setup (Setup 1) with one tracer in two experiments, let $J_1^{[t,i]}$ be the influx of the tracer associated with the boundary conditions (BVi) in (4.1) for one experiment; let $J_1^{[t,o]}$ be the efflux of the tracer associated with the boundary conditions (BVo) in (4.2) for the other experiment.



BVo	Concentration	Valence	Flux
Main ion species	$c_1^{[m,o]}$	$z_1 > 0$	$J_1^{[m,o]}$
Tracer	$c_1^{[t,o]}$	$z_1 > 0$	$J_1^{[t,o]}$
Counter ion	$c_2^{[o]}$	$z_2 < 0$	$J_2^{[o]}$

Then the flux ratio between $J_1^{[t,i]}$ and $J_1^{[t,o]}$ is

$$\frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -\frac{L_1^{[t,i]} e^{p_1^{[i]}(0;z_1,d_1)}}{R_1^{[t,o]} e^{p_1^{[o]}(1;z_1,d_1)}} \int_0^1 \frac{e^{p_1^{[o]}(x;z_1,d_1)}}{D_1(x)h(x)} dx \left(\int_0^1 \frac{e^{p_1^{[i]}(x;z_1,d_1)}}{D_1(x)h(x)} dx \right)^{-1}, \tag{4.3}$$

where $p_1^{[i]}(x; z_1, d_1)$ defined in (2.7) is determined by the profiles of concentrations from the solution of BVP associated with the boundary condition (BVi), and $p_1^{[o]}(x; z_1, d_1)$ defined in (2.7) is determined by the profiles of concentrations from the solution of BVP associated with the boundary condition (BVo).

Proof For the experiment associated with the boundary conditions (BVi) where $L_1^{[t,i]} > 0$ and $R_1^{[t,i]} = 0$, formula (3.1) gives the influx of the tracer

$$J_1^{[t,i]} = L_1^{[t,i]} e^{p_1^{[i]}(0;z_1,d_1)} \left(\int_0^1 \frac{e^{p_1^{[i]}(x;z_1,d_1)}}{D_1(x)h(x)} dx \right)^{-1}.$$

Similarly, for the experiment associated with the boundary conditions (BVo) where $L_1^{[t,o]}=0$ and $R_1^{[t,o]}>0$, formula (3.1) gives the efflux of the tracer

$$J_1^{[t,o]} = -R_1^{[t,o]} e^{p_1^{[o]}(1;z_1,d_1)} \left(\int_0^1 \frac{e^{p_1^{[o]}(x;z_1,d_1)}}{D_1(x)h(x)} dx \right)^{-1}.$$

Formula (4.3) for the ratio of $J_1^{[t,i]}$ and $J_1^{[t,o]}$ then follows.

Corollary 4.2 Assume Hypotheses 2.1 and 2.2. For the one-isotope-setup (Setup 1) with ideal ionic mixtures, the flux ratio of the two unidirectional fluxes is

$$\frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -\frac{L_1^{[t,i]}e^{z_1\zeta_0V_0}}{R_1^{[t,o]}}\int_0^1 \frac{e^{z_1\zeta_0\phi^{[o]}(x)}}{D_1(x)h(x)}dx \; \Big(\int_0^1 \frac{e^{z_1\zeta_0\phi^{[i]}(x)}}{D_1(x)h(x)}dx\Big)^{-1},$$

where $\phi^{[i]}(x)$ is the profile of electric potential associated to the boundary condition (BVi) and $\phi^{[o]}(x)$ is that associated to the boundary condition (BVo).

Note that, even for ideal ionic mixtures where (see (2.7))

$$p_1^{[i]}(x; z_1, d_1) = z_1 \zeta_0 \phi^{[i]}(x)$$
 and $p_1^{[o]}(x; z_1, d_t) = z_1 \zeta_0 \phi^{[o]}(x)$,

the two profiles $\phi^{[i]}(x)$ and $\phi^{[o]}(x)$ are different due to different boundary conditions in (BVi) and (BVo). This difference in the electrical potential reflects the effects of permanent charge, more than the difference in boundary conditions. Thus, even for ideal ionic mixtures, the PNP model shows that the flux ratio in the one-isotope-setup (Setup 1) is specific and contains information on the permanent charge.



4.2 Flux Ratio for the Two-Isotope-Setup (Setup 2)

For this setup, one uses one main ion species, one counter ion species, and TWO tracers T_1 and T_2 (two different isotopes of the main ion species) in the SAME experiment. This is essentially the same setup used by Ussing in his derivation of formula (1.1). It turns out the flux ratio from this setup is universal when local models for excess potentials are used.

The boundary concentrations for tracers are as follows:

for tracer
$$T_1$$
: $L_1^{[t_1]} > 0$ at $x = 0$ and $R_1^{[t_1]} = 0$ at $x = 1$; for tracer T_2 : $L_1^{[t_2]} = 0$ at $x = 0$ and $R_1^{[t_2]} > 0$ at $x = 1$.

This would yield an estimate for the *influx* $J_1^{[t_1,i]}$ of tracer T_1 and an estimate for the *efflux* $J_1^{[t_2,o]}$ of tracer T_2 . We will examine the flux ratio $J_1^{[t_1,i]}/J_1^{[t_2,o]}$.

In the following table, we summarize the notations used.

Setup 2	Concentration	Valence	Flux
Main ion	$c_1^{[m]}$	$z_1 > 0$	$J_1^{[m]}$
Tracer T ₁	$c_1^{[t_1]}$	$z_1 > 0$	$J_1^{[t_1,i]}$
Tracer T ₂	$c_1^{[t_2]}$	$z_1 > 0$	$J_1^{[t_2,o]}$
Counter ion	c_2	$z_2 < 0$	J_2

The superscript $[t_1]$ in $c_1^{[t_1]}$, $J_1^{[t_1,i]}$, etc. indicates the corresponding quantity is associated with tracer T_1 , and the superscript i in $J_1^{[t_1,i]}$ indicates that it is the inward unidirectional flux of tracer T_1 . Similar remark applies to $[t_2]$ and o for tracer T_2 .

of tracer T_1 . Similar remark applies to $[t_2]$ and o for tracer T_2 . Let $(\phi(x), c_1^{[m]}(x), c_1^{[t_1]}(x), c_1^{[t_2]}(x), c_2(x), J_1^{[m]}, J_1^{[t_1,i]}, J_1^{[t_2,o]}, J_2)$ be a solution of boundary value problem of system (2.1) with boundary conditions

$$\phi(0) = V_0, \quad c_1^{[m]}(0) = L_1, \quad c_1^{[t_1]}(0) = L_1^{[t_1]}, \quad c_1^{[t_2]}(0) = 0, \quad c_2(0) = L_2;$$

$$\phi(1) = 0, \quad c_1^{[m]}(1) = R_1, \quad c_1^{[t_1]}(1) = 0, \quad c_1^{[t_2]}(1) = R_1^{[t_2]}, \quad c_2(1) = R_2.$$
(4.4)

The crucial observation is, since the two tracers are involved in the same experiment and they are assumed to have the same electrical and chemical properties (such as same valence z_1 and same diameter d_1 , etc.), both tracers have the same function

$$p_1(x; z_1, d_1) = z_1 \zeta_0 \phi(x) + \frac{1}{k_B T} \mu^{ex}(x; z_1, d_1)$$

defined in (2.7) and the same diffusion coefficient D_1 . Concerning the flux ratio, we have the following.

Theorem 4.3 Assume Hypotheses 2.1 and 2.2. For the two-isotope-setup (Setup 2) with two tracers T_1 and T_2 of the same valence and same diameter in one experiment, the flux ratio between the influx $J_1^{[t_1,i]}$ of tracer T_1 and the efflux $J_1^{[t_2,o]}$ of tracer T_2 is

$$\frac{J_1^{[t_1,i]}}{J_1^{[t_2,i]}} = -\frac{L_1^{[t_1]}}{R_1^{[t_2]}} \frac{e^{p_1(0;z_1,d_1)}}{e^{p_1(1;z_1,d_1)}}.$$
(4.5)



Proof Since the two tracers are involved in the same experiment and they have the same valence and diameter, the profile of the excess potential beyond the ideal component $k_B T p_1(x; z_1, d_1)$ is the same for both tracers T_1 and T_2 . Note also that the two tracers would have the same diffusion coefficient D_1 . Thus, for the tracer T_1 with $L_1^{[t_1]} > 0$ and $R_1^{[t_1]} = 0$, formula (3.1) gives its influx

$$J_1^{[t_1,i]} = L_1^{[t_1]} e^{p_1(0;z_1,d_1)} \left(\int_0^1 \frac{e^{p_1(x;z_1,d_1)}}{D_1(x)h(x)} dx \right)^{-1}.$$

Similarly, for the tracer T_2 with $L_1^{[t_2]} = 0$ and $R_1^{[t_2]} > 0$, its efflux is

$$J_1^{[t_2,o]} = -R^{[t_2]}e^{p_1(1;z_1,d_1)} \left(\int_0^1 \frac{e^{p_1(x;z_1,d_1)}}{D_1(x)h(x)} dx \right)^{-1}.$$

The formula (4.5) for the ratio of $J_1^{[t_1,i]}$ and $J_1^{[t_2,o]}$ then follows directly.

Note that, with local models for excess components, $p_1(0; z_1, d_1)$ and $p_1(1; z_1, d_1)$ in formula (4.5) are determined by the boundary concentrations of the whole ionic solution, not just those of tracers. Nevertheless, when local models for excess components are used in PNP models, the flux ratio from this setup (Setup 2) is completely determined by the boundary conditions—independent of the channel structure. It is universal for all channel types (described by PNP type models) independent of the parameters of the channel.

Corollary 4.4 Assume Hypotheses 2.1 and 2.2. For the two-isotope-setup (Setup 2) with two tracers in one experiment, if ionic mixture is treated as ideal ionic solution, then the flux ratio between the influx $J_1^{[t_1,i]}$ of tracer T_1 and the efflux $J_1^{[t_2,o]}$ of tracer T_2 is

$$\frac{J_1^{[t_1,i]}}{J_1^{[t_2,o]}} = -\frac{L_1^{[t_1]}}{R_1^{[t_2]}} e^{z_1 \zeta_0 V_0}.$$
(4.6)

Proof For ideal ionic solutions, it follows from (2.7) that $p_1(x; z_1, d_1) = z_1 \zeta_0 \phi(x)$. Formula (4.6) for ideal ionic mixtures is then a direct consequence of (4.5).

4.3 The One-Isotope-Setup (Setup 1) Versus the Two-Isotope-Setup (Setup 2) for Flux Ratios

We comment more on differences among estimators of flux ratios from the two setups.

At this moment, we are not able to give a comprehensive comparison between the flux ratios from the two setups. But, for the following situations, one may conclude that the flux ratio from the one-isotope-setup (Setup 1) is better than that from the two-isotope-setup (Setup 2) if the goal is to learn about the permanent charge.

For simplicity, for the one-isotope-setup (Setup 1), we take, $L_1^{[t,i]}=\rho$ at x=0 and $R_1^{[t,i]}=0$ at x=1 for (BVi) in (4.1), and $L_1^{[t,o]}=0$ at x=0 and $R_1^{[t,o]}=\rho$ at x=1for (BVo) in (4.2); for the two-isotope-setup (Setup 2), we take, $L_1^{[t_1]} = \rho$ and $L_1^{[t_2]} = 0$ at x = 0, and $R_1^{[t_1]} = 0$ and $R_1^{[t_2]} = \rho$ at x = 1.

(i) We already see that, for PNP with any local model for the excess potentials, the flux ratio from the two-isotope-setup (Setup 2) is given by (4.5) recast as follows:

$$\frac{J_1^{[t_1,i]}}{J_1^{[t_2,o]}} = -e^{p_1(0;z_1,d_1) - p_1(1;z_1,d_1)}.$$



In particular, the two-isotope estimator has nothing to do with the channel structure. The two isotope estimator is universal.

On the other hand, it follows from (4.3), the estimator of the flux ratio from the one-isotope-setup (Setup 1) is

$$\frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -e^{p_1^{[i]}(0;z_1,d_1) - p_1^{[o]}(1;z_1,d_1)} \int_0^1 \frac{e^{p_1^{[o]}(x;z_1,d_1)}}{D_1(x)h(x)} dx$$
$$\left(\int_0^1 \frac{e^{p_1^{[i]}(x;z_1,d_1)}}{D_1(x)h(x)} dx\right)^{-1}.$$

For PNP with *local model* for the excess potentials, we do have

$$e^{p_1^{[i]}(0;z_1,d_1)-p_1^{[o]}(1;z_1,d_1)}=e^{p_1(0;z_1,d_1)-p_1(1;z_1,d_1)},$$

and hence, the first factor in the expression of $J_1^{[t,i]}/J_1^{[t,o]}$ from the one-isotope-setup (Setup 1) equals, itself, to the flux ratio $J_1^{[t_1,i]}/J_1^{[t_2,o]}$ from the two-isotope-setup (Setup 2). The last two factors in the expression of $J_1^{[t,i]}/J_1^{[t,o]}$ contain significant information, namely, both factors involve permanent charge effects, even for PNP with ideal electrochemical components only. In this sense, the flux ratio measured in the one-isotope-setup (Setup 1) contains more information on channel structure than that in the two-isotope-setup (Setup 2). Although this came as a surprise to some of us, who had been inoculated with traditional views of unifluxes long ago [21,46], it should not have. Setup 1 with one tracer involves two different spatial arrangements, and so it should give more information, particularly about any asymmetry in the charge distribution.

Recall that $p_1^{[i]}(x;z_1,d_1)$ is determined by the profiles of concentrations from the solution of BVP associated to the boundary condition (BVi) in (4.1) and $p_1^{[o]}(x;z_1,d_1)$ is determined by the profiles of concentrations from the solution of BVP associated to the boundary condition (BVo) in (4.2). The difference between $p_1^{[o]}(x;z_1,d_1)$ and $p_1^{[i]}(x;z_1,d_1)$ should be of order ρ . We are expecting that the channel structure appears in terms of order ρ . This is indeed true as shown in formula (5.14) for the simple case that was treated in Sect. 5.

(ii) As claimed in Remark 2.3, the above discussion is valid even if the local assumption (2.2) on the excess potentials is required only in the ionic solution outside the channel. We now consider PNP with *nonlocal* models for the excess potentials everywhere (assuming the BVP is well-defined).

It is a reasonable assumption that the nonlocal model for the excess potentials and its local version differ in terms that are higher order (quadratic) in ionic diameters.

Denote c_0 a characteristic concentration (number per length for one-dimensional model) of the ionic mixture. Let z be the valence and d be the diameter of the tracer.

We will assume the ionic mixture is reasonably dilute near x = 0 and x = 1, and the permanent charge is small relative to the characteristic concentration.

For clarity of the statement, denote the flux ratio from the one-isotope-setup (Setup 1) by $\sigma_1(\rho, d, Q)$ and the flux ratio from the two-isotope-setup (Setup 2) by $\sigma_2(\rho, d, Q)$. Then, one can argue that,

$$\sigma_1(\rho, d, Q) = -e^{z\xi_0 V_0} \Big(1 + a_1(\rho, c_0)(c_0 d) + a_2(\rho, c_0)(c_0 d)^2 + G(\rho, c_0) \frac{Q}{c_0} + h.o.t. \Big),$$

$$\sigma_2(\rho, d, Q) = -e^{z\xi_0 V_0} \Big(1 + a_1(\rho, c_0)(c_0 d) + a_2(\rho, c_0)(c_0 d)^2 + a_2(\rho, c_0)(c_0 d)^2 + a_2(\rho, c_0)(c_0 d)^2 \Big)$$



$$+b(\rho,c_0)\frac{Q}{c_0}(c_0d)^2+h.o.t.$$
.

Note that the first three terms for both σ_1 and σ_2 are the same and they DO NOT contain information of channel structure. Those terms are universal. The term $G(\rho, c_0) \frac{Q}{c_0}$ for σ_1 and the term $b(\rho, c_0) \frac{Q}{c_0} (c_0 d)^2$ for σ_2 contain information of channel structure. They are specific.

The dilute assumption would imply that $(c_0d)^2 \ll 1$ (for one-dimensional PNP).

Therefore, permanent charge Q appears in the zeroth order $O(d^0)$ -term in σ_1 but it appears in σ_2 until the quadratic order $O(d^2)$. We conclude that the one-isotope-setup (Setup 1) is better than the two-isotope-setup (Setup 2) in capturing the effect of permanent charge in this situation.

When the ionic mixture is crowded, the above formulas for σ_1 and σ_2 are not valid and we would not be able to compare them in any definite terms at this moment.

5 Case Studies for Flux Ratios from the One-Isotope-Setup

In this section, we consider specific flux ratios from the one-isotope-setup (Setup 1) in special cases to illustrate further some detailed information of channel structure that could be extracted from flux ratios. We assume

(A1) the permanent charge is given by

$$Q(x) = \begin{cases} 0 & \text{for } x \in (0, a) \cup (b, 1), \\ Q_0 & \text{for } x \in (a, b), \end{cases}$$
 (5.1)

where 0 < a < b < 1 and Q_0 is a constant.

Note that the channel length has been normalized to 1 (see below for a dimensionless rescaling).

5.1 Rescaling of the Model System (2.1)

The main results for this special case rely heavily on the work in [51,56] where the results are stated in terms of dimensionless variables after a rescaling. We will translate the results in terms of the original variables but for the reader's convenience in comparing the statements, we present a full dimensionless rescaling below.

The following rescaling (see [32]) or its variations have been widely used for convenience of mathematical analysis. Set

$$C_0 = \max \left\{ \sup_{x} |Q(x)|, L_k, R_k \right\}, \quad \hat{D}_0 = \sup_{x,k} \{D_k(x)\}, \quad \hat{\varepsilon}_r = \sup_{x} \varepsilon_r(x).$$

Let the channel length be l. Note that, in the previous sections, we have normalized the length of the channel to l=1 and will still use this normalization except in the following rescaling. We make the re-scaling to get dimensionless variables

$$\varepsilon^{2} = \frac{\hat{\varepsilon}_{r} \varepsilon_{0} k_{B} T}{e_{0}^{2} l^{2} C_{0}}, \quad \hat{D}_{k}(x) = \frac{D_{k}(x)}{\hat{D}_{0}}, \quad \hat{Q}(x) = \frac{Q(x)}{C_{0}}, \quad \hat{\varepsilon}_{r}(x) = \frac{\varepsilon_{r}(x)}{\hat{\varepsilon}_{r}}$$

$$\hat{\phi}(x) = \frac{e_{0}}{k_{B} T} \phi(x) = \zeta_{0} \phi(x), \quad \hat{c}_{k}(x) = \frac{c_{k}(x)}{C_{0}}, \quad \hat{J}_{k} = \frac{J_{k}}{l C_{0} \hat{D}_{0}}.$$
(5.2)



In terms of the new variables, the BVP (2.1) and (2.2) becomes

$$\frac{\varepsilon^2}{h(x)} \frac{d}{dx} \left(\hat{\varepsilon}_r(x) h(x) \frac{d\hat{\phi}}{dx} \right) = -\sum_{s=1}^n z_s \hat{c}_s - \hat{Q}(x),$$

$$\frac{1}{k_B T} \hat{D}_k(x) h(x) \hat{c}_k \frac{d\mu_k}{dx} = -\hat{J}_k, \quad \frac{d\hat{J}_k}{dx} = 0,$$
(5.3)

with boundary conditions at x = 0 and x = 1

$$\hat{\phi}(0) = \zeta_0 V_0, \ \hat{c}_k(0) = \frac{L_k}{C_0}; \quad \hat{\phi}(1) = 0, \ \hat{c}_k(1) = \frac{R_k}{C_0}.$$
 (5.4)

We will assume a special form for the permanent charge and include a hard-sphere potential. More precisely, we assume

(A2) $\hat{\varepsilon}_r(x)$ and $\hat{D}_k(x) = D_k$ are constants, and the dimensionless quantity ε is small. (A3) a one-dimensional local hard-sphere potential model is

$$\frac{1}{k_B T} \mu_k^{LHS}(x) = -\ln\left(1 - \sum_{j=1}^n d_j C_0 \hat{c}_j(x)\right) + \frac{d_k \sum_{j=1}^n C_0 \hat{c}_j(x)}{1 - \sum_{j=1}^n d_j C_0 \hat{c}_j(x)}$$

$$= \sum_{j=1}^n (d_j + d_k) C_0 \hat{c}_j(x) + O(d_k d_j) \tag{5.5}$$

where d_i is the diameter of the jth ion species.

The PNP model with local hard-sphere models (5.5) was studied in [54]. The local hard-sphere model (5.5) is an approximation of the nonlocal hard-sphere model adopted in [50,58] from [73].

The effects of the permanent charge and ion sizes on flux ratios will be examined. This will be accomplished by considering the permanent charge effect first and followed by ion size effect, and then the combination of these two. All these are done with extra assumptions so that a regular perturbation approach allows us to obtain detailed and useful information. Hopefully, this perturbation result provides insights and indications for more realistic models and for the real biological problem. While our analysis is neither general nor perfect, we (immodestly) believe it significantly more helpful than no discussion at all [37,77] or analysis that assumes electrical potentials are independent of charge and structure.

In the rest, we consider an ionic mixture of two (n = 2) ion species containing one main ion species with valence $z_1 > 0$ and diameter d_1 and a counter ion species with valence $z_2 < 0$ and diameter d_2 . Our assumptions are (A1)-(A3), in addition to Hypotheses 2.1 and 2.2. Set $d = d_1$ and $\lambda = d_2/d_1$. For the local hard-sphere model (5.5) in (A3), in terms of the original variables, one has, from (2.7),

$$p_1(x; z_1, d_1) = z_1 \zeta_0 \phi(x) + \frac{1}{k_B T} \mu_1^{LHS}(x)$$

$$= z_1 \zeta_0 \phi(x) + d(2c_1(x) + (1 + \lambda)c_2(x)) + O(d^2).$$
(5.6)

5.2 Approximations of Specific Flux Ratios

Consider the one-isotope-setup (Setup 1) with one tracer but two sets of boundary conditions. For one experiment, the tracer is injected from the left boundary with concentrations $L_1^{[t,i]} = \rho$ and $R_1^{[t,i]} = 0$ that produces the influx $J_1^{[t,i]}$. In another experiment, the same tracer is



injected from the right boundary with concentrations $R_1^{[t,o]} = \rho$ and $L_1^{[t,o]} = 0$ that produces the efflux $J_1^{[t,o]}$.

Our goal here is to provide an explicit approximation formula for the flux ratio. Of course, this is nearly impossible in general and only *approximations* are possible. Experimentalists are mostly concerned with particular cases, particular channels of biological and medical interest. Each of those cases will allow its own appropriate approximations because each case will be known in detail experimentally. Thus, the lack of generality is much less serious than it seems. The tools provided here will allow analysis appropriate for any particular system that is reasonably well studied. Our approximation has two levels. More precisely, with the assumption that ε is small, we will only examine the zeroth order in ε term of the flux ratio. (We will abuse the notion in the following to refer to the zeroth order in ε term of the flux ratio simply as the flux ratio.) Then the flux ratio depends on ion diameters, permanent charge, and the injected concentrations of the tracer, and, with the assumption that these quantities are also small, we are able to obtain an approximate formula of the flux ratio with *explicit* leading order terms in these quantities.

The following quantities will be needed to state the results. Recall that h(x) is the cross-section area of the channel over x, and $Q(x) = Q_0$ for $x \in (a, b)$ and Q(x) = 0 for $x \notin [a, b]$. We denote $H(x) = \int_0^x h^{-1}(s)ds$. For ease of notation, we set

$$s = \frac{L_1}{R_1}, \quad \alpha = \frac{H(a)}{H(1)}, \quad \beta = \frac{H(b)}{H(1)},$$
 (5.7)

and define $f_1(s)$, $f_2(V_0, s)$, $g_1(V_0, s, \alpha, \beta)$, and $g_2(s, \alpha, \beta)$ as

$$f_{1}(s) = \frac{2s \ln s - s^{2} + 1}{s(s-1) \ln s},$$

$$f_{2}(V_{0}, s) = \frac{s+1}{s(z_{1}\zeta_{0}V_{0} + \ln s)} - \frac{e^{z_{1}\zeta_{0}V_{0}} + 1}{se^{z_{1}\zeta_{0}V_{0}} - 1},$$

$$(5.8)$$

$$g_{1}(V_{0}, s, \alpha, \beta) = -\frac{(\beta - \alpha)[(\alpha + \beta - 2\alpha\beta)(s-1)^{2} + 2s]}{(z_{1} - z_{2})[(1 - \alpha)s + \alpha]^{2}[(1 - \beta)s + \beta]^{2}(\ln s)^{2}} \left(z_{2}\zeta_{0}V_{0} + \ln s\right)$$

$$+ \frac{2(\beta - \alpha)(s^{2} - 1)}{(z_{1} - z_{2})[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta]s(\ln s)^{3}} \left(z_{2}\zeta_{0}V_{0} + \frac{\ln s}{2}\right)$$

$$+ \frac{(\beta - \alpha)(s + 1)}{(z_{1} - z_{2})[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta](s - 1) \ln s} z_{2}\zeta_{0}V_{0}$$

$$+ \frac{(2 \ln s + s - 1/s)[\ln((1 - \beta)s + \beta) - \ln((1 - \alpha)s + \alpha)]}{(z_{1} - z_{2})(s - 1)^{2}(\ln s)^{2}} z_{2}\zeta_{0}V_{0},$$

$$g_{2}(s, \alpha, \beta) = \frac{s+1}{(z_{1} - z_{2})s(s - 1) \ln s} \ln \frac{(1 - \beta)s + \beta}{(1 - \alpha)s + \alpha}$$

$$+ \frac{(\beta - \alpha)(s^{2} - 1)}{(z_{1} - z_{2})[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta]s(\ln s)^{2}}.$$

$$(5.9)$$

Denote the boundary concentrations of the main ion species and the counter ion species, before the tracer is added, by (L_1, L_2) at x = 0 and (R_1, R_2) at x = 1, and assume the electroneutrality conditions among them

$$z_1L_1 + z_2L_2 = 0$$
 and $z_1R_1 + z_2R_2 = 0$. (5.10)

For the electroneutrality boundary conditions, we consider the following two cases.



5.2.1 Total Electroneutrality Boundary Conditions

The first case is, after the tracer is included, one requires the total electroneutrality boundary conditions among all three ion species; that is, the boundary conditions for the two experiments are, respectively,

(BVi):
$$\begin{cases} \phi^{[i]}(0) = V_0, & \phi^{[i]}(1) = 0, \\ c_1^{[m,i]}(0) = L_1, & c_1^{[m,i]}(1) = R_1, \text{ (main ions)} \\ c_1^{[t,i]}(0) = \rho > 0, & c_1^{[t,i]}(1) = 0, \text{ (tracer)} \\ c_2^{[i]}(0) = L_2 - \frac{z_1}{z_2}\rho, c_2^{[i]}(1) = R_2; \text{ (counterions)} \end{cases}$$

$$\begin{cases} \phi^{[o]}(0) = V_0, & \phi^{[o]}(1) = 0, \\ c_1^{[m,o]}(0) = L_1, c_1^{[m,o]}(1) = R_1, \text{ (main ions)} \\ c_1^{[t,o]}(0) = 0, & c_1^{[t,o]}(1) = \rho > 0, \text{ (tracer)} \\ c_2^{[o]}(0) = L_2, & c_2^{[o]}(1) = R_2 - \frac{z_1}{z_2}\rho. \text{ (counterions)} \end{cases}$$

$$(5.12)$$

(BVo):
$$\begin{cases} \phi^{[o]}(0) = V_0, & \phi^{[o]}(1) = 0, \\ c_1^{[m,o]}(0) = L_1, & c_1^{[m,o]}(1) = R_1, & \text{(main ions)} \\ c_1^{[t,o]}(0) = 0, & c_1^{[t,o]}(1) = \rho > 0, & \text{(tracer)} \\ c_2^{[o]}(0) = L_2, & c_2^{[o]}(1) = R_2 - \frac{z_1}{z_2}\rho. & \text{(counterions)} \end{cases}$$
(5.12)

That is, for (BVi), one adds the extra amount $-z_1\rho/z_2$ of counter ion concentration at x=0to compensate the inclusion of the tracer concentration ρ at x=0; and, for (BVo), one adds the extra amount $-z_1 \rho/z_2$ of counter ion concentration at x=1 to compensate the inclusion of the tracer concentration ρ at x = 1. Therefore.

For (BVi):
$$z_1(L_1 + \rho) + z_2(L_2 - z_1\rho/z_2) = 0$$
 and $z_1R_1 + z_2R_2 = 0$,
For (BVo): $z_1L_1 + z_2L_2 = 0$ and $z_1(R_1 + \rho) + z_2(R_2 - z_1\rho/z_2) = 0$. (5.13)

Then we have

Theorem 5.1 Assume d, ρ , and $|Q_0|$ are small. The flux ratio between the influx $J_1^{[t,i]}$ associated to the boundary condition (5.11) and the efflux $J_1^{[t,o]}$ associated to the boundary condition (5.12) is, with $s = L_1/R_1$,

$$\begin{split} \frac{J_{1}^{[t,i]}}{J_{1}^{[t,o]}} &= -e^{z_{1}\zeta_{0}V_{0}} \Big(1 + \Big(2(L_{1} - R_{1}) + (1 + \lambda)(L_{2} - R_{2}) \Big) d \Big) \\ &- e^{z_{1}\zeta_{0}V_{0}} \left(f_{1}(s) + f_{2}(V_{0}, s) \right) \frac{\rho}{R_{1}} - e^{z_{1}\zeta_{0}V_{0}} g_{1}(V_{0}, s, \alpha, \beta) \frac{Q_{0}}{R_{1}} \frac{\rho}{R_{1}} \\ &+ O(\rho^{2}, \rho d, d^{2}, \rho Q_{0}^{2}, \rho^{2} Q_{0}, \rho d Q_{0}), \end{split}$$
(5.14)

where α and β are in (5.7), f_1 and f_2 are in (5.8), and g_1 are in (5.9).

Formula (5.14) will be established in "Appendix" (Sect. 7). The flux ratio is specific due to the third term involving the key parameters Q_0 , α and β of the prescribed channel structure (see (5.1) and (5.7)).

5.2.2 Partial Electroneutrality Boundary Conditions

The other case is to simply keep the concentrations of the main ion species and the counter ion species for both experiments after the tracer is included; that is, the boundary conditions are

(BVi):
$$\begin{cases} \phi^{[i]}(0) = V_0, & \phi^{[i]}(1) = 0, \\ c_1^{[m,i]}(0) = L_1, & c_1^{[m,i]}(1) = R_1, & \text{(main ions)} \\ c_1^{[i,i]}(0) = \rho > 0, & c_1^{[i,i]}(1) = 0, & \text{(tracer)} \\ c_2^{[i]}(0) = L_2 > 0, & c_2^{[i]}(1) = R_2 > 0. & \text{(counterions)} \end{cases}$$
(5.15)



(BVo):
$$\begin{cases} \phi^{[o]}(0) = V_0, & \phi^{[o]}(1) = 0, \\ c_1^{[m,o]}(0) = L_1 > 0, & c_1^{[m,o]}(1) = R_1 > 0, \text{ (main ions)} \\ c_1^{[t,o]}(0) = 0, & c_1^{[t,o]}(1) = \rho > 0, \text{ (tracer)} \\ c_2^{[o]}(0) = L_2 > 0, & c_2^{[o]}(1) = R_2 > 0. \text{ (counterions)} \end{cases}$$
(5.16)

In this case, one has

For (BVi):
$$z_1(L_1 + \rho) + z_2L_2 = z_1\rho \approx 0$$
 and $z_1R_1 + z_2R_2 = 0$,
For (BVo): $z_1L_1 + z_2L_2 = 0$ and $z_1(R_1 + \rho) + z_2R_2 = z_1\rho \approx 0$. (5.17)

Thus, one only has approximate electroneutrality boundary conditions after the tracer is added. But, since the amounts of tracers injected are small and the net amounts of charge resulting from approximate electroneutrality are exceedingly small, this approximate electroneutrality boundary condition is realistic and more practical too.

Theorem 5.2 Assume d, ρ , and $|Q_0|$ are small. The flux ratio between the influx $J_1^{[t,i]}$ associated to the boundary condition (5.15) and the efflux $J_1^{[t,o]}$ associated to the boundary condition (5.16) is, with $s = L_1/R_1$,

$$\frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -e^{z_1\zeta_0 V_0} \left(1 + \left(2(L_1 - R_1) + (1+\lambda)(L_2 - R_2) \right) d \right)
- e^{z_1\zeta_0 V_0} \left(\frac{-z_2}{z_1 - z_2} f_1(s) + f_2(V_0, s) \right) \frac{\rho}{R_1}
- e^{z_1\zeta_0 V_0} \frac{-z_2}{z_1 - z_2} \left(g_1(V_0, s, \alpha, \beta) + g_2(s, \alpha, \beta) \right) \frac{Q_0}{R_1} \frac{\rho}{R_1}
+ O(\rho^2, \rho d, d^2, \rho Q_0^2, \rho^2 Q_0, \rho d Q_0),$$
(5.18)

where α and β are in (5.7), f_1 and f_2 are in (5.8), and g_1 and g_2 are in (5.9).

The derivation of formula (5.18) will also be given in "Appendix" (Sect. 7).

5.3 Comments on Formulas (**5.14**) and (**5.18**)

The derivation of formulas (5.14) and (5.18) in Sect. 7 is rather complicated. To gain additional confidence in the correctness of the formula, we have cross-checked it using a symmetry of the problem, that is, the result should be symmetric if one swaps the channel between the left end and the right end. More precisely, if we set $\hat{x} = 1 - x$, then x = 0 becomes $\hat{x} = 1$, and x = 1 becomes $\hat{x} = 0$. If we denote the relevant quantities for the new situation with an overhat, then $\hat{L}_j = R_j$, $\hat{R}_j = L_j$, $\hat{V}_0 = -V_0$, $\hat{s} = \hat{L}_1/\hat{R}_1 = 1/s$, $\hat{J}_1^{[t,i]} = -J_1^{[t,o]}$ and $\hat{J}_1^{[t,o]} = -J_1^{[t,i]}$, etc. Therefore, one should have

$$\frac{\hat{J}_{1}^{[t,i]}}{\hat{J}_{1}^{[t,o]}} = \frac{J_{1}^{[t,o]}}{J_{1}^{[t,i]}}.$$

The latter is equivalent to, up to the leading orders in (5.14) and (5.18), the relations

$$f_1(1/s) = -sf_1(s), \quad f_2(-V_0, 1/s) = -sf_2(V_0, s),$$

$$g_1(-V_0, 1/s, 1 - \beta, 1 - \alpha) = -s^2g_1(V_0, s, \alpha, \beta),$$

$$g_2(1/s, 1 - \beta, 1 - \alpha) = -s^2g_2(s, \alpha, \beta)$$



where f_1 , f_2 , g_1 and g_2 are defined in (5.8) and (5.9). We have verified them all!

For *ideal* ionic solutions, formulas (5.14) and (5.18) reduce to, for the total electroneutrality boundary conditions (5.11) and (5.12),

$$\frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -e^{z_1\zeta_0V_0} - e^{z_1\zeta_0V_0} \left(f_1(s) + f_2(V_0, s) + g_1(V_0, s, \alpha, \beta) \frac{Q_0}{R_1} \right) \frac{\rho}{R_1} + O(\rho^2, \rho Q_0^2),$$
(5.19)

and, for the approximate electroneutrality boundary conditions (5.15) and (5.16),

$$\frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -e^{z_1\zeta_0V_0} - e^{z_1\zeta_0V_0} \left(\frac{-z_2}{z_1 - z_2} f_1(s) + f_2(V_0, s)\right) \frac{\rho}{R_1} \\
- e^{z_1\zeta_0V_0} \frac{-z_2}{z_1 - z_2} \left(g_1(V_0, s, \alpha, \beta) + g_2(s, \alpha, \beta)\right) \frac{Q_0}{R_1} \frac{\rho}{R_1} + O(\rho^2, \rho Q_0^2). \tag{5.20}$$

It is noted that, even for ideal ionic solutions, the flux ratio from the one-isotope-setup (Setup 1) is specific and captures some properties of the channel structure. *Implications of formula* (5.14) The following properties of f_1 , f_2 , g_1 , and g_2 can be established easily and will be used in the discussions below.

Lemma 5.3 For 0 < s < 1, $f_1(s) > 0$, for s > 1, $f_1(s) < 0$,

$$\lim_{s \to 0^{+}} f_{1}(s) = +\infty, \quad \lim_{s \to 1} f_{1}(s) = \lim_{s \to \infty} f_{1}(s) = 0, \quad \lim_{z_{1} \zeta_{0} V_{0} \to -\ln s} f_{2}(V_{0}, s) = \frac{s-1}{2s},$$

$$\lim_{s \to 1} g_{1}(V_{0}, s, \alpha, \beta) = -\frac{z_{2} \zeta_{0} V_{0}(\beta - \alpha)}{6(z_{1} - z_{2})} \left((2\alpha + 2\beta - 1)^{2} + 4[(\alpha - 1)^{2} + (\beta - 1)^{2} - 1] \right)$$

$$-\frac{2(\beta - \alpha)(\alpha + \beta - 1)}{z_{1} - z_{2}},$$

$$\lim_{s \to 1} g_{2}(s, \alpha, \beta) = -\frac{(\beta - \alpha)(\alpha + \beta - 1)}{z_{1} - z_{2}}.$$
(5.21)

We discuss some indications of each of the three leading terms on the right-hand side of the formula (5.14). Similar comments apply to formula (5.18).

(a) The first term

$$-e^{z_1\zeta_0V_0}\Big(1+\big(2(L_1-R_1)+(1+\lambda)(L_2-R_2)\big)d\Big)$$

represents directly the asymmetry of the electrochemical potentials (the concentration and the electrical 'driving force' using the language of the laboratory, introduced by Hodgkin and Huxley) at the two boundary points x = 0 and x = 1 (independent of the concentration ρ of the tracer). In particular, as $\rho \to 0$ in (5.14),

$$\lim_{\rho \to 0} \frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -e^{z_1 \zeta_0 V_0} - e^{z_1 \zeta_0 V_0} (2(L_1 - R_1) + (1 + \lambda)(L_2 - R_2))d + O(d^2).$$

Note that, the value for the limit of the flux ratio, NOT equaling to -1 in general, reflects the asymmetry of the boundary conditions. The effects caused by permanent charge disappears in the $\rho \to 0$ limit. A direct justification (as an alternative to a consequence of the formula (5.14)) of the latter is given in Remark 7.1. Remark 7.1 also explains why there is no dQ_0 term in the approximation formula (5.14).



(b) In formula (5.14), the term

$$-e^{z_1\zeta_0V_0}(f_1(s)+f_2(V_0,s))\frac{\rho}{R_1}$$

represents the interaction between the tracer and the asymmetry of the boundary electrochemical potentials.

(c) In formula (5.14), the term

$$-e^{z_1\zeta_0V_0}g_1(V_0, s, \alpha, \beta)\frac{\rho Q_0}{R_1^2}$$

contains the interaction between the tracer, the asymmetry of boundary electrochemical potentials, and the permanent charge (in this simplified setting).

(d) If the boundary conditions are symmetric, that is, $V_0 = 0$, $L_1 = R_1$ and $L_2 = R_2$, then, from Lemma 5.3, formula (5.14) reduces to

$$\frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -1 + \frac{2(\beta - \alpha)(\alpha + \beta - 1)}{z_1 - z_2} \frac{Q_0}{R_1} \frac{\rho}{R_1} + O(\rho^2, \rho Q_0^2).$$

In this case, the effect of permanent charge on the flux ratio is particularly captured. Flux ratio and the flux ratio exponent n' Next, we discuss the implications of formula (5.14) for a relation between the flux ratio with the flux ratio exponent n' introduced by Hodgkin and Kenyes in (1.3), under further assumptions. Similar comment applies to the term in formula

Recall, from (1.3) with $L_1^{[t,i]} = R_1^{[t,o]} = \rho$, that

$$\frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -e^{z_1\zeta_0 V_0 n'}.$$

Therefore, the flux ratio exponent n' is given by, ignoring the higher order terms,

$$\begin{split} n' &= \frac{1}{z_1 \zeta_0 V_0} \ln \left(-\frac{J_1^{[t,i]}}{J_1^{[t,o]}} \right) \\ &\approx 1 + \frac{g_1(V_0,s,\alpha,\beta) Q_0/R_1 + f_1(s) + f_2(V_0,s)}{z_1 \zeta_0 V_0} \frac{\rho}{R_1} \\ &+ \frac{2d_1(L_1 - R_1) + (d_1 + d_2)(L_2 - R_2)}{z_1 \zeta_0 V_0}. \end{split}$$

In particular, if the concentrations L_j 's and R_j 's at the boundaries are such that $2d_1(L_1 - R_1) + (d_1 + d_2)(L_2 - R_2)$ can be ignored, then one has

$$n' \approx 1 + \frac{g_1(V_0, s, \alpha, \beta)Q_0/R_1 + f_1(s) + f_2(V_0, s)}{z_1\zeta_0V_0} \frac{\rho}{R_1}.$$

Since the above formula is obtained under the assumption that Q_0 is small and the ionic mixture is reasonably dilute, we cannot apply it to large Q_0 . BUT, if we pretend that the formula were true for large Q_0 , then $g_1(V_0, s, \alpha, \beta)Q_0/R_1$ dominates $f_1(s) + f_2(V_0, s)$, and hence,

$$n' \approx 1 + \frac{g_1(V_0, s, \alpha, \beta)Q_0}{z_1\zeta_0V_0} \frac{\rho}{R_1^2},$$

which implies, when $g_1(V_0, s, \alpha, \beta) \neq 0$,

$$n'>1 \ \ \text{if} \ \ \frac{g_1(V_0,s,\alpha,\beta)}{z_1\zeta_0V_0}Q_0>0 \quad \ \text{and} \quad \ n'<1 \ \ \text{if} \ \ \frac{g_1(V_0,s,\alpha,\beta)}{z_1\zeta_0V_0}Q_0<0;$$

that is, n' > 1 for Q_0 with one sign and n' < 1 for Q_0 with the opposite sign. Detecting (α, β, Q_0) using (5.14) Assume the permanent charge has the general structure characterized by (α, β, Q_0) . We will propose a procedure for determining these quantities. Rearrange formula (5.14) to get

$$\begin{split} e^{-z_1\zeta_0V_0} \frac{J_1^{[t,i]}}{J_1^{[t,o]}} + 1 + \Big(2(L_1 - R_1) + (1+\lambda)(L_2 - R_2)\Big)d\\ + (f_1(s) + f_2(V_0, s))\frac{\rho}{R_1}\\ = -g_1(V_0, s, \alpha, \beta)\frac{\rho Q_0}{(R_1)^2} + O(\rho^2, \rho d, d^2, \rho Q_0^2, \rho^2 Q_0, \rho d Q_0). \end{split}$$

All terms on the left-hand side can be determined either by experimental setup or by measurement. Under the assumption, the first term on the right-hand side is the leading term that contains information on net or overall effect of permanent charge and channel geometry through its dependence on Q_0 and (α, β) . In general, three choices of (V_0, L_1, R_1) lead to three equations for (Q_0, α, β) that could determine the values of Q_0, α and β .

6 Discussion

As an extremely important experimental method in studying of channel properties, flux ratios have been widely applied [37,77]. Their dependence on physical parameters is subtle and is dictated by details of experimental designs. To emphasize the importance of the subtleness of flux ratios, we classify them into two main classes: universal and specific. Universal flux ratios are those independent of channel structures and specific flux ratios contain information of channel structures.

In this paper, we have examined two applications of flux ratios: (i) proportionality constant of the flux of a main ion species and the flux of its tracer; (ii) flux ratios of tracers associated to two experimental setups.

For the first topic, it is shown that, based on analysis of PNP type models including *local* excess potentials in Sect. 3, the proportionality constant of the flux of a main ion species and the flux of its tracer is universal and can be completely determined by boundary conditions, and hence, one can estimate the flux of the main ion species from that of its tracer. Furthermore, an experimental design is proposed (Remark 3.3) based on the analysis so that the proportionality constant can be determined in a simple and precise way even for PNP models with *nonlocal* models of excess potentials.

For the second topic, based on analysis of PNP type models with *local* excess potentials in Sect. 4, we examined two popular experimental designs for measuring flux ratios of tracers. We showed that the two-isotope-setup (Setup 2) yields universal flux ratios that do not reveal channel structure but the one-isotope-setup (Setup 1) is specific even with dilute ionic mixtures. As claimed in Remark 2.3, it is not hard to see that the local nature in Hypothesis 2.2 can be replaced by assuming the hypothesis only at the bathes as long as the BVP is well-posed.



Presumably, if one takes PNP with *nonlocal* excess potential models (inside and outside of the channel), then the flux ratios for both setups might capture information on channel structures. However, at this moment, it is not clear how different they are, and this requires a serious investigation of PNP systems with nonlocal excess potential models. To our best knowledge, PNP including nonlocal excess potential models has not been mathematically analyzed. In fact, the well-posedness issue for such a model is not clear due to its infinite number of freedoms; that is, what should be "the boundary conditions" in order for the boundary value problem of a PNP model with nonlocal excess potentials to have a unique or finite many solutions? An initial effort is taken in [75] for a simplified setup and hope this activity can stimulate further investigations on PNP model with nonlocal excess potentials.

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7 Appendix: Derivations of Results in Sect. 5.2

In this section, we provide a derivation of formula (5.14) in Theorem 5.1 and formula (5.18) in Theorem 5.2 from the basic formula (4.3) in Theorem 4.1 for flux ratios from the one-isotope-setup (Setup 1). The derivation for both formulas are similar so we will provide the detailed derivation for formula (5.14) in Sect. 7.2 and comment on differences in the derivation for formula (5.18) in Sect. 7.3.

7.1 A Reformulation of (4.3) for Cases in Sect. 5.2

We will first recall the setup of the case specified in Sect. 5.2 and give a new form of formula (4.3) for the special case, which is convenient for us to apply previously established results in late part.

Recall that, for the one-isotope-setup (Setup 1), one tracer is used for two experimental settings with two different sets of boundary conditions for tracers. For one experiment, the tracer is injected from the left boundary with concentration $L_1^{[t,i]} = \rho$ and zero right boundary concentration $R_1^{[t,i]} = 0$ that produces the influx $J_1^{[t,i]}$. In another experiment, the same tracer is injected from the right boundary with concentration $R_1^{[t,o]} = \rho$ and zero left boundary concentration $L_1^{[t,o]} = 0$ that produces the efflux $J_1^{[t,o]}$.

Formula (4.3) in Theorem 4.1 for the flux ratio between $J_1^{[t,i]}$ and $J_1^{[t,o]}$ is

$$\frac{J_{1}^{[t,i]}}{J_{1}^{[t,o]}} = -\frac{L_{1}^{[t,i]}e^{p_{1}^{[i]}(0;z_{1},d_{1})}}{R_{1}^{[t,o]}e^{p_{1}^{[o]}(1;z_{1},d_{1})}} \int_{0}^{1} \frac{e^{p_{1}^{[o]}(x;z_{1},d_{1})}}{D_{1}(x)h(x)} dx \left(\int_{0}^{1} \frac{e^{p_{1}^{[i]}(x;z_{1},d_{1})}}{D_{1}(x)h(x)} dx \right)^{-1}, \tag{7.1}$$

where $p_1^{[i]}(x; z_1, d_1)$ defined in (2.7) is determined by the profiles of concentrations from the solution of BVP associated with the boundary condition (BVi), and $p_1^{[o]}(x; z_1, d_1)$ defined in (2.7) is determined by the profiles of concentrations from the solution of BVP associated with the boundary condition (BVo).

Remark 7.1 Note that, as $\rho \to 0$, one has $p_1^{[i]}(x; z_1, d_1) = p_1^{[o]}(x; z_1, d_1)$, and hence,

$$\lim_{\rho \to 0} \frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -\frac{L_1^{[t,i]}e^{p_1^{[i]}(0;z_1,d_1)}}{R_1^{[t,o]}e^{p_1^{[o]}(1;z_1,d_1)}};$$



in particular, this limit does not contain information on permanent charge Q. An technical implication is that all terms involving Q_0 in the approximation of $J_1^{[t,i]}/J_1^{[t,o]}$ should have a factor of ρ . This explains why there is no dQ_0 -term in the leading order expansions of $J_1^{[t,i]}/J_1^{[t,o]}$ in formula (5.14) in Theorem 5.1.

For the case studied in Sect. 5.2, we are able to obtain an approximation for the flux ratio, up to leading orders, explicitly in terms of given quantities of the problem.

It follows from (3.1) in Proposition 3.1 that

$$\Big(\int_0^1 \frac{e^{p_1^{[i]}(x;z_1,d_1)}}{D_1(x)h(x)} dx\Big)^{-1} = \frac{J_1^{[i]}}{(L_1 + L_1^{[i,i]})e^{p_1^{[i]}(0;z_1,d_1)} - R_1e^{p_1^{[i]}(1;z_1,d_1)}},$$

where $J_1^{[i]} = J_1^{[m,i]} + J_1^{[i,i]}$ is the sum of the fluxes of the main ion species and its tracer. Similarly,

$$\int_0^1 \frac{e^{p_1^{[o]}(x;z_1,d_1)}}{D_1(x)h(x)} dx = \frac{L_1 e^{p_1^{[o]}(0;z_1,d_1)} - (R_1 + R_1^{[t,o]}) e^{p_1^{[o]}(1;z_1,d_1)}}{J_1^{[o]}},$$

where $J_1^{[o]} = J_1^{[m,o]} + J_1^{[t,o]}$ is the sum of the fluxes of the main ion species and its tracer. Therefore,

$$\frac{J_1^{[t,i]}}{J_1^{[t,o]}} = -(I) \cdot (II) \cdot \frac{J_1^{[i]}}{J_1^{[o]}}$$
(7.2)

where the factors (I) and (II) are given by

$$(I) = \frac{L_1^{[t,i]} e^{p_1^{[i]}(0;z_1,d_1)}}{R_1^{[t,o]} e^{p_1^{[o]}(1;z_1,d_1)}},$$

$$(II) = \frac{L_1 e^{p_1^{[o]}(0;z_1,d_1)} - (R_1 + R_1^{[t,o]}) e^{p_1^{[o]}(1;z_1,d_1)}}{(L_1 + L_1^{[t,i]}) e^{p_1^{[i]}(0;z_1,d_1)} - R_1 e^{p_1^{[i]}(1;z_1,d_1)}}.$$

$$(7.3)$$

The factors (I) and (II) on the right-hand side of (7.2) are determined by boundary conditions and are independent of the permanent charge. We will first determine these two factors and determine the last factor $J_1^{[i]}/J_1^{[o]}$ afterwards.

7.2 Derivation of Formula (5.14)

For this formula, the electroneutrality boundary conditions (5.13) are assumed to hold among all ion species including the tracer. It follows from (5.6) that, for the boundary condition associated to (BVi) in (5.13),

$$\begin{aligned} p_1^{[i]}(0; z_1, d_1) &= z_1 \zeta_0 V_0 + d \Big(2(L_1 + \rho) + (1 + \lambda)(L_2 - z_1 \rho / z_2) \Big) + O(d^2), \\ &= z_1 \zeta_0 V_0 + d \Big(2L_1 + (1 + \lambda)L_2 \Big) + O(d^2, d\rho), \\ p_1^{[i]}(1; z_1, d_1) &= d \Big(2R_1 + (1 + \lambda)R_2 \Big) + O(d^2); \end{aligned}$$

and, for the boundary condition associated to (BVo) in (5.13),

$$p_1^{[o]}(0; z_1, d_1) = z_1 \zeta_0 V_0 + d(2L_1 + (1+\lambda)L_2) + O(d^2),$$



$$p_1^{[o]}(1; z_1, d_1) = d(2(R_1 + \rho) + (1 + \lambda)(R_2 - z_1\rho/z_2)) + O(d^2)$$

= $d(2R_1 + (1 + \lambda)R_2) + O(d^2, d\rho)$.

Thus, the factor (I) on the right-hand side of (7.2) is

$$(I) = e^{p_1^{[i]}(0;z_1,d_1) - p_1^{[o]}(1,z_1,d_1)}$$

= $e^{z_1\zeta_0 V_0} \Big(1 + \Big(2(L_1 - R_1) + (1+\lambda)(L_2 - R_2) \Big) d \Big) + O(d^2, d\rho),$ (7.4)

and the factor (II) on the right-hand side of (7.2) is, with $s = L_1/R_1$,

$$(II) = \frac{L_1 e^{z_1 \zeta_0 V_0} - (R_1 + \rho) + \left[(2L_1^2 + (1 + \lambda)L_1 L_2) e^{z_1 \zeta_0 V_0} - (2R_1^2 + (1 + \lambda)R_1 R_2) \right] d}{(L_1 + \rho) e^{z_1 \zeta_0 V_0} - R_1 + \left[(2L_1^2 + (1 + \lambda)L_1 L_2) e^{z_1 \zeta_0 V_0} - (2R_1^2 + (1 + \lambda)R_1 R_2) \right] d} + O(\rho^2, \rho d, d^2)$$

$$= 1 - \frac{e^{z_1 \zeta_0 V_0} + 1}{s e^{z_1 \zeta_0 V_0} - 1} \frac{\rho}{R_1} + O(\rho^2, \rho d, d^2). \tag{7.5}$$

It remains to approximate the factor $J_1^{[i]}/J_1^{[o]}$ in (7.2) that depends on the permanent charge Q and hence the full profile of the electric potential and the ion concentrations. Its approximation is complicated even for the simple case we considered in Sect. 5. We start with a general expression

$$\frac{J_1^{[i]}}{J_1^{[\rho]}} = S_0(\rho) + S_1(\rho)d + S_2(\rho)Q_0 + O(d^2, \rho dQ_0, \rho Q_0^2),$$

and determine the quantities $S_k(\rho)$'s for k=0,1,2. In particular, we are interested in $S_0(\rho)$ up to $O(\rho)$ order, $S_1(\rho)=S_1(0)+O(\rho)$ due to the factor d in $S_1(\rho)d$, and $S_2(\rho)$ up to $O(\rho)$. The reason for the latter is, from Remark 7.1, any term involving Q_0 should have a factor ρ . The advantage of this expression is as follows. One can assume the ionic solution is ideal to get the term $S_0(\rho)+S_2(\rho)Q_0$ (Sect. 7.2.1) and then assume the ionic solution is nonideal but the permanent charge is zero to get $S_0(\rho)+S_1(\rho)d$ (Sect. 7.2.2). The superposition of them then provides the approximation for $J_1^{[i]}/J_1^{[o]}$.

7.2.1 Case with Ideal Ionic Solution for $S_0(\rho) + S_2(\rho)Q_0$

We will apply results from [51] for the classical PNP for this case.

It follows from results in [51] (displays (4.4) and (4.5) in [51]) that the influx of the tracer for the boundary concentrations in (BVi) is

$$J_1^{[i]} = J_{10}^{[i]} + J_{11}^{[i]} Q_0 + O(Q_0^2), \tag{7.6}$$

where

$$J_{10}^{[i]} = \frac{D_1(L_1 + \rho - R_1)}{H(1)(\ln(L_1 + \rho) - \ln R_1)} \frac{\mu_1^{\delta, i}}{k_B T},$$

$$J_{11}^{[i]} = \frac{D_1 A^{[i]}(z_2(1 - B^{[i]})\zeta_0 V_0 + \ln(L_1 + \rho) - \ln R_1)}{(z_1 - z_2)H(1)(\ln(L_1 + \rho) - \ln R_1)^2} \frac{\mu_1^{\delta, i}}{k_B T},$$
(7.7)

and

$$\frac{1}{k_B T} \mu_1^{\delta,i} := \frac{1}{k_B T} \left(\mu^{[i]}(0) - \mu^{[i]}(1) \right) = z_1 \zeta_0 V_0 + \ln(L_1 + \rho) - \ln R_1, \tag{7.8}$$

is the difference between the boundary electrochemical potentials for (BVi), and

$$A^{[i]} = -\frac{(\beta - \alpha)(L_1 + \rho - R_1)^2}{((1 - \alpha)(L_1 + \rho) + \alpha R_1)((1 - \beta)(L_1 + \rho) + \beta R_1) \ln \frac{L_1 + \rho}{R_1}},$$

$$B^{[i]} = \frac{1}{A^{[i]}} \ln \frac{(1 - \beta)(L_1 + \rho) + \beta R_1}{(1 - \alpha)(L_1 + \rho) + \alpha R_1}.$$
(7.9)

Similarly, the efflux of the tracer for the boundary concentrations in (BVo) is

$$J_1^{[o]} = J_{10}^{[o]} + J_{11}^{[o]} Q_0 + O(Q_0^2), (7.10)$$

where

$$J_{10}^{[o]} = \frac{D_1(L_1 - (R_1 + \rho))}{H(1)(\ln L_1 - \ln(R_1 + \rho))} \frac{\mu_1^{\delta, o}}{k_B T},$$

$$J_{11}^{[o]} = \frac{D_1 A^{[o]}(z_2(1 - B^{[o]})\zeta_0 V_0 + \ln L_1 - \ln(R_1 + \rho))}{(z_1 - z_2)H(1)(\ln L_1 - \ln(R_1 + \rho))^2} \frac{\mu_1^{\delta, o}}{k_B T},$$
(7.11)

and

$$\frac{1}{k_B T} \mu_1^{\delta,o} := \frac{1}{k_B T} \left(\mu^{[o]}(0) - \mu^{[o]}(1) \right) = z_1 \zeta_0 V_0 + \ln L_1 - \ln(R_1 + \rho) \tag{7.12}$$

is the differences between the boundary electrochemical potentials (BVo), and

$$A^{[o]} = -\frac{(\beta - \alpha)(L_1 - R_1 - \rho)^2}{((1 - \alpha)L_1 + \alpha(R_1 + \rho))((1 - \beta)L_1 + \beta(R_1 + \rho))\ln\frac{L_1}{R_1 + \rho}},$$

$$B^{[o]} = \frac{1}{A^{[o]}}\ln\frac{(1 - \beta)L_1 + \beta(R_1 + \rho)}{(1 - \alpha)L_1 + \alpha(R_1 + \rho)}.$$
(7.13)

Therefore,

$$\begin{split} \frac{J_{1}^{[i]}}{J_{1}^{[o]}} &= \frac{J_{10}^{[i]} + J_{11}^{[i]} Q_{0}}{J_{10}^{[o]} + J_{11}^{[o]} Q_{0}} + O(Q_{0}^{2}) \\ &= F_{0} \left(1 + \frac{F_{1}}{F_{0}} Q_{0} \right) + O(Q_{0}^{2}), \end{split}$$
(7.14)

where

$$F_{0} = \frac{J_{10}^{[i]}}{J_{10}^{[o]}} = \frac{L_{1} + \rho - R_{1}}{L_{1} - (R_{1} + \rho)} \frac{\ln L_{1} - \ln(R_{1} + \rho)}{\ln(L_{1} + \rho) - \ln R_{1}} \frac{\mu_{1}^{\delta, i}}{\mu_{1}^{\delta, o}},$$

$$\frac{F_{1}}{F_{0}} = \frac{J_{11}^{[i]}}{J_{10}^{[i]}} - \frac{J_{11}^{[o]}}{J_{10}^{[o]}} = \frac{A^{[i]} \left(z_{2}(1 - B^{[i]})\zeta_{0}V_{0} + \ln(L_{1} + \rho) - \ln R_{1}\right)}{(z_{1} - z_{2})(L_{1} + \rho - R_{1})\left(\ln(L_{1} + \rho) - \ln R_{1}\right)}$$

$$- \frac{A^{[o]} \left(z_{2}(1 - B^{[o]})\zeta_{0}V_{0} + \ln L_{1} - \ln(R_{1} + \rho)\right)}{(z_{1} - z_{2})(L_{1} - (R_{1} + \rho))\left(\ln L_{1} - \ln(R_{1} + \rho)\right)}.$$
(7.15)

Lemma 7.2 With $s = L_1/R_1$, one has

$$F_0 = 1 + \left(f_1(s) + \frac{s+1}{s(z_1 \zeta_0 V_0 + \ln s)}\right) \frac{\rho}{R_1} + O(\rho^2),$$



where $f_1(s)$ is defined in (5.8), and

$$\frac{F_1}{F_0} = g_1(V_0, s, \alpha, \beta) \frac{\rho}{R_1^2} + O(\rho^2),$$

where $g_1(V_0, s, \alpha, \beta)$ is given in (5.9). As a consequence,

$$S_0(\rho) = 1 + \left(f_1(s) + \frac{s+1}{s(z_1\zeta_0V_0 + \ln s)}\right)\frac{\rho}{R_1} \quad and \quad S_2(\rho) = g_1(V_0, s, \alpha, \beta)\frac{\rho}{R_1^2}. \tag{7.16}$$

Proof For the term F_0 , it follows (7.15), (7.8) and (7.12) that

$$\begin{split} F_0 &= \frac{s-1+\frac{\rho}{R_1}}{s-1-\frac{\rho}{R_1}} \cdot \frac{\ln s - \ln(1+\frac{\rho}{R_1})}{\ln s + \ln(1+\frac{\rho}{sR_1})} \frac{z_1 \zeta_0 V_0 + \ln(s+\frac{\rho}{R_1})}{z_1 \zeta_0 V_0 + \ln s - \ln(1+\frac{\rho}{R_1})}, \\ &= 1 + \left(\frac{2s \ln s - s^2 + 1}{s(s-1) \ln s} + \frac{s+1}{s(z_1 \zeta_0 V_0 + \ln s)}\right) \frac{\rho}{R_1} + O(\rho^2), \end{split}$$

which is the claimed formula for F_0 .

The approximate formula for F_1/F_0 is lengthy but otherwise straightforward.

With $s = L_1/R_1$ and $L_1^{[t,i]} = R_1^{[t,o]} = \rho$, it follows from (7.15) that

$$\begin{split} \frac{F_1}{F_0} &= \frac{z_2(A^{[i]} - A^{[i]}B^{[i]})\zeta_0V_0}{(z_1 - z_2)R_1(s - 1 + \rho/R_1)\left(\ln s + \rho/(sR_1)\right)} \\ &+ \frac{A^{[i]}}{(z_1 - z_2)R_1(s - 1 + \rho/R_1)} \\ &- \frac{z_2(A^{[o]} - A^{[o]}B^{[o]})\zeta_0V_0}{(z_1 - z_2)R_1(s - 1 - \rho/R_1)\left(\ln s - \rho/R_1\right)} \\ &- \frac{A^{[o]}}{(z_1 - z_2)R_1(s - 1 - \rho/R_1)} + O(\rho^2). \end{split}$$

Next, we fix $A^{[i]}$, $B^{[i]}$, $A^{[o]}$ and $B^{[o]}$, and expand the above in ρ to get

$$\begin{split} \frac{F_1}{F_0} &= \frac{z_2 \zeta_0 V_0 (A^{[i]} - A^{[i]} B^{[i]} - A^{[o]} + A^{[o]} B^{[o]})}{(z_1 - z_2) R_1 (s - 1) \ln s} \\ &\quad + \frac{(s - 1) (A^{[i]} - A^{[o]})}{(z_1 - z_2) R_1 (s - 1)^2} \\ &\quad - \frac{z_2 \zeta_0 V_0 [(A^{[i]} - A^{[i]} B^{[i]}) (\ln s + 1 - 1/s) + (A^{[o]} - A^{[o]} B^{[o]}) (\ln s + s - 1)]}{(z_1 - z_2) (s - 1)^2 (\ln s)^2} \frac{\rho}{R_1^2} \\ &\quad - \frac{A^{[i]} + A^{[o]}}{(z_1 - z_2) (s - 1)^2} \frac{\rho}{R_1^2} + O(\rho^2). \end{split}$$

Now, we expand $A^{[i]}$, $A^{[o]}$, $B^{[i]}$ and $B^{[o]}$ defined in (7.9) and (7.13) in ρ as

$$\begin{split} A^{[i]} &= A_0^{[i]} + A_1^{[i]} \frac{\rho}{R_1} + O(\rho^2), \\ A^{[o]} &= A_0^{[o]} + A_1^{[o]} \frac{\rho}{R_1} + O(\rho^2), \\ A^{[i]} B^{[i]} &= (A^{[i]} B^{[i]})_0 + (A^{[i]} B^{[i]})_1 \frac{\rho}{R_1} + O(\rho^2), \end{split}$$

$$A^{[o]}B^{[o]} = (A^{[o]}B^{[o]})_0 + (A^{[o]}B^{[o]})_1 \frac{\rho}{R_1} + O(\rho^2).$$

It follows directly that

$$A_{0}^{[i]} = A_{0}^{[o]} = -(\beta - \alpha) \frac{(s - 1)^{2}}{[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta] \ln s},$$

$$A_{1}^{[i]} = -(\beta - \alpha) \frac{2(s - 1)}{[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta] \ln s}$$

$$+ (\beta - \alpha) \frac{(s - 1)^{2}[2(1 - \alpha)(1 - \beta)s + \alpha + \beta - 2\alpha\beta]}{[(1 - \alpha)s + \alpha]^{2}[(1 - \beta)s + \beta]^{2} \ln s}$$

$$+ (\beta - \alpha) \frac{(s - 1)^{2}}{[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta]s(\ln s)^{2}},$$

$$A_{1}^{[o]} = (\beta - \alpha) \frac{2(s - 1)}{[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta] \ln s}$$

$$+ (\beta - \alpha) \frac{(s - 1)^{2}[(\alpha + \beta - 2\alpha\beta)s + 2\alpha\beta]}{[(1 - \alpha)s + \alpha]^{2}[(1 - \beta)s + \beta]^{2} \ln s}$$

$$- (\beta - \alpha) \frac{(s - 1)^{2}}{[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta](\ln s)^{2}},$$

$$(A^{[i]}B^{[i]})_{0} = (A^{[o]}B^{[o]})_{0} = \ln \frac{(1 - \beta)s + \beta}{(1 - \alpha)s + \alpha},$$

$$(A^{[i]}B^{[i]})_{1} = \frac{1 - \beta}{(1 - \beta)s + \beta} - \frac{\alpha}{(1 - \alpha)s + \alpha},$$

$$(A^{[o]}B^{[o]})_{1} = \frac{\beta}{(1 - \beta)s + \beta} - \frac{\alpha}{(1 - \alpha)s + \alpha}.$$

In particular,

$$\begin{split} A_0^{[i]} - A_0^{[o]} &= 0, \quad (A^{[i]}B^{[i]})_0 - (A^{[o]}B^{[o]})_0 = 0, \\ A_0^{[i]} - (A^{[i]}B^{[i]})_0 &= -\frac{(\beta - \alpha)(s - 1)^2}{[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta] \ln s} - \ln\frac{(1 - \beta)s + \beta}{(1 - \alpha)s + \alpha}, \\ A_1^{[i]} - A_1^{[o]} &= -\frac{4(\beta - \alpha)(s - 1)}{[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta] \ln s} \\ &\quad + \frac{(\beta - \alpha)(s - 1)^2[(2 - 3\alpha - 3\beta + 4\alpha\beta)s + \alpha + \beta - 4\alpha\beta]}{[(1 - \alpha)s + \alpha]^2[(1 - \beta)s + \beta]^2 \ln s} \\ &\quad + \frac{(\beta - \alpha)(s + 1)(s - 1)^2}{[(1 - \alpha)s + \alpha][(1 - \beta)s + \beta]s(\ln s)^2}, \\ (A^{[i]}B^{[i]})_1 - (A^{[o]}B^{[o]})_1 &= \frac{1 - 2\beta}{(1 - \beta)s + \beta} - \frac{1 - 2\alpha}{(1 - \alpha)s + \alpha}. \end{split}$$

Combining the above estimates, one has

$$\begin{split} \frac{F_1}{F_0} &= -\frac{4(\beta-\alpha)z_2\zeta_0V_0}{(z_1-z_2)[(1-\alpha)s+\alpha][(1-\beta)s+\beta](\ln s)^2}\frac{\rho}{(R_1)^2} \\ &+ \frac{(\beta-\alpha)z_2\zeta_0V_0(s-1)[(2-3\alpha-3\beta+4\alpha\beta)s+\alpha+\beta-4\alpha\beta]}{(z_1-z_2)[(1-\alpha)s+\alpha]^2[(1-\beta)s+\beta]^2(\ln s)^2}\frac{\rho}{(R_1)^2} \\ &+ \frac{(\beta-\alpha)z_2\zeta_0V_0(s+1)(s-1)}{(z_1-z_2)[(1-\alpha)s+\alpha][(1-\beta)s+\beta]s(\ln s)^3}\frac{\rho}{(R_1)^2} \end{split}$$



$$\begin{split} &-\frac{z_2\zeta_0V_0}{(z_1-z_2)(s-1)\ln s}\bigg[\frac{1-2\beta}{(1-\beta)s+\beta}-\frac{1-2\alpha}{(1-\alpha)s+\alpha}\bigg]\frac{\rho}{(R_1)^2} \\ &+\frac{(\beta-\alpha)z_2\zeta_0V_0(2\ln s+s-1/s)}{(z_1-z_2)[(1-\alpha)s+\alpha][(1-\beta)s+\beta](\ln s)^3}\frac{\rho}{(R_1)^2} \\ &+\frac{z_2\zeta_0V_0(2\ln s+s-1/s)}{(z_1-z_2)(s-1)^2(\ln s)^2}\ln\frac{(1-\beta)s+\beta}{(1-\alpha)s+\alpha}\frac{\rho}{(R_1)^2} \\ &-\frac{(\beta-\alpha)[(\alpha+\beta-2\alpha\beta)(s-1)^2+2s]}{(z_1-z_2)[(1-\alpha)s+\alpha]^2[(1-\beta)s+\beta]^2\ln s}\frac{\rho}{(R_1)^2} \\ &+\frac{(\beta-\alpha)(s+1)(s-1)}{(z_1-z_2)[(1-\alpha)s+\alpha][(1-\beta)s+\beta]s(\ln s)^2}\frac{\rho}{(R_1)^2}+O(\rho^2). \end{split}$$

The fifth term above can be split and combine with the first and the third terms to get the formula for F_1/F_0 claimed in the statement of the lemma.

7.2.2 A Case with a Hard-Sphere Component for $S_0(\rho) + S_1(\rho)d$

In this section, we examine the flux ratio for PNP models with a hard-sphere component (point-charge with volume exclusion) and assume zero permanent charge.

Recall the local hard-sphere potential (5.5)

$$\frac{1}{k_B T} \mu_k^{LHS}(x) = -\ln\left(1 - \sum_{j=1}^n d_j c_j(x)\right) + \frac{d_k \sum_{j=1}^n c_j(x)}{1 - \sum_{j=1}^n d_j c_j(x)}$$
$$= \sum_{j=1}^n (d_j + d_k) c_j(x) + O(d_k d_j)$$

where d_j is the diameter of the jth ion species.

For two ion species with diameters d_1 and d_2 , set $d = d_1$ and $d_2 = \lambda d$, and expand the fluxes as $J_k = J_{k0} + J_{k1}d + O(d^2)$, k = 1, 2. As observed in [29], the Nernst-Planck equations imply that the flux J_i is proportional to the transmembrane electrochemical potential $\mu_i^{\delta} = \mu_i(0) - \mu_i(1)$ where

$$\frac{1}{k_B T} \mu_1^{\delta} = z_1 \zeta_0 V_0 + \ln L_1 - \ln R_1
+ \frac{2z_2 - (1 + \lambda)z_1}{z_2} (L_1 - R_1)d + O(d^2),
\frac{1}{k_B T} \mu_2^{\delta} = z_2 \zeta_0 V_0 + \ln L_2 - \ln R_2
- \frac{(1 + \lambda)z_2 - 2\lambda z_1}{z_1} (L_2 - R_2)d + O(d^2).$$
(7.18)

It follows from results in [50,54], for example, from Corollary 3.6 in [54] (with different but equivalent expressions) that the flux $J_1^{[i]}$ is given by

$$J_1^{[i]} = \left(1 + \frac{2(\lambda z_1 - z_2)}{z_1 z_2} w_1^{[i]} d\right) \frac{D_1 w_0^{[i]}}{z_1 H(1)} \frac{\mu_1^{\delta, i}}{k_B T} + O(d^2),$$

where, with $\rho = L_1^{[t,i]} = R_1^{[t,o]}$,

$$\frac{1}{k_B T} \mu_1^{\delta, i} = z_1 \zeta_0 V_0 + \ln(L_1 + \rho) - \ln R_1$$



$$+\frac{2z_2-(1+\lambda)z_1}{z_2}(L_1+\rho-R_1)d+O(d^2)$$

is the difference between the boundary electrochemical potentials for (BVi), and

$$\begin{split} w_0^{[i]} &= \frac{z_1(L_1 + \rho - R_1)}{\ln(L_1 + \rho) - \ln R_1} \text{ and } \\ w_1^{[i]} &= \frac{z_1(L_1 + \rho - R_1)}{\ln(L_1 + \rho) - \ln R_1} - \frac{z_1(L_1 + \rho + R_1)}{2}. \end{split}$$

Similarly, the flux $J_1^{[o]}$ is given by

$$J_1^{[o]} = \left(1 + \frac{2(\lambda z_1 - z_2)}{z_1 z_2} w_1^{[o]} d\right) \frac{D_1 w_0^{[o]}}{z_1 H(1)} \frac{\mu_1^{\delta, o}}{k_B T} + O(d^2),$$

where

$$\begin{split} \frac{1}{k_B T} \mu_1^{\delta,o} &= z_1 \zeta_0 V_0 + \ln L_1 - \ln(R_1 + \rho) \\ &+ \frac{2z_2 - (1+\lambda)z_1}{z_2} (L_1 - R_1 - \rho)d + O(d^2) \end{split}$$

is the difference between the boundary electrochemical potentials for (BVo), and

$$\begin{split} w_0^{[o]} &= \frac{z_1(L_1 - R_1 - \rho)}{\ln L_1 - \ln(R_1 + \rho)} \text{ and } \\ w_1^{[o]} &= \frac{z_1(L_1 - R_1 - \rho)}{\ln L_1 - \ln(R_1 + \rho)} - \frac{z_1(L_1 + R_1 + \rho)}{2}. \end{split}$$

Recall that $s = L_1/R_1$. One gets

$$\begin{split} \frac{1}{k_B T} \mu_1^{\delta,i} &= z_1 \zeta_0 V_0 + \ln s + \frac{\rho}{s R_1} + \frac{2z_2 - (1+\lambda)z_1}{z_2} (s-1) R_1 d + O(\rho d, d^2), \\ w_0^{[i]} &= \frac{s-1}{\ln s} z_1 R_1 + \frac{s \ln s - (s-1)}{s (\ln s)^2} z_1 \rho + O(\rho^2), \\ w_1^{[i]} &= \frac{s-1}{\ln s} z_1 R_1 - \frac{s+1}{2} z_1 R_1 + \left(\frac{s \ln s - (s-1)}{s (\ln s)^2} - \frac{1}{2} \right) z_1 \rho + O(\rho^2); \\ \frac{1}{k_B T} \mu_1^{\delta,o} &= z_1 \zeta_0 V_0 + \ln s - \frac{\rho}{R_1} + \frac{2z_2 - (1+\lambda)z_1}{z_2} (s-1) R_1 d + O(\rho d, d^2), \\ w_0^{[o]} &= \frac{s-1}{\ln s} z_1 R_1 + \frac{s-1 - \ln s}{(\ln s)^2} z_1 \rho + O(\rho^2), \\ w_1^{[o]} &= \frac{s-1}{\ln s} z_1 R_1 - \frac{s+1}{2} z_1 R_1 + \left(\frac{s-1 - \ln s}{(\ln s)^2} - \frac{1}{2} \right) z_1 \rho + O(\rho^2). \end{split}$$

Thus,

$$\begin{split} \frac{\mu_1^{\delta,i}}{\mu_1^{\delta,o}} &= 1 + \frac{s+1}{s(z_1 \zeta_0 V_0 + \ln s)} \frac{\rho}{R_1} + O(\rho^2, \rho d, d^2), \\ \frac{w_0^{[i]}}{w_0^{[o]}} &= 1 + \frac{2s \ln s - s^2 + 1}{s(s-1) \ln s} \frac{\rho}{R_1} + O(\rho^2), \\ w_1^{[i]} - w_1^{[o]} &= \frac{2s \ln s - s^2 + 1}{s(\ln s)^2} z_1 \rho + O(\rho^2). \end{split}$$



Therefore, the ratio between the fluxes $J_1^{[i]}$ and $J_1^{[o]}$ is given by

$$\begin{split} \frac{J_1^{[i]}}{J_1^{[o]}} &= \frac{z_1 z_2 + 2(\lambda z_1 - z_2) w_1^{[i]} d}{z_1 z_2 + 2(\lambda z_1 - z_2) w_1^{[o]} d} \cdot \frac{w_0^{[i]}}{w_0^{[o]}} \frac{\mu_1^{\delta, i}}{\mu_1^{\delta, o}} + O(d^2) \\ &= \left(1 + \frac{2(\lambda z_1 - z_2)}{z_1 z_2} (w_1^{[i]} - w_1^{[o]}) d\right) \frac{w_0^{[i]}}{w_0^{[o]}} \frac{\mu_1^{\delta, i}}{\mu_1^{\delta, o}} + O(d^2) \\ &= 1 + \left(\frac{2s \ln s - s^2 + 1}{s(s - 1) \ln s} + \frac{s + 1}{t(z_1 \zeta_0 V_0 + \ln s)}\right) \frac{\rho}{R_1} + O(\rho^2, \rho d, d^2). \end{split}$$

As a consequence,

$$S_0(\rho) = 1 + \left(\frac{2s\ln s - s^2 + 1}{s(s-1)\ln s} + \frac{s+1}{s(z_1\zeta_0V_0 + \ln s)}\right)\frac{\rho}{R_1} \text{ and } S_1(0) = 0.$$
 (7.19)

Note that $S_0(\rho)$ obtained here agrees with that in (7.16), as expected. The conclusion $S_1(0) =$ 0 implies that there is not linear term in d in the approximation for $J_1^{[i]}/J_1^{[o]}$.

7.2.3 Approximation of $J_1^{[i]}/J_1^{[o]}$

The superposition of (7.16) and (7.19) then gives

$$\frac{J_1^{[i]}}{J_1^{[o]}} = 1 + \left(\frac{2s\ln s - s^2 + 1}{s(s-1)\ln s} + \frac{s+1}{s(z_1\zeta_0V_0 + \ln s)}\right)\frac{\rho}{R_1} + g_1(V_0, s, \alpha, \beta)\frac{\rho Q_0}{R_1^2} + O(\rho^2, d^2, \rho dQ_0).$$
(7.20)

Finally, formula (5.14) in Theorem 5.1 can be obtained from the formula (7.2) by multiplying the three factors estimated in (7.4), (7.5) and (7.20).

7.3 Derivation of Formula (5.18)

We now derive formula (5.18) for the case where approximate electroneutrality boundary conditions are assumed; that is, we assume the boundary concentrations L_1 and R_1 for the main ion species and those L_2 and R_2 for the counterion species stay the same when tracer is added. Therefore, the electroneutrality boundary conditions are only approximate with the tracer concentration ρ being small. In this approximate electroneutrality boundary conditions, there will be boundary layers to compensate the imperfect electroneutrality.

More precisely, for (BVi) with tracer concentrations $c_1^{[t,i]}(0)=L_1^{[t,i]}=\rho>0$ at x=0 and $c_1^{[t,i]}(1)=R_1^{[t,i]}=0$ at x=1, one has

(BVi):
$$z_1(L_1 + \rho) + z_2L_2 = z_1\rho \approx 0$$
 and $z_1R_1 + z_2R_2 = 0$,

and there will be one boundary layer at x = 0.

For (BVo) with tracer concentrations $c_1^{[t,o]}(0) = L_1^{[t,o]} = 0$ at x = 0 and $c_1^{[t,o]}(1) = 0$ $R_1^{[t,o]} = \rho > 0$ at x = 1, one has

(BVo):
$$z_1L_1 + z_2L_2 = 0$$
 and $z_1(R_1 + \rho) + z_2R_2 = z_1\rho \approx 0$,

and there will be one boundary layer at x = 1.



For (BVi), let $(\phi_{\infty}^{[i]}, c_{1,\infty}^{[i]}, c_{1,\infty}^{[i,i]}, c_{2,\infty}^{[i]})$ be the corresponding values of $(\phi^{[i]}, c_1^{[i]}, c_1^{[i]}, c_2^{[i]})$ at the limiting point of the boundary layer at x=0. Then, it follows from [56] (Lemma 3.2 and Proposition 3.3 in [56]) and (5.17) that

$$\begin{split} \phi_{\infty}^{[i]} &= V_0 - \frac{1}{\zeta_0(z_1 - z_2)} \ln \frac{-z_2 L_2}{z_1(L_1 + \rho)} = V_0 + \frac{1}{\zeta_0(z_1 - z_2)} \frac{\rho}{L_1} + O(\rho^2), \\ c_{1,\infty}^{[i]} &= L_1 \left(\frac{L_1}{L_1 + \rho} \right)^{\frac{z_1}{z_1 - z_2}} = L_1 - \frac{z_1}{z_1 - z_2} \rho + O(\rho)^2, \\ c_{1,\infty}^{[i,i]} &= \rho \left(\frac{L_1}{L_1 + \rho} \right)^{\frac{z_1}{z_1 - z_2}} = \rho - \frac{z_1}{z_1 - z_2} \frac{\rho^2}{L_1} + O(\rho)^3 \\ c_{2,\infty}^{[i]} &= L_2 \left(\frac{L_1}{L_1 + \rho} \right)^{\frac{z_2}{z_1 - z_2}} = L_2 - \frac{z_1 L_2}{(z_1 - z_2) L_1} \rho + O(\rho)^2. \end{split}$$
(7.21)

It is easy to check that $z_1(c_{1,\infty}^{[i]}+c_{1,\infty}^{[i,i]})+z_2c_{2,\infty}^{[i]}=0$, which is known to be true for the limiting point [56].

Similarly, for (BVo), let $(\phi_{\infty}^{[o]}, c_{1,\infty}^{[o]}, c_{2,\infty}^{[o]}, c_{2,\infty}^{[o]})$ be the corresponding values of $(\phi^{[o]}, c_1^{[o]}, c_1^{[o]}, c_1^{[o]})$ at the limiting point of the boundary layer at x = 1. Then,

$$\phi_{\infty}^{[o]} = -\frac{1}{\zeta_{0}(z_{1} - z_{2})} \ln \frac{-z_{2}R_{2}}{z_{1}(R_{1} + \rho)} = \frac{1}{\zeta_{0}(z_{1} - z_{2})} \frac{\rho}{R_{1}} + O(\rho^{2}),$$

$$c_{1,\infty}^{[o]} = R_{1} \left(\frac{R_{1}}{R_{1} + \rho}\right)^{\frac{z_{1}}{z_{1} - z_{2}}} = R_{1} - \frac{z_{1}}{z_{1} - z_{2}} \rho + O(\rho)^{2},$$

$$c_{1,\infty}^{[t,o]} = \rho \left(\frac{R_{1}}{R_{1} + \rho}\right)^{\frac{z_{1}}{z_{1} - z_{2}}} = \rho - \frac{z_{1}}{z_{1} - z_{2}} \frac{\rho^{2}}{R_{1}} + O(\rho)^{3},$$

$$c_{2,\infty}^{[o]} = R_{2} \left(\frac{R_{1}}{R_{1} + \rho}\right)^{\frac{z_{2}}{z_{1} - z_{2}}} = R_{2} - \frac{z_{1}R_{2}}{(z_{1} - z_{2})R_{1}} \rho + O(\rho)^{2}.$$

$$(7.22)$$

One can derive the formula (5.18) following exactly the same procedure as in Sect. 7.2. Another approach is to make use of the derivation in Sect. 7.2 with necessary modifications. We have used both approaches and, not surprisingly, got the same approximate formula (5.18). The latter is simpler and is presented below.

More precisely, we need some modifications in the derivation in Sect. 7.2.

For (BVi), the boundary conditions should be replaced by

$$(\phi_{\infty}^{[i]},c_{1,\infty}^{[i]},c_{1,\infty}^{[t,i]},c_{2,\infty}^{[i]}) \ \ \text{at} \ \ x=0; \quad (0,R_1,0,R_2) \ \ \text{at} \ \ x=1.$$

For (BVo), the boundary conditions should be replaced by

$$(V_0, L_1, 0, L_2)$$
 at $x = 0$; $(\phi_{\infty}^{[o]}, c_{1,\infty}^{[o]}, c_{1,\infty}^{[t,o]}, c_{2,\infty}^{[o]})$ at $x = 1$.

With these modifications, it is not hard to get, from (5.6) that, for the boundary condition associated to (BVi) in (5.17),

$$\begin{split} p_1^{[i]}(0^+;z_1,d_1) &= z_1 \zeta_0 \phi_\infty^{[i]} + d \left(2(c_{1,\infty}^{[i]} + c_{1,\infty}^{[t,i]}) + (1+\lambda) c_{2,\infty}^{[i]} \right) + O(d^2) \\ &= z_1 \zeta_0 V_0 + \frac{z_1}{z_1 - z_2} \frac{\rho}{L_1} + d \left(2L_1 + (1+\lambda)L_2 \right) + O(d^2,d\rho), \\ p_1^{[i]}(1;z_1,d_1) &= d \left(2R_1 + (1+\lambda)R_2 \right) + O(d^2); \end{split}$$



and, for the boundary condition associated to (BVo) in (5.17),

$$\begin{split} p_1^{[o]}(0;z_1,d_1) &= z_1 \zeta_0 V_0 + d(2L_1 + (1+\lambda)L_2) + O(d^2), \\ p_1^{[o]}(1^-;z_1,d_1) &= z_1 \zeta_0 \phi_{\infty}^{[o]} + d(2(c_{1,\infty}^{[o]} + c_{1,\infty}^{[t,o]}) + (1+\lambda)c_{2,\infty}^{[o]}) + O(d^2) \\ &= \frac{z_1}{z_1 - z_2} \frac{\rho}{R_1} + d(2R_1 + (1+\lambda)R_2) + O(d^2,d\rho). \end{split}$$

Thus, it follows from the definitions of the factors in (7.2) that

$$(I) = \frac{c_{1,\infty}^{[t,i]}}{c_{1,\infty}^{[t,o]}} \left(e^{p_1^{[i]}(0;z_1,d_1) - p_1^{[o]}(1^-;z_1,d_1)} \right) = \left(1 + \frac{z_1(s-1)}{(z_1 - z_2)s} \frac{\rho}{R_1} \right) e^{z_1 \zeta_0 V_0}$$

$$\times \left(1 + \frac{z_1(1-s)}{(z_1 - z_2)s} \frac{\rho}{R_1} + \left(2(L_1 - R_1) + (1+\lambda)(L_2 - R_2) \right) d \right)$$

$$+ O(d^2, d\rho, \rho^2)$$

$$= e^{z_1 \zeta_0 V_0} \left(1 + \left(2(L_1 - R_1) + (1+\lambda)(L_2 - R_2) \right) d \right) + O(d^2, d\rho, \rho^2),$$

$$(7.23)$$

and

$$(II) = \frac{L_1 e^{p_1^{[o]}(0; z_1, d_1)} - (c_{1,\infty}^{[o]} + c_{1,\infty}^{[t,o]}) e^{p_1^{[o]}(1^-; z_1, d_1)}}{(c_{1,\infty}^{[i]} + c_{1,\infty}^{[t,i]}) e^{p_1^{[i]}(0^+; z_1, d_1)} - R_1 e^{p_1^{[i]}(1; z_1, d_1)}} + O(\rho^2, \rho d, d^2)$$

$$= 1 - \frac{e^{z_1 \zeta_0 V_0} + 1}{s e^{z_1 \zeta_0 V_0} - 1} \frac{\rho}{R_1} + O(\rho^2, \rho d, d^2).$$
(7.24)

Also, F_0 in (7.15) should be replaced by

$$\begin{split} F_0 &= \frac{c_{1,\infty}^{[i]} + c_{1,\infty}^{[t,i]} - R_1}{L_1 - (c_{1,\infty}^{[o]} + c_{1,\infty}^{[t,o]})} \frac{\ln L_1 - \ln(c_{1,\infty}^{[o]} + c_{1,\infty}^{[t,o]})}{\ln(c_{1,\infty}^{[i]} + c_{1,\infty}^{[t,i]}) - \ln R_1} \\ &\times \frac{z_1 \zeta_0 \phi_{\infty}^{[i]} + \ln(c_{1,\infty}^{[i]} + c_{1,\infty}^{[t,i]}) - \ln R_1}{z_1 \zeta_0 \phi_{\infty}^{[o]} + \ln L_1 - \ln(c_{1,\infty}^{[o]} + c_{1,\infty}^{[t,o]})}. \end{split}$$

A straightforward calculations gives

$$F_0 = 1 + \left(\frac{-z_2}{z_1 - z_2} f_1(s) + \frac{s+1}{s(z_1 \zeta_0 V_0 + \ln s)}\right) \frac{\rho}{R_1} + O(\rho^2),$$

where $f_1(s)$ is defined in (5.8).

The most complicate term is F_0/F_1 in (7.15). By a close examination of the terms involved in the expression, the following modifications are needed. One is to replace ρ with $-z_2\rho/(z_1-z_2)$. The other is, in the last expression of F_0/F_1 in (7.15), to replace V_0 by $\phi_{\infty}^{[i]}$ in the first term and to replace V_0 by $V_0-\phi_{\infty}^{[o]}$ in the second term. The combined effect of the latter is the extra term

$$\begin{split} (E) = & \frac{A^{[i]}(1-B^{[i]})}{(z_1-z_2)\left(L_1-\frac{z_2}{z_1-z_2}\rho-R_1\right)\left(\ln(L_1-\frac{z_2}{z_1-z_2}\rho)-\ln R_1\right)} \frac{z_2}{z_1-z_2} \frac{\rho}{sR_1} \\ & + \frac{A^{[o]}(1-B^{[o]})}{(z_1-z_2)\left(L_1-R_1+\frac{z_2}{z_1-z_2}\rho\right)\left(\ln L_1-\ln(R_1-\frac{z_2}{z_1-z_2}\rho)\right)} \frac{z_2}{z_1-z_2} \frac{\rho}{R_1} \end{split}$$



$$=\frac{z_2}{(z_1-z_2)^2}\frac{A_0^{[i]}+A_0^{[0]}s}{s(s-1)\ln s}\frac{\rho}{R_1^2}-\frac{z_2}{(z_1-z_2)^2}\frac{A_0^{[i]}B_0^{[i]}+A_0^{[0]}B_0^{[0]}s}{s(s-1)\ln s}\frac{\rho}{R_1^2}.$$

Using the expressions of $A_0^{[i]}$, $A_0^{[0]}$, $A_0^{[i]}B_0^{[i]}$ and $A_0^{[0]}B_0^{[0]}$ in (7.17), one gets

$$(E) = g_2(s, \alpha, \beta) \frac{-z_2}{z_1 - z_2} \frac{\rho}{R_1^2},$$

where $g_2(s, \alpha, \beta)$ is given in (5.9). Therefore, we have

$$\begin{split} \frac{F_1}{F_0} &= \frac{-z_2}{z_1 - z_2} g_1(V_0, s, \alpha, \beta) \frac{\rho}{R_1^2} + (E) \\ &= \frac{-z_2}{z_1 - z_2} \left(g_1(V_0, s, \alpha, \beta) + g_2(s, \alpha, \beta) \right) \frac{\rho}{R_1^2} + O(\rho^2), \end{split}$$

and hence,

$$\frac{J_1^{[i]}}{J_1^{[o]}} = F_0 \left(1 + \frac{F_1}{F_0} Q_0 \right) = 1
+ \left(\frac{-z_2}{z_1 - z_2} f_1(s) + \frac{s+1}{s(z_1 \zeta_0 V_0 + \ln s)} \right) \frac{\rho}{R_1}
+ \left(g_1(V_0, s, \alpha, \beta) + g_2(s, \alpha, \beta) \right) \frac{-z_2}{z_1 - z_2} \frac{\rho Q_0}{R_1^2} + O(\rho^2, d^2, \rho d Q_0).$$
(7.25)

The formula (5.18) in Theorem 5.2 then follows from (7.2), and the estimates (7.23), (7.24) and (7.25).

References

- Abaid, N., Eisenberg, R.S., Liu, W.: Asymptotic expansions of I-V relations via a Poisson-Nernst-Planck system. SIAM J. Appl. Dyn. Syst. 7, 1507-1526 (2008)
- Barcilon, V.: Ion flow through narrow membrane channels: Part I. SIAM J. Appl. Math. 52, 1391–1404 (1992)
- Barcilon, V., Chen, D.-P., Eisenberg, R.S.: Ion flow through narrow membrane channels: Part II. SIAM J. Appl. Math. 52, 1405–1425 (1992)
- Barcilon, V., Chen, D.-P., Eisenberg, R.S., Jerome, J.W.: Qualitative properties of steady-state Poisson– Nernst–Planck systems: perturbation and simulation study. SIAM J. Appl. Math. 57, 631–648 (1997)
- Bass, L., Bracken, A., Hilden, J.: Flux ratio theorems for nonstationary membrane transport with temporary capture of tracer. J. Theor. Biol. 118, 327–338 (1988)
- Bass, L., McNabb, A.: Flux ratio theorems for nonlinear membrane transport under nonstationary conditions. J. Theor. Biol. 133, 185–191 (1988)
- Begenisich, T., Busath, D.: Sodium flux ratio in voltage-clamped squid giant axons. J Gen. Physiol. 77(5), 489–502 (1981)
- Benos, D.J., Hyde, B.A., Latorre, R.: Sodium flux ratio through the amiloride-sensitive entry pathway in frog skin. J. Gen. Physiol. 81, 667–685 (1993)
- 9. Boda, D., Busath, D., Eisenberg, B., Henderson, D., Nonner, W.: Monte Carlo simulations of ion selectivity in a biological Na⁺ channel: charge–space competition. Phys. Chem. Chem. Phys. **4**, 5154–5160 (2002)
- Boda, D., Busath, D.D., Henderson, D., Sokolowski, S.: Monte Carlo simulations of the mechanism of channel selectivity: the competition between volume exclusion and charge neutrality. J. Phys. Chem. B. 104, 8903–8910 (2000)
- Boda, D., Nonner, W., Valisko, M., Henderson, D., Eisenberg, B., Gillespie, D.: Steric selectivity in Na channels arising from protein polarization and mobile side chains. Biophys. J. 93, 1960–1980 (2007)
- Boda, D., Valisko, M., Eisenberg, B., Nonner, W., Henderson, D., Gillespie, D.: Effect of protein dielectric coefficient on the ionic selectivity of a calcium channel. J. Chem. Phys. 125, 034901(1-11) (2006)



- Boda, D., Valisko, M., Eisenberg, B., Nonner, W., Henderson, D., Gillespie, D.: The combined effect of pore radius and protein dielectric coefficient on the selectivity of a calcium channel. Phys. Rev. Lett. 98, 168102(1-4) (2007)
- Boda, D., Varga, T., Henderson, D., Busath, D., Nonner, W., Gillespie, D., Eisenberg, B.: Monte Carlo simulation study of a system with a dielectric boundary: application to calcium channel selectivity. Mol. Simul. 30, 89–96 (2004)
- Busath, D., Begenisich, T.: Unidirectional sodium and potassium fluxes through the sodium channel of squid giant axons. Biophys. J. 40, 41–49 (1982)
- Catterall, W.A.: Ion channel voltage sensors: structure, function, and pathophysiology. Neuron 67, 915– 928 (2010)
- Catterall, W.A.: Molecular properties of voltage-sensitive sodium channels. Annu. Rev. Biochem. 55, 953–985 (1986)
- Chen, X.H., Bezprozvanny, I., Tsien, R.W.: Molecular basis of proton block of L-type Ca²⁺ channels. J. Gen. Physiol. 108, 363–374 (1996)
- Crozier, P.S., Henderson, D., Rowley, R.L., Busath, D.D.: Model channel ion currents in NaCl-extended simple point charge water solution with applied-field molecular dynamics. Biophys. J. 81, 3077–3089 (2001)
- Crozier, P.S., Rowley, R.L., Holladay, N.B., Henderson, D., Busath, D.D.: Molecular dynamics simulation
 of continuous current flow through a model biological membrane channel. Phys. Rev. Lett. 86, 2467–2470
 (2001)
- Curtis, B.A., Eisenberg, R.S.: Calcium influx in contracting and paralyzed frog twitch muscle fibers. J. Gen. Physiol. 85, 383–408 (1985)
- Doyle, D.A., Cabral, J.M., Pfuetzner, R.A., Kuo, A., Gulbis, J.M., Cohen, S.L., Chait, B.T., MacKinnon, R.: The structure of the potassium channel: molecular basis of K⁺ conduction and selectivity. Science 280, 69–77 (1998)
- 23. Eisenberg, B.: Ionic interactions are everywhere. Physiology 28, 28–38 (2013)
- 24. Eisenberg, B.: Interacting ions in biophysics: real is not ideal. Biophys. J. 104, 1849–1866 (2013)
- Eisenberg, B.: Crowded charges in ion channels. In: Rice, S.A. (ed.) Advances in Chemical Physics, pp. 77–223. Wiley, New York (2011)
- 26. Eisenberg, B.: Proteins, channels, and crowded ions. Biophys. Chem. 100, 507-517 (2003)
- 27. Eisenberg, R.S.: From structure to function in open ionic channels, J. Membr. Biol. 171, 1–24 (1999)
- Eisenberg, B., Liu, W.: Poisson–Nernst–Planck systems for ion channels with permanent charges. SIAM J. Math. Anal. 38, 1932–1966 (2007)
- Eisenberg, B., Liu, W., Xu, H.: Reversal charge and reversal potential: case studies via classical Poisson– Nernst–Planck models. Nonlinearity 28, 103–128 (2015)
- 30. Favre, I., Moczydlowski, E., Schild, L.: On the structural basis for ionic selectivity among Na⁺, K⁺, and Ca²⁺ in the voltage-gated sodium channel. Biophys. J. **71**, 3110–3125 (1996)
- Gillespie, D.: A review of steric interactions of ions: why some theories succeed and others fail to account for ion size. Microfluid Nanofluidics 18, 717–738 (2015)
- 32. Gillespie, D.: A Singular Perturbation Analysis of the Poisson–Nernst–Planck System: Applications to Ionic Channels. Ph.D. Dissertation, Rush University at Chicago (1999)
- Gillespie, D., Nonner, W., Henderson, D., Eisenberg, R.S.: A physical mechanism for large-ion selectivity of ion channels. Phys. Chem. Chem. Phys. 4, 4763–4769 (2002)
- Gillespie, D., Nonner, W., Eisenberg, R.S.: Coupling Poisson–Nernst–Planck and density functional theory to calculate ion flux. J. Phys. Condens. Matter 14, 12129–12145 (2002)
- Gillespie, D., Nonner, W., Eisenberg, R.S.: Density functional theory of charged, hard-sphere fluids. Phys. Rev. E 68, 0313503(1-10) (2003)
- 36. Hille, B.: Ion Channels of Excitable Membranes, 3rd edn. Sinauer Associates Inc., Sunderland (2001)
- Hille, B.: Transport across cell membranes: carrier mechanisms, Chapter 2. In: Patton, H.D., Fuchs, A.F.,
 Hille, B., Scher, A.M., Steiner, R.D. (eds.) Textbook of Physiology. Philadelphia, Saunders 1, 24–47 (1989)
- 38. Hodgkin, A.L.: The ionic basis of electrical activity in nerve and muscle. Biol. Rev. 26, 339-409 (1951)
- Hodgkin, A.L.: Ionic movements and electrical activity in giant nerve fibres. Proc. R. Soc. Lond. Ser. B 148, 1–37 (1958)
- 40. Hodgkin, A.L., Huxley, A.F.: Currents carried by sodium and potassium ions through the membrane of the giant axon of Loligo. J. Physol. **116**, 449–472 (1952)
- Hodgkin, A.L., Huxley, A.F.: The components of membrane conductance in the giant axon of Loligo. J. Physiol. 116, 473–496 (1952)
- 42. Hodgkin, A.L., Huxley, A.F.: A quantitative description of membrane current and its application to conduction and excitation in nerve. J. Physiol. 117, 500–544 (1952)



- Hodgkin, A.L., Huxley, A., Katz, B.: Ionic currents underlying activity in the giant axon of the squid. Arch. Sci. Physiol. 3, 129–150 (1949)
- Hodgkin, A.L., Katz, B.: The effect of sodium ions on the electrical activity of the giant axon of the squid.
 Physiol. 108, 37–77 (1949)
- Hodgkin, A.L., Keynes, R.D.: The potassium permeability of a giant nerve fibre. J. Physiol. 128, 61–88 (1955)
- 46. Horowicz, P., Gage, P.W., Eisenberg, R.S.: The role of the electrochemical gradient in determining potassium fluxes in frog striated muscle. J. Gen. Physiol. **51**, 193s–203s (1968)
- 47. Im, W., Beglov, D., Roux, B.: Continuum solvation model: electrostatic forces from numerical solutions to the Poisson–Boltzmann equation. Comput. Phys. Commun. 111, 59–75 (1998)
- Im, W., Roux, B.: Ion permeation and selectivity of OmpF porin: a theoretical study based on molecular dynamics, Brownian dynamics, and continuum electrodiffusion theory. J. Mol. Biol. 322, 851–869 (2002)
- 49. Jackson, M.: Molecular and Cellular Biophysics. University Press, Cambridge (2006)
- Ji, S., Liu, W.: Poisson–Nernst–Planck systems for ion flow with density functional theory for hard-sphere potential: I–V relations and critical potentials. Part I: analysis. J. Dyn. Differ. Equ. 24, 955–983 (2012)
- Ji, S., Liu, W., Zhang, M.: Effects of (small) permanent charge and channel geometry on ionic flows via classical Poisson–Nernst–Planck models. SIAM J. Appl. Math. 75, 114–135 (2015)
- 52. Kedem, O., Essig, A.: Isotope flows and flux ratios in biological membranes. J. Gen. Physiol. **48**(6), 1047 (1965)
- Kurnikova, M.G., Coalson, R.D., Graf, P., Nitzan, A.: A lattice relaxation algorithm for 3D Poisson– Nernst–Planck theory with application to ion transport through the gramicidin A channel. Biophys. J. 76, 642–656 (1999)
- Lin, G., Liu, W., Yi, Y., Zhang, M.: Poisson–Nernst–Planck systems for ion flow with a local hard-sphere potential for ion sizes. SIAM J. Appl. Dyn. Syst. 12, 1613–1648 (2013)
- Liu, W.: Geometric singular perturbation approach to steady-state Poisson–Nernst–Planck systems. SIAM J. Appl. Math. 65, 754–766 (2005)
- Liu, W.: One-dimensional steady-state Poisson–Nernst–Planck systems for ion channels with multiple ion species. J. Differ. Equ. 246, 428–451 (2009)
- Liu, W., Wang, B.: Poisson–Nernst–Planck systems for narrow tubular-like membrane channels. J. Dyn. Diff. Equ. 22, 413–437 (2010)
- Liu, W., Tu, X., Zhang, M.: Poisson–Nernst–Planck systems for ion flow with density functional theory for hard-sphere potential: I–V relations and critical potentials. Part II: numerics. J. Dyn. Differ. Equ. 24, 985–1004 (2012)
- Liu, W., Xu, H.: A complete analysis of a classical Poisson–Nernst–Planck model for ionic flow. J. Differ. Equ. 258, 1192–1228 (2015)
- Long, S.B., Campbell, E.B., Mackinnon, R.: Crystal structure of a mammalian voltage-dependent Shaker family K⁺ channel. Science 309, 897–903 (2005)
- 61. Long, S.B., Tao, X., Campbell, E.B., MacKinnon, R.: Atomic structure of a voltage-dependent K⁺ channel in a lipid membrane-like environment. Nature **450**, 376–382 (2007)
- McNabb, A., Bass, L.: Flux-ratio theorems for nonlinear equations of generalized diffusion. IMA J. Appl. Math. 43, 1–9 (1989)
- McNabb, A., Bass, L.: Flux theorems for linear multicomponent diffusion. IMA J. Appl. Math. 44, 155–161 (1990)
- Nadler, B., Schuss, Z., Singer, A., Eisenberg, B.: Diffusion through protein channels: from molecular description to continuum equations. Nanotech 3, 439–442 (2003)
- Naranjo, D., Moldenhauer, H., Pincuntureo, M., Díaz-Franulic, I.: Pore size matters for potassium channel conductance. J. Gen. Physiol. 148, 277–291 (2016)
- Nonner, W., Eisenberg, B.: Electrodiffusion in ionic channels of biological membranes. J. Mol. Fluids 87, 149–162 (2000)
- Nonner, W., Eisenberg, R.S.: Ion permeation and glutamate residues linked by Poisson–Nernst–Planck theory in L-type Calcium channels. Biophys. J. 75, 1287–1305 (1998)
- Noskov, S.Y., Im, W., Roux, B.: Ion permeation through the z₁-hemolysin channel: theoretical studies based on Brownian dynamics and Poisson–Nernst–Planck electrodiffusion theory. Biophys. J. 87, 2299– 2309 (2004)
- 69. Noskov, S.Y., Roux, B.: Ion selectivity in potassium channels. Biophys. Chem. 124, 279–291 (2006)
- Park, J.-K., Jerome, J.W.: Qualitative properties of steady-state Poisson–Nernst–Planck systems: mathematical study. SIAM J. Appl. Math. 57, 609–630 (1997)
- Payandeh, J., Scheuer, T., Zheng, N., Catterall, W.A.: The crystal structure of a voltage-gated sodium channel. Nature 475, 353–358 (2011)



- Rakowski, R.F., Gadsby, D.C., De Weer, P.: Single ion occupancy and steady-state gating of Na channels in squid giant axon. J. Gen. Physiol. 119, 235–249 (2002)
- Rosenfeld, Y.: Free energy model for the inhomogeneous fluid mixtures: Yukawa-charged hard spheres, general interactions, and plasmas. J. Chem. Phys. 98, 8126–8148 (1993)
- Schuss, Z., Nadler, B., Eisenberg, R.S.: Derivation of Poisson and Nernst–Planck equations in a bath and channel from a molecular model. Phys. Rev. E 64, 1–14 (2001)
- Sun, L., Liu, W.: Boundary value problems of Poisson–Nernst–Planck systems with nonlocal excess potentials: a case study. J. Dyn. Differ. Equ. (2017). doi:10.1007/s10884-017-9578-2
- Teorell, T.: Membrane electrophoresis in relation to bio-electrical polarization effects. Arch. Sci. Physiol. 3, 205–218 (1949)
- 77. Tosteson, D.: Membrane Transport: People and Ideas. American Physiological Society, Bethesda (1989)
- Ussing, H.H.: The distinction by means of tracers between active transport and diffusion. Acta Physiol. Scand. 19, 43–56 (1949)
- Yang, J., Ellinor, P.T., Sather, W.A., Zhang, J.F., Tsien, R.W.: Molecular determinants of Ca²⁺ selectivity and ion permeation in L-type Ca²⁺ channels. Nature 366, 158–161 (1993)
- Ye, S., Li, Y., Jiang, Y.: Novel insights into K⁺ selectivity from high-resolution structures of an open K⁺ channel pore. Nat. Struct. Mol. Biol. 17, 1019–1023 (2010)
- Yue, L., Navarro, B., Ren, D., Ramos, A., Clapham, D.E.: The cation selectivity filter of the bacterial sodium channel, NaChBac. J. Gen. Physiol. 120, 845–853 (2002)

