

A Bubble Model for the Gating of K_v Channels

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Abstract

Voltage-gated K_v channels play fundamental roles in many biological processes, such as the generation of the action potential. The gating mechanism of K_v channels is characterized experimentally by single-channel recordings and ensemble properties of the channel currents. In this work, we propose a bubble model coupled with a Poisson-Nernst-Planck (PNP) system to capture the key characteristics, particularly the delay in the opening of channels. The coupled PNP system is solved numerically by a finite-difference method and the solution is compared with an analytical approximation. We hypothesize that the stochastic behaviour of the gating phenomenon is due to randomness of the bubble and channel sizes. The predicted ensemble average of the currents under various applied voltage across the channels is consistent with experimental observations, and the Cole-Moore delay is captured by varying the holding potential.

Keywords: voltage-gated channels, Poisson-Nernst-Planck system, bubble model, Cole-Moore delay

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1. Introduction

Voltage-gated ion channels play fundamental roles in many biological activities, such as signal generation and propagation in the nervous system, pacemaker activity in the heart, and coordination of contraction in skeletal muscle [1, 2, 3]. For example, the voltage-gated Na (Na_v) and K (K_v) channels are key players in the generation of action potential (AP) signals in the nervous system [4], cardiac and skeletal muscle. This rapid and transient change of membrane potential propagates long distances (meters) in the nervous system and muscle fibers as well. The opening and closing of ion channels as the voltage changes across the membrane determine the depolarization (positive change in potential) and repolarization (negative change of membrane potential) that form the propagating AP [5, 6, 7, 8].

The opening of ion channels follows the change in voltage with a delay and that delay is an important determinant of the conduction velocity. The conduction velocity helps determine how fast the nervous system can function. One of the objectives of the present work is to model the delay in the opening of single K_v channels as well as their ensemble properties. The delay in the opening of Na_v channels is particularly important in determining the conduction velocity of the action potential. Therefore, understanding the mechanism of delay is of great biological importance. It is not unreasonable to expect that the delay is set by a process that is optimized as much as possible within the constraints of physics, protein structure, and evolutionary history [9].

Hodgkin and Huxley (HH) provided an empirical model of the generation of AP in 1952 [10]. The conductances they used are ensemble averages of those from many channels. Understanding the molecular mechanisms that produce these conductances and the AP is one of the main goals of biophysics for the past seventy years. Recent advances in structural biology [11] and single-channel recording [12] have catalyzed our understanding of the physical mechanisms that produce these conductances. The ionic basis of selective conduction is now understood reasonably well for sodium channels [13, 14, 15, 16].

The opening and closing of voltage-dependent channels involves many steps [17, 18, 19]. Some of the steps in the voltage-dependent gating of K_v are now known in molecular and physical detail [20, 21, 22, 23, 24, 25, 26, 27, 28, 4, 29, 30, 31, 32]. The first step is the response of the voltage sensor to the voltage change, and significant progress has been made in understanding the

physics of that response. It is plausible [10] that the permeability changes depend on the presence of voltage sensors in the form of charged or dipole particles, as suggested earlier in a different form [7, 33]. The second step is the communication of the voltage sensor with the conduction pore of the channel. This was revealed experimentally in the single-channel ON-OFF currents (that occur at random intervals) measured by bilayer or patch-clamp experiments from one channel protein at a time [34, 35]. The development of patch-clamp experiments [36] was a breakthrough in the understanding of the gating mechanisms and provided experimental verification at high resolution of many studies and models.

In the patch-clamp experiments, the recordings of single K_v channels showed a delay of currents in response to a step voltage change. The ionic current was generated rapidly after the delay, and vanished when the channel closed suddenly [29, 30, 4, 37]. The recordings also showed that the delays varied in each ON-OFF experiment: the gating transitions are stochastic. The ensemble average has a smoother transient time course for the currents (or opening and closing of channels), which resembles the classical macroscopic currents (or voltage-dependent conductances) in the HH model.

The delay in opening was first studied in the inaugural issue of the *Biophysical Journal* [38] in the ensemble of channels. Cole and Moore were able to control the resting potential (i.e., their holding potential) present before the AP mechanism was turned on. The earlier work of Hodgkin and Huxley had not addressed this issue in detail because the actual resting potential of their squid nerve was substantially different from that used as a holding potential [39]. Hodgkin and Huxley chose to use nerve fibers with more positive resting potentials so their voltage clamp system could control the voltage throughout the nerve fiber, something not easy to do [40]. Cole and Moore found the delay in the response of the nerve fiber to a change in voltage was much larger when the initial potential (also called the holding potential) was more negative.

Given the importance of this delay (we call the Cole-Moore delay), it is striking that a molecular scale biophysical explanation has not been developed, as far as we know, until very recently [41]. Given the obvious evolutionary disadvantage of additional delay, it seems likely that whatever is responsible for the delay is an essential component of the ionic channels that create the AP. We expect the cause of the Cole-Moore delay to be found in many channel types where it has not been investigated in detail.

The amount of work on channel proteins that produce the AP has in-

creased spectacularly in the last decades. The most important single advance (from a biophysical point of view) is the ON-OFF properties of the single channels, that in ensemble produce the Cole-Moore delay. Many researchers have proposed that the ON-OFF property arises from the collapse of a bubble. When the single-channel current is zero, a region of the voltage sensor with low effective dielectric constant [26] acts as a hydrophobic gasket that excludes water and ions from that region of the protein, forming a dewetted region, which is known as a bubble. Direct evidence for the existence of bubbles is emerging as structural biologists exploit the magnificent capabilities of modern techniques of x-ray crystallography and cryoelectron microscopy [20, 42].

Various modeling efforts have been devoted to understanding the gating mechanisms of K_v channels [22]. In the early years, kinetic models (or called Markov models) were used for channel gating, by assuming the voltage sensor has multiple subunits which make transitions between different states [43, 44, 45]. Formally, such kinetic models have some similarity to Hodgkin and Huxley's, as the four n -gates in the HH model can be interpreted as four independent subunits that control the gating [4]. Such models have been able to predict some important features of the gating mechanism of K_v channels (e.g., Shaker channel) and to fit experimental data, but could not reveal much about the physics of the gating process. With the availability of more structural information about channels and advances in computing power, quantitative models using molecular dynamics (MD) have been developed in recent decades [46, 47, 2]. MD simulations incorporating physical laws and interactions of atoms provide insights into the movement of the voltage sensors, intermediate states, and closure of the pore (forming a dewetted region). However, the MD approach is limited by the timescale of the simulations, resolving events in the timescale of 10^{-15} s, and the total simulation length is orders of magnitude lower than the timespan (e.g., 10^{-3} s) of experimentally or biologically relevant processes. This makes it difficult to directly validate the MD results by using the macroscopic currents in experiments. To overcome these limitations, alternative multiscale or macroscopic models [48, 49, 31, 28] have been developed with reasonable approximations. Some models are based on the formulation of Brownian dynamics, where the voltage sensor is treated as a Brownian particle [21]. Brownian models are able to predict macroscopic gating currents, where the free parameters involved have been estimated based on multiscale modeling approaches [26].

Here we take a different approach. Following the previous hypothesis

of the hydrophobic region, we construct a specific macroscopic model of a bubble within the framework of Poisson-Nernst-Planck (PNP) systems and show how it produces the time course of single K_v channels and the ensemble properties, including the Cole-Moore delay. The PNP system and its variants have been found successful in modeling and simulation of many biological processes [50, 51, 28, 52, 53, 54, 55], such as current-voltage curves through ion channels, the selectivity of ion channels, and ion transport processes in the cell and tissue scales. In this work, a bubble is assumed to be present in the pore (or filter) region of the K_v channel, due to the properties of the gating sensor and channel walls. In the bubble, ions are not present and so cannot carry charge through it, whereas outside the bubble, ion transport is governed by the PNP system. The model is constructed so it can easily accommodate more specific structural information such as the shape, permanent charge (e.g., the spatial distribution of acid and base residue side chains), and dielectric properties of the voltage sensor and conduction pore of channels. We calculate the properties of a single channel containing a bubble and an ensemble average based on a simple statistical distribution of such channels to represent the macroscopic currents usually recorded in studies of the opening and closing of channels. This average does not depend on models [56, 57] of single-channel kinetics. It only assumes that the opening of each channel (or voltage sensor) is independent of the others (because channels are many Debye lengths apart, shielded by the ions, water dipoles (and quadrupoles), and the ionic atmosphere of proteins and lipid bilayer).

This manuscript is arranged as follows. Section 2 sets up the bubble model within the framework of PNP systems, followed by a nondimensionalization. In section 3, the results for a single channel are presented. The bubble model is solved by a finite-difference method and also solved with analytical approximations. The results for the profiles of quantities in the model and the macroscopic currents through the channel are cross-validated by both methods. Section 4 shows the results for ensemble properties of the K_v channels and the Cole-Moore delay, with certain assumptions on the statistical distributions of the bubble locations and cross-sectional area of the channel. Finally, some concluding remarks are provided in Section 5.

2. A bubble model for a voltage-gated Potassium channel

2.1. The model setup

We consider a voltage-gated Potassium (K_v) channel in one spatial dimension, as shown in Figure 1. The total length of channel is set as $2L$, and the length of the middle (filter and pore) region is $2s$. The positions $x = \pm s$ are the locations of the two edges of the middle region. The bubble, which carried negative charges with magnitude $q_b > 0$, can occupy all or part of it, and is centered at $x = x_b$. We assume that the charge is uniformly distributed inside the bubble. The left chamber is connected to a bath environment similar to the exterior of a cell, while the right chamber is connected to one similar to interior of a cell. We further assume that the right interface of the bubble is fixed at $x = s$ and the left interface $x = s_b = -s + 2x_b$ is mobile. We anticipate that when the voltage at the right end of the channel is elevated, the bubble shrinks and moves to the right. When the left and right interfaces coincide, the bubble vanishes.

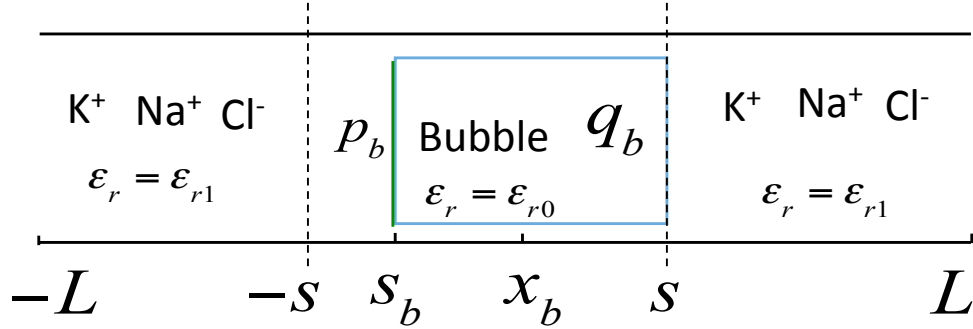


Figure 1: Sketch of the K_v channel with the bubble in the middle region.

We consider the case with three ions species K^+ , Na^+ and Cl^- (sometimes called the major bio-ions) outside of the bubble, and the ions can not penetrate into the bubble. Outside of the bubble, the PNP system is used to model ion transport

$$\begin{aligned}
 -\epsilon_0 \partial_x (\epsilon_r \partial_x \phi) &= e_0 (c_1 + c_2 - c_3), & -L < x < s_b, & s < x < L \\
 \frac{\partial c_i}{\partial t} &= -\partial_x J_i = D_i \partial_x \left(\partial_x c_i + \frac{e_0 z_i}{k_B T} c_i \partial_x \phi \right), & i &= 1, 2, 3,
 \end{aligned} \tag{1}$$

where c_1 , c_2 and c_3 are the concentrations of K^+ , Na^+ and Cl^- with valences $z_1 = 1$, $z_2 = 1$, $z_3 = -1$, ϕ is the electric potential, ϵ_r is the dielectric constant, D_i ($i = 1, 2, 3$) are diffusion coefficients, and ϵ_0, e_0, k_B, T are constants given in Appendix A.

The boundary conditions are given by

$$\begin{aligned}\phi(-L, t) &= 0, & \phi(L, t) &= V_0 + V_1 H(t - t_1), \\ c_i(-L, t) &= c_i^L, & c_i(L, t) &= c_i^R, \quad i = 1, 2, 3,\end{aligned}\tag{2}$$

where V_0 is the initial (holding) membrane potential when the bubble is in equilibrium (or resting state), V_1 is the voltage jump at $t = t_1$, $H(t)$ is a Heaviside function, and c_i^L and c_i^R ($i = 1, 2, 3$) are given bath concentrations at the left and right ends [30], which are electro-neutral. In the experiment, the holding potential V_0 is not the same as the Nernst potential of K^+ . The leak current is allowed to flow through a different pathway while maintaining V_0 .

Inside the bubble, we have

$$-\epsilon_0 \partial_x (\epsilon_r \partial_x \phi) = -\frac{q_b}{V_b}, \quad s_b(t) < x < s,\tag{3}$$

where $V_b = (s - s_b)A$ is the volume of the bubble and A is the cross sectional area for the bubble region. The dielectric constant is defined as

$$\epsilon_r = \begin{cases} \epsilon_{r0}, & [s_b, s] \\ \epsilon_{r1}, & \text{others.} \end{cases}\tag{4}$$

In addition, we assume that there exists a dipole on the left interface of the bubble $x = s_b$, responsible for maintaining a voltage difference on the two sides of the bubble. Since the membrane potential is not 0 at equilibrium, the presence of the dipole with a suitable dipole strength p_b guarantees that the bubble is in equilibrium initially. We can rewrite the equation of ϕ in a compact form in the entire domain

$$-\epsilon_0 \partial_x (\epsilon_r \partial_x \phi) = e_0(c_1 + c_2 - c_3) - \frac{q_b}{V_b} + p_b \partial_x (\delta(x - s_b)), \quad -L < x < L,\tag{5}$$

with the interpretation that $c_i = 0$ ($i = 1, 2, 3$) in the bubble and $q_b = 0$ outside of the bubble.

The total electric force on the bubble is

$$\int_A \int_{s_b}^s -\frac{q_b}{V_b} (-\partial_x \phi) dx dA = q_b \frac{\phi(s) - \phi(s_b)}{s - s_b}, \quad (6)$$

then the motion of the bubble is modeled by

$$\frac{dx_b}{dt} = \frac{q_b D_b}{k_B T} \frac{\phi(s) - \phi(s_b)}{s - s_b}, \quad (7)$$

where D_b ($\ll D_i$) is the diffusion coefficient of the bubble. Using the relationship $s_b = -s + 2x_b$, we can rewrite equation (7) as

$$\frac{ds_b}{dt} = \frac{2q_b D_b}{k_B T} \frac{\phi(s) - \phi(s_b)}{s - s_b}. \quad (8)$$

At the two interfaces $x = s_b$ and s , the electric potential and electric displacement are continuous, and there is no ionic flux across the bubble interfaces. Mathematically, we set

$$[\phi] = 0, \quad [\epsilon_r \partial_x \phi] = 0, \quad J_i = 0, \quad (i = 1, 2, 3), \quad (9)$$

where square brackets mean the jump across the interface, e.g., $[\phi(s)] = \phi(s+) - \phi(s-)$. If we include the effect of dipole (p_b in equation (5)) on the interface, we obtain a nonzero jump $[\phi]$ at $x = s_b$. When the two interfaces coincide (i.e., $s_b = s$), the bubble collapses. And we assume that the dipole disappears (i.e., it is treated as an intrinsic property of the bubble) and the interface conditions are replaced by continuity conditions

$$[\phi] = 0, \quad [\epsilon_r \partial_x \phi] = 0, \quad [c_i] = 0, \quad [J_i] = 0, \quad (i = 1, 2, 3). \quad (10)$$

In summary, we have a system of equations for ion transport coupled with the motion of the bubble, given by (5), (1)₂ and (8), together with boundary and interface conditions (2,9,10). The total current is conserved in this model, by including three different types of current, given in Appendix B. This is a special case of the continuity of total current for Maxwell equations [58, 59], and is also similar to the case of a PNP system for electric eels [50].

Remark 1. If the dipole does not vanish (i.e., it is treated as property of the channel or channel wall) after the bubble collapses, we will have nonzero jump $[\phi]$ related to the dipole, and $[c_i] = 0$ ($i = 1, 2, 3$) are replaced by continuity of electro-chemical potentials.

2.2. Nondimensionalization

In this subsection, we nondimensionalize our model, which will be used in the calculations in the subsequent sections. We adopt the following scales

$$\begin{aligned}
\tilde{x} &= \frac{x}{L}, & \tilde{s} &= \frac{s}{L}, & \tilde{x}_b &= \frac{x_b}{L}, & \tilde{V}_b &= \frac{V_b}{LA}, \\
\tilde{\phi} &= \frac{\phi}{k_B T/e_0}, & \tilde{V}_0 &= \frac{V_0}{k_B T/e_0}, & \tilde{V}_1 &= \frac{V_1}{k_B T/e_0}, \\
\tilde{c}_i &= \frac{c_i}{c_0}, & \tilde{c}_i^L &= \frac{c_i^L}{c_0}, & \tilde{c}_i^R &= \frac{c_i^R}{c_0}, & \tilde{D}_i &= \frac{D_i}{D_0}, \quad (i = 1, 2, 3), \\
\tilde{D}_b &= \frac{D_b}{D_0}, & \tilde{p}_b &= \frac{p_b}{e_0 c_0 L^2}, & \tilde{q}_b &= \frac{q_b}{e_0}, \\
\tilde{t} &= \frac{t}{t_0}, & t_0 &= \frac{L^2}{D_0}, & \tilde{J} &= \frac{J}{J_0}, & J_0 &= \frac{D_0 c_0}{L}.
\end{aligned} \tag{11}$$

Some typical values in the above scales and the following boundary conditions are based on [30] and given in Appendix A.

Substituting (11) into the system in the previous subsection, we obtain a dimensionless system for variables with tilde (like $\tilde{\phi}$). In order to simply the notations, we drop the tilde and use the quantities (like ϕ) in the dimensionless system. We have the following set of equations in nondimensional form

$$\begin{aligned}
-\epsilon \partial_x (\epsilon_r \partial_x \phi) &= c_1 + c_2 - c_3 - \frac{1}{\beta} \frac{q_b}{(s - s_b)} + p_b \partial_x (\delta(x - s_b)), & -1 < x < 1 \\
\frac{\partial c_i}{\partial t} &= -\partial_x J_i = D_i \partial_x (\partial_x c_i + z_i c_i \partial_x \phi), & i = 1, 2, 3, & -1 < x < s_b, s < x < 1,
\end{aligned} \tag{12}$$

with the interpretation that $c_i = 0$ ($i = 1, 2, 3$) in the bubble $x \in [s_b, s]$ and $q_b = 0$ outside of the bubble. Here the two dimensionless parameters are defined by

$$\epsilon = \frac{\epsilon_0 k_B T}{e_0^2 c_0 L^2}, \quad \beta = LA c_0. \tag{13}$$

The dielectric constant remains the same

$$\epsilon_r = \begin{cases} \epsilon_{r0}, & [s_b, s] \\ \epsilon_{r1}, & \text{others} \end{cases} \tag{14}$$

The motion of the bubble is given by

$$\frac{ds_b}{dt} = 2D_b q_b \frac{\phi(s) - \phi(s_b)}{s - s_b}. \quad (15)$$

Boundary conditions are given by

$$\begin{aligned} \phi(-1, t) = 0, \quad \phi(1, t) = V_0 + V_1 * H(t - t_1), \\ c_i(-1, t) = c_i^L, \quad c_i(1, t) = c_i^R, \quad (i = 1, 2, 3). \end{aligned} \quad (16)$$

Interface conditions are

$$[\phi] = 0, \quad [\epsilon_r \partial_x \phi] = 0, \quad J_i = 0, \quad (i = 1, 2, 3), \quad \text{at } x = s_b, s. \quad (17)$$

After the bubble collapses (for the case that the dipole disappears), we have

$$[\phi] = 0, \quad [\epsilon_r \partial_x \phi] = 0, \quad [c_i] = 0, \quad [J_i] = 0, \quad (i = 1, 2, 3), \quad \text{at } x = s_b = s. \quad (18)$$

3. Results for a single channel

We first compute the initial state when the bubble is in equilibrium by solving the system of equations with a numerical method, followed by the results of the non-equilibrium state including the motion of the bubble and time evolution of the concentrations and electric potential. After the bubble collapses, the ionic fluxes reaches a steady state. In addition, we also present the results obtained with an approximate solution (and numerical evidence) for the intermediate quasi-static states and the final steady state.

3.1. Initial state and strength of dipole

We examine the case that the bubble initially occupies the entire middle region and stays at equilibrium, i.e., $s_b = -s$. When $V_0 = 0$, the bubble is in equilibrium due to symmetry. If $V_0 \neq 0$, on the other hand, equilibrium is achieved for an appropriate dipole strength p_b .

Near the interface $x = s_b$, the effect of the other terms is small compared the dipole, and equation (12) becomes

$$-\epsilon \partial_x (\epsilon_r \partial_x \phi) = p_b \partial_x (\delta(x - s_b)), \quad (19)$$

and integrating once gives

$$-\epsilon \epsilon_r \partial_x \phi(x) = p_b \delta(x - s_b) + C. \quad (20)$$

By integrating again and taking the limit of $x \rightarrow s_b$, we obtain

$$[\phi(s_b)] = -\frac{p_b}{\epsilon} \left(\frac{1}{2\epsilon_{r0}} + \frac{1}{2\epsilon_{r1}} \right). \quad (21)$$

Therefore, for a given V_0 , we find the following relationship

$$-\frac{p_b}{\epsilon} \left(\frac{1}{2\epsilon_{r0}} + \frac{1}{2\epsilon_{r1}} \right) = V_0, \quad (22)$$

and then the bubble will be in equilibrium as in the symmetric case with $V_0 = 0$.

For the equilibrium profile, the fluxes are 0 and one can not distinguish the effects of the two positive ions Na^+ and K^+ . We can group the two positive ion species and treat them as a single species. The boundary conditions for $c_1 + c_2$ and c_3 will be the same, and hence we will have exact symmetry for this equilibrium case. The equilibrium profiles can be determined analytically, and we take $V_0 = 0$ and $p_b = 0$ in the derivation. Since the bubble is in equilibrium, inside the bubble we have (note $s_b = -s$)

$$\phi(x) = B_1 x^2 + \phi(0), \quad B_1 = \frac{q_b}{4s\epsilon\epsilon_{r0}\beta}. \quad (23)$$

Taking the derivative and together with interface conditions at $x = s$, we have

$$\epsilon_{r1}\phi'(s+) = \epsilon_{r0}\phi'(s-) = \epsilon_{r0}2B_1s = \frac{q_b}{2\epsilon\beta}. \quad (24)$$

Due to symmetry, we only consider the right chamber $s < x < 1$. It is easy to verify that the PNP system (12) in equilibrium reduces to

$$\epsilon\epsilon_{r1}\phi'' = c_3 - (c_1 + c_2) = e^\phi - e^{-\phi}, \quad (25)$$

where $c_3^R = 1$ has been used. Integrating once gives

$$\frac{1}{2}\epsilon\epsilon_{r1}[(\phi'(x))^2 - (\phi'(s+))^2] = e^\phi + e^{-\phi} - (e^{\phi_s} + e^{-\phi_s}), \quad (26)$$

where $\phi_s = \phi(s)$. Then, by combining with (23), we get

$$(\phi'(x))^2 = G(\phi) = \left(\frac{q_b}{2\epsilon\beta\epsilon_{r1}} \right)^2 + \frac{2}{\epsilon\epsilon_{r1}} (e^\phi + e^{-\phi} - (e^{\phi_s} + e^{-\phi_s})), \quad (27)$$

which leads to the solution

$$x = \int_{\phi_s}^{\phi} \frac{1}{\sqrt{G(\phi)}} d\phi + s. \quad (28)$$

The unknown constant ϕ_s in the solution can be determined by the condition

$$1 = \int_{\phi_s}^0 \frac{1}{\sqrt{G(\phi)}} d\phi + s. \quad (29)$$

Remark 2. Because of symmetry, we can estimate ϕ_s from the above derivation as

$$\phi_s \approx -\ln\left(\frac{q_b^2}{8\epsilon\epsilon_{r1}\beta^2}\right) \quad (30)$$

for q_b in a certain range.

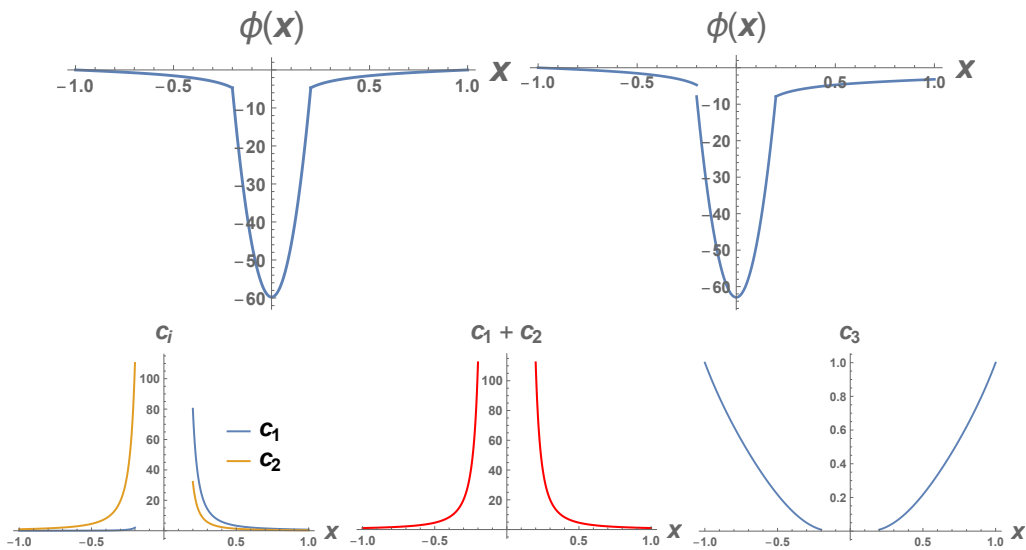


Figure 2: Equilibrium electric potential ϕ and concentrations c_1, c_2, c_3 when $q_b = 2$.

For the numerical results obtained in this paper, we vary the potentials at the two end of the domain while fixing the magnitude of permanent charge as $q_b = 2$. Most of the other parameter values used for the computation are also fixed and given in Appendix A.

In Figure 2(a), the electric potential ϕ is plotted for the case of $V_0 = 0$. When $V_0 = -3.18$ (i.e., -80 mV), we obtain $p_b \approx 0.044$ using (22) and the

electric potential is plotted in Figure 2(b), where the jump at the interface $x = s_b$ is due to the presence of the dipole. The concentrations c_1 , c_2 and c_3 (which can be computed from solution of ϕ) are shown in Figures 2(c-e). It can be seen that $c_1 + c_2$ is symmetric (Figure 2(d)) as expected. The initial membrane potential V_0 is balanced by the jump of ϕ due to the presence of the dipole. In the non-equilibrium case (before the bubble collapses), we ignore both the initial membrane potential V_0 and the dipole, so that the value of ϕ is continuous at the interfaces. The solutions in Figure 2 will be verified by numerical simulations in the subsequent subsections.

3.2. The dynamics of the bubble motion and channel currents

In this part, we present numerical solutions of the PNP system and bubble motion. Inside the bubble, there exist no ions and their concentrations c_i ($i = 1, 2, 3$) are zero. For convenience, the PNP system is solved inside the bubble by assigning small diffusion coefficients ($D_1 = D_2 = 10^{-15}$).

The finite difference method is used to solve the system, with a uniform mesh $h = x_k - x_{k-1}$. A temporal semi-implicit discrete scheme is used with $t_n = n\Delta t$ and $x_k = x_0 + kh$, given by

$$\begin{aligned}
& -\epsilon \frac{\epsilon_{r,k-1/2}}{h^2} \phi_{k-1}^{n+1} + \epsilon \frac{\epsilon_{r,k-1/2} + \epsilon_{r,k+1/2}}{h^2} \phi_k^{n+1} - \epsilon \frac{\epsilon_{r,k+1/2}}{h^2} \phi_{k+1}^{n+1} \\
& \quad - c_{1,k}^{n+1} - c_{2,k}^{n+1} + c_{3,k}^{n+1} = -q_k^{n+1}, \\
\frac{c_{i,k}^{n+1} - c_{i,k}^n}{\Delta t} &= -\frac{J_{i,k+1/2}^{n+1} - J_{i,k-1/2}^{n+1}}{h}, \quad i = 1, 2, 3, \\
J_{i,k+1/2}^{n+1} &= -D_{i,k+1/2} \frac{c_{i,k+1}^{n+1} - c_{i,k}^{n+1}}{h} - D_{i,k+1/2} z_i c_{k+1/2}^n \frac{\phi_{k+1}^{n+1} - \phi_k^{n+1}}{h},
\end{aligned} \tag{31}$$

where harmonic average is used for the diffusion coefficient

$$D_{i,k+1/2} = \frac{2}{\frac{1}{D_{i,k}} + \frac{1}{D_{i,k+1}}}, \quad i = 1, 2, 3. \tag{32}$$

In this way, we ensure that the ionic fluxes are small near the interface as approximations of $J_i = 0$ ($i = 1, 2, 3$). When the bubble collapses, the diffusion coefficient is guaranteed to be the same as that outside of the bubble, and the continuity conditions are recovered. The quantities $\epsilon_{r,k+1/2}$ and q_k^n in (31) are defined in Appendix B. The discrete scheme also preserves the continuity of the total current, as in the original continuous model.

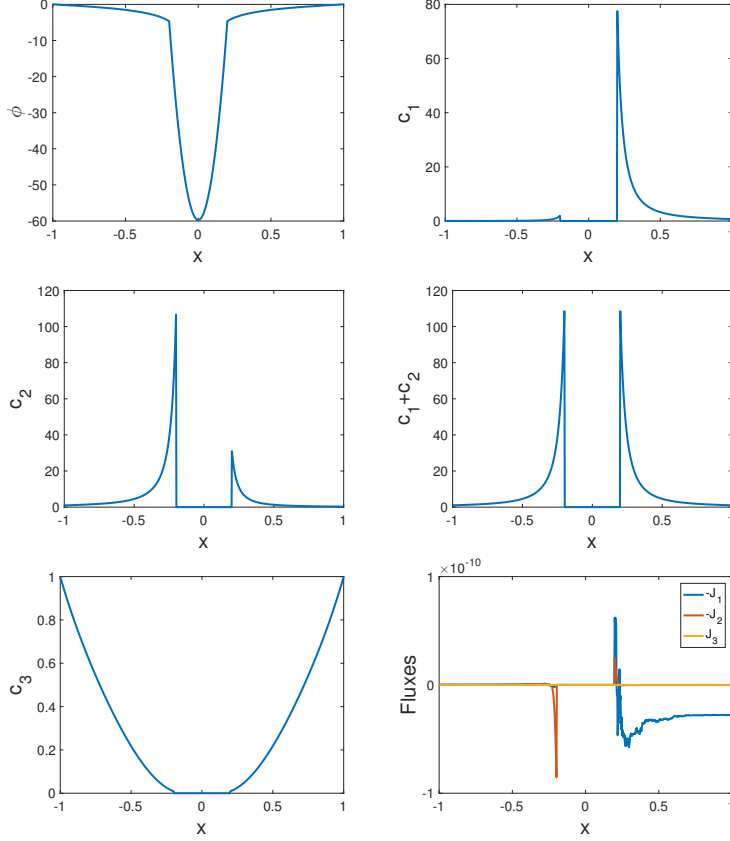


Figure 3: Equilibrium electric potential ϕ , concentrations c_1 , c_2 , $c_1 + c_2$, c_3 , and ionic fluxes J_i ($i = 1, 2, 3$) with $h = 0.0025$.

For $q_b = 2$, we first compute the initial equilibrium when the bubble occupies the entire middle region. The initial condition at $t = 0$ is set as

$$\begin{aligned} \phi(x, 0) &= 0, \quad -1 < x < 1, \\ c_i(x, 0) &= \begin{cases} c_i^L & -1 < x < s_b = -s, \\ 0 & s_b < x < s, \\ c_i^R & s < x < 1, \end{cases} \end{aligned} \quad (33)$$

where $i = 1, 2, 3$. We also set $V_0 = 0$ and $p_b = 0$ in the computation so that ϕ is continuous. The computation is carried out until the system reaches a steady state. For a given mesh size $h = 0.0025$, Figure 3 shows the

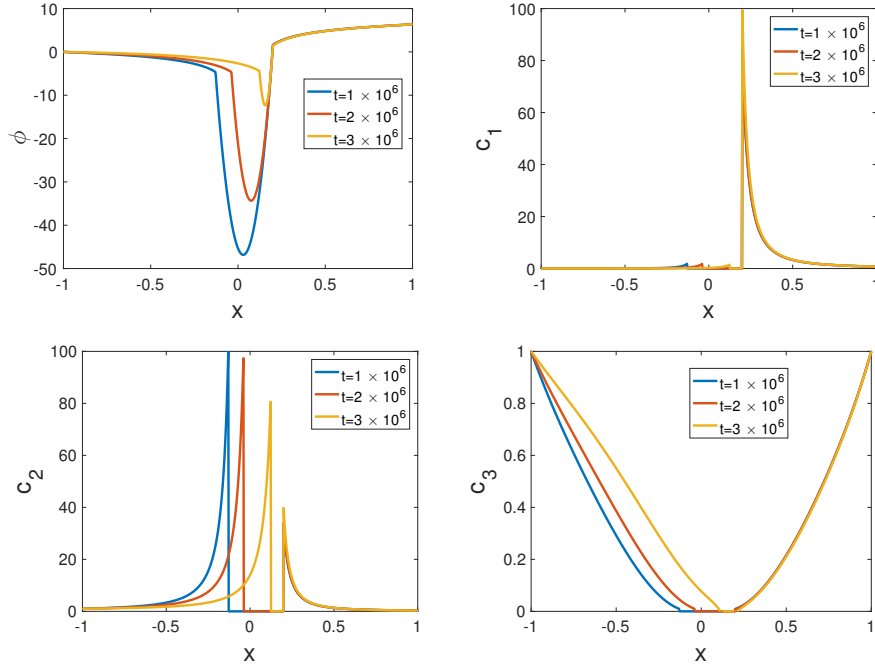


Figure 4: Electric potential ϕ and ionic concentrations c_1, c_2, c_3 at three different times with $V_1 = 6.36$.

numerical solution of electric potential ϕ , concentrations c_i and ionic fluxes J_i ($i = 1, 2, 3$), which are in good agreement with the analytical results in the previous subsection.

Next, we present the results on the bubble motion and dynamic behaviour of the PNP system. We start from the equilibrium state at $t = 0$ and increase the electric potential from zero to $\phi(1, t) = V_1 = 6.36$ (i.e., 160 mV) for $0 < t < t^*$ (we already set $V_0 = 0$ and $p_b = 0$), where t^* is the unknown time when the bubble collapses. Figure 4 shows ϕ, c_i ($i = 1, 2, 3$) at three different times. The minimum value for ϕ inside the bubble gradually increases in Figure 4(a), and the interface s_b moves to the right as indicated by Figure 4. Figure 5 shows the ionic fluxes at three different times, which are small. After the bubble collapses and the dipole disappears, we reset $\phi(1, t) = V_0 + V_1 = 3.18$. Figure 6 shows the three ionic fluxes at $x = \pm 1$. It can be seen that they remain small until the bubble collapses (i.e., $s_b = s$) at $t^* = 3.13 \times 10^6$, which is 17.6 ms in dimensional unit. The ionic fluxes

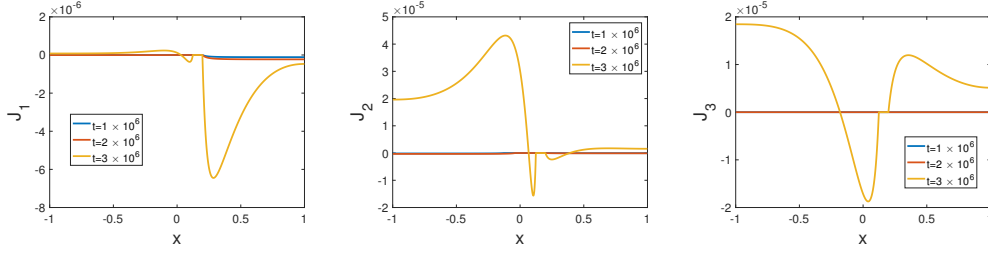


Figure 5: The fluxes J_i ($i = 1, 2, 3$) at three different times with $V_1 = 6.36$.

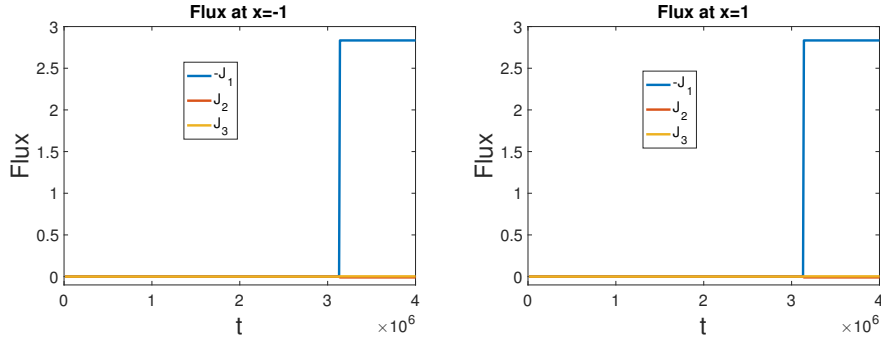


Figure 6: The dynamics of ionic fluxes J_i ($i = 1, 2, 3$) with $V_1 = 6.36$.

and ϕ, c_i ($i = 1, 2, 3$) reach a steady state soon after the bubble collapses, as shown in Figure 7. At steady state, the dimensionless ionic flux J_1 and the dimensional current I are found to be

$$J_1 \approx -2.834, \quad I = |J_1|e_0AJ_0 \approx 10 \text{ pA}. \quad (34)$$

Remark 3. The value of the steady state current I obtained above is close to that given in Figure 2(a) of [30]. When the voltage jump V_1 is reset to zero after system reaches a steady state, the ionic fluxes reduce to zero immediately, indicating the closure of the ion channel. In this sense, our proposed model provides a plausible gating mechanism once the bubble is generated. However, the mechanism of the bubble generation is not considered here and will be the subject of a future study.

3.3. Quasi-static equilibrium

Since the motion of the bubble is extremely slow compared with the diffusive timescale of the ions, ionic fluxes are essentially zero (Figure 5) before

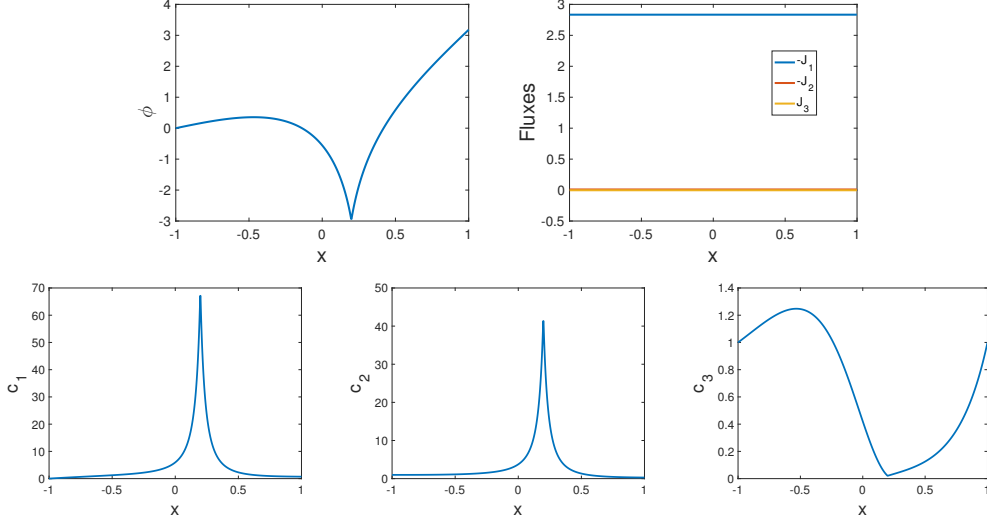


Figure 7: The steady state with $V_1 = 6.36$.

the bubble collapses. Therefore, we can use quasi-static solution with zero ionic fluxes as an approximation of the intermediate states. A hybrid method can be used to determine the solution of intermediate states by first obtaining an analytical solution (in terms of integrals), where integration constants involved can be determined easily using a numerical method afterwards.

Given boundary condition V_1 and interface position s_b , solving the quasi-static equilibrium is similar to that for solving the initial state. We set $V_0 = 0$ and $p_b = 0$ so that the continuity condition of ϕ can be used at interface s_b . Inside the bubble, we have

$$\phi(x) = B_1(x - s)^2 + \tilde{\phi}_s(x - s) + \phi_s, \quad B_1 = \frac{q_b}{2(s - s_b)\epsilon\epsilon_{r0}\beta}, \quad (35)$$

where $\phi_s, \tilde{\phi}_s$ are to be determined. The solutions of ϕ outside of the bubble can be written as

$$\begin{aligned} x &= \int_{\phi_s}^{\phi} \frac{1}{\sqrt{G_1(\phi; \phi_s, \tilde{\phi}_s)}} d\phi + s, \quad s < x < 1, \\ x &= - \int_{\phi_{sb}}^{\phi} \frac{1}{\sqrt{G_2(\phi; \phi_s, \tilde{\phi}_s)}} d\phi + s_b, \quad -1 < x < s_b, \end{aligned} \quad (36)$$

where $\phi_{s_b} = \phi(s_b)$ can be expressed by ϕ_s and $\tilde{\phi}_s$. The derivation for $G_1(\phi), G_2(\phi)$ are given in Appendix C. For given parameter values including V_1 and s_b , the two unknowns ϕ_s and $\tilde{\phi}_s$ can be determined by the two boundary conditions $\phi(1) = V_1$ and $\phi(-1) = 0$, i.e.,

$$1 = \int_{\phi_s}^{V_1} \frac{1}{\sqrt{G_1(\phi; \phi_s, \tilde{\phi}_s)}} d\phi + s, \quad -1 = - \int_{\phi_{s_b}}^0 \frac{1}{\sqrt{G_2(\phi; \phi_s, \tilde{\phi}_s)}} d\phi + s_b, \quad (37)$$

and $\phi(x), c_i(x)$ ($i = 1, 2, 3$) can be obtained afterwards. As an example, for $q_b = 2$, $V_1 = 6.36$ and $s_b = 0$, solutions of ϕ and c_i ($i = 1, 2, 3$) can be computed using the procedure outlined above and plotted in Figure 8.

For fixed V_1 , we can treat $\phi(s), \phi(s_b)$ as functions of the parameter s_b , which can be determined by

$$\frac{ds_b}{dt} = 2D_b q_b \frac{\phi(s) - \phi(s_b)}{s - s_b} = 2D_b q_b f(s_b). \quad (38)$$

Integrating in time, we obtain t^* , the time delay after the voltage jump and before the bubble collapses,

$$t^* = \int_{-s}^s \frac{1}{2D_b q_b f(x)} dx. \quad (39)$$

Figure 9(a) shows the dependence of quantities $\phi(s)$ and $\phi(s_b)$ on s_b and Figure 9(b) shows the function $f(s_b)$. From (39), we find that $t^* \approx 3.26 \times 10^6$, which is 18.3 ms in dimensional unit, which is slightly longer than that obtained using the finite difference method (17.6 ms) previously.

3.4. The steady state after the collapse of the bubble

After the bubble collapses, interface conditions $J_i = 0$ ($i = 1, 2, 3$) are replaced by continuity conditions $[J_i] = 0$ and q_b becomes a point charge (a delta function). Due to the presence of q_b , the concentration of c_3 is approximately zero near $x = s$, and we assume $J_3/D_3 \approx 0$. The system at the steady state can be approximated by

$$\begin{aligned} -\epsilon\epsilon_{r1}\phi''(x) &= c_1 + c_2 - c_3 - \frac{q_b}{\beta}\delta(x - s), \\ -J_1 &= c'_1 + c_1\phi', \\ -\frac{J_2}{D_2} &= c'_2 + c_2\phi', \\ 0 &= c'_3 - c_3\phi', \end{aligned} \quad (40)$$

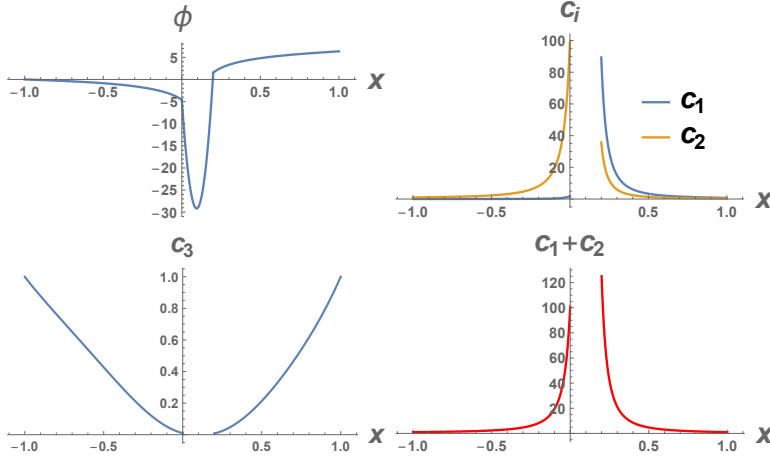


Figure 8: The quasi-static solution of ϕ , c_1 , c_2 , c_3 and $c_1 + c_2$ for $s_b = 0$ and $V_1 = 6.36$.

where $D_1 = 1$ has been used. If we combine the effects of c_1, c_2 and define $J_p = J_1 + \frac{J_2}{D_2}$, then the system can be reduced to a single equation of ϕ (see the derivation in Appendix C)

$$\begin{aligned}
 -\epsilon\epsilon_{r1}\phi''(x) &= \frac{1}{2}\epsilon\epsilon_{r1} [(\phi'(x))^2 - (\phi'(1))^2] - J_p(x-1) - 2(e^{\phi-V} - 1), \\
 &\quad \text{for } s < x < 1, \\
 -\epsilon\epsilon_{r1}\phi''(x) &= \frac{1}{2}\epsilon\epsilon_{r1} [(\phi'(x))^2 - (\phi'(-1))^2] - J_p(x+1) - 2(e^{\phi} - 1), \\
 &\quad \text{for } -1 < x < s,
 \end{aligned} \tag{41}$$

where $V = V_0 + V_1$ and $c_3^L = c_3^R = 1$ have been used. The point charge (delta function) at $x = s$ gives the jump condition

$$[\phi'] = \frac{q_b}{\beta\epsilon\epsilon_{r1}}. \tag{42}$$

Given $\phi'(1)$, $\phi'(-1)$, and J_p , the solutions can be easily determined numerically, in the two regions $s < x < 1$ and $-1 < x < s$. The three constants $\phi'(1)$, $\phi'(-1)$, J_p can be determined by condition (42), $[\phi] = 0$ and $[c_1 + c_2] = 0$ at $x = s$ (in practice the numerical procedure is more stable if the ratio $(c_1(s+) + c_2(s+))/(c_1(s-) + c_2(s-)) = 1$ is used instead of $[c_1 + c_2] = 0$). Once $\phi(x)$ is obtained, c_1 and flux J_1 can be computed by equation (40)₂ and

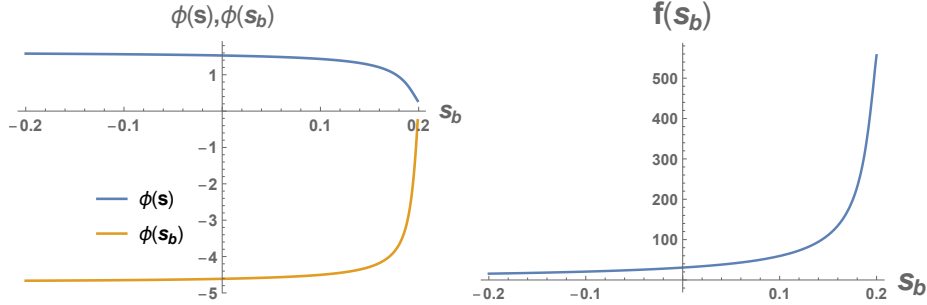


Figure 9: The dependence of $\phi(s)$ and $\phi(s_b)$ on s_b and the function $f(s_b)$ for $V_1 = 6.36$.

the continuity condition $[c_1] = 0$ at $x = s$. Similarly, c_2 and flux J_2 can be computed by equation (40)₃ and the continuity condition $[c_2] = 0$ at $x = s$.

Figure 10 shows the semi-analytical approximation ϕ and c_i ($i = 1, 2, 3$) at steady state for $V_1 = 6.36$, which agrees with those in Figure 7 except for c_3 . For $V_1 = 6.36$, ionic flux J_1 is found to be $J_1 \approx -2.855$ (also ≈ 10 pA in units), which is close to -2.834 in (34) obtained by the finite difference method. The advantage of the method in this subsection is that the computation is extremely fast compared with the full finite difference method. It is much more efficient to use the semi-analytical approximation to compute the steady states (particularly the currents) with various different voltage jump V_1 .

Figure 11 shows the results with $V_1 = 1.59$ (i.e., 40 mV in physical units), and the flux is $J_1 \approx -0.264$ (i.e., 0.933 pA in units). In above computations, J_2 is very small since a small D_2 is used, therefore the dimensionless total current is almost the same as J_1 . Figure 12 shows the dependence of dimensionless flux $-J_1$ and the dimensional current on the voltage $V = V_0 + V_1$ at steady state.

Remark 4. In the present simple model, the permanent charge is evenly distributed in the bubble only and the size effect of different ions are not considered. We do not expect our model to capture the current-voltage relation for large V_1 , including the saturation phenomenon observed experimentally in the literature. To make our model more realistic, we need to know the distribution of permanent charge (i.e., acid base side chains) along the system. When that information is available, it can be incorporated into our model by adding permanent charge to the channel wall in the region $-s$ to

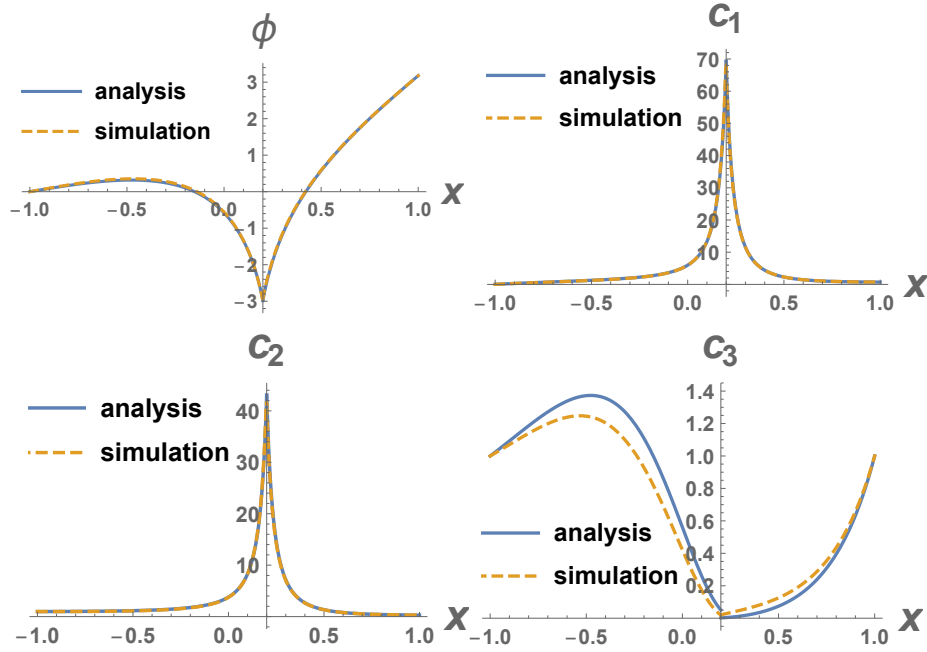


Figure 10: Comparison of ϕ and c_i ($i = 1, 2, 3$) at steady state with $V_1 = 6.36$ between semi-analytical approximation (solid lines) and the finite-difference solution (dashed lines).

$+s$ (see Fig. 1) as in a practical implementation [60]. The studies [54, 55] by Weishi Liu and his group have illustrated the effects of permanent charge on current-voltage relation. With ionic size effect and the permanent charge, saturation phenomenon of current-voltage curves can be modelled as shown in [51].

Remark 5. For the case that the dipole does not disappear after bubble collapses, Figure 13 shows the results for steady state flux, which are quite similar to those in Figure 12 for the above case when dipole disappears after bubble collapses.

4. Ensemble properties

In this section, we extend our model by including stochastic effect in two aspects. We assume that the initial position of the bubble and the cross sectional area of the channel are both random and compute the ensemble

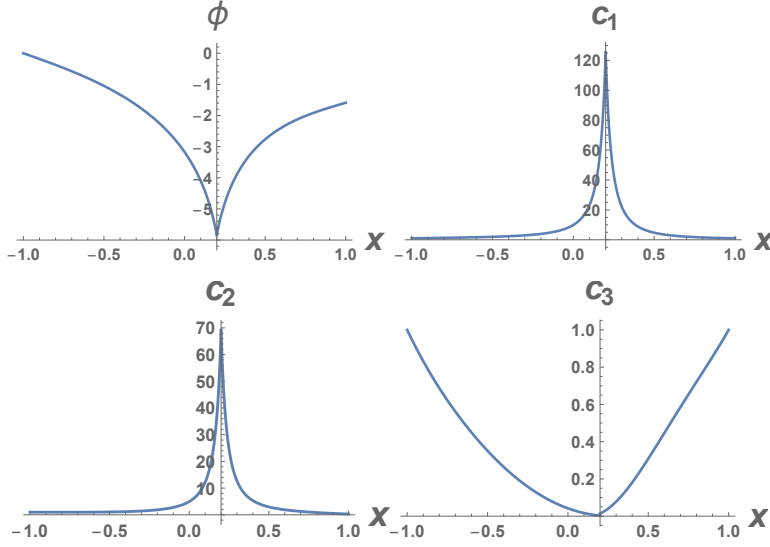


Figure 11: Steady state ϕ and c_i ($i = 1, 2, 3$) for $V_1 = 1.59$.

averages of the macroscopic currents through the channel and estimate the Cole-Moore delay based on certain statistical distributions.

First, we assume that the initial interface position s_b is random, which could be due to the tiny fluctuations of strength of dipoles in different channels or due to the mechanism of bubble formation (which is not considered in the present work). For illustration, we consider that s_b follows a normal distribution

$$s_b \sim N(\mu, \sigma^2), \quad \mu = 0, \quad \sigma = 0.05, \quad (43)$$

where the choice of σ ensures that $s_b \in [-s, s]$ with $s = 0.2$ for almost all the generated data. We can use the previous function $f(s_b)$ to compute the ensemble properties of the channel, since there is negligible effect on the curves of $f(s_b)$ with different starting value of s_b . With each different initial position s_b , the dynamics of the fluxes (particularly the time delay t^* for opening of the channel) will be different. By taking the average of these fluxes, we get the ensemble curve for the dynamics of the current through the channel (i.e., fluxes of K^+). Figure 14 (b,c) show the ensemble curves for the current I and the ratio I/V_1 with 50 channels and with 4 different voltage jumps, which are given in Figure 14(a). Figure 14 (b) shows similar trend and scale with experiments in Figure 2(a,c) in [30].

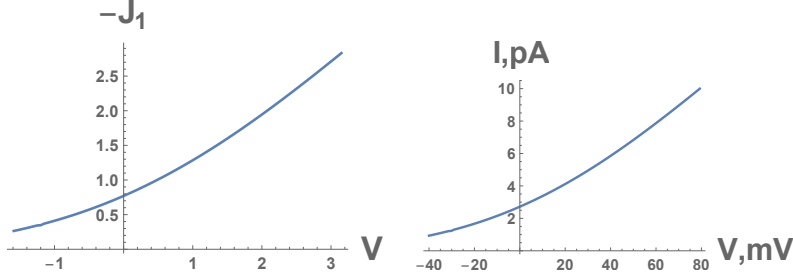


Figure 12: The dependence of the dimensionless flux J_1 and the dimensional current I on the voltage $V = V_0 + V_1$ at steady state.

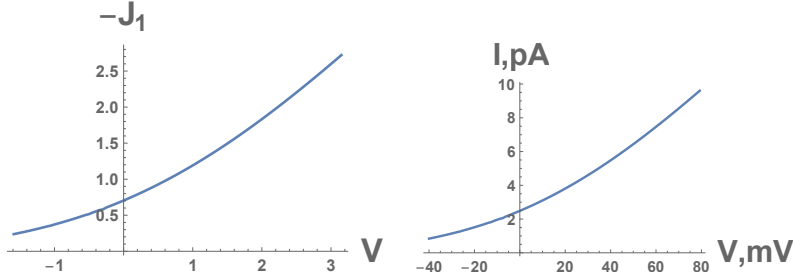


Figure 13: The dependence of the dimensional flux J_1 and the dimensional current I on the voltage $V = V_0 + V_1$ at steady state for the case that the dipole does not disappear after the bubble collapses.

The case is more complicated when cross sectional area A is random. We set $A = A_0 A_1$, where $A_1 \sim N(1, \sigma_A^2)$ with $\sigma_A = 0.03$ and $A_0 = (0.7\text{nm})^2$ (the same as the value in Appendix A). The area A will affect the dimensionless parameter β , and hence influences the effective permanent charge q_b/β .

We start by examining the effect of A_1 on t^* . Figure 15 shows $f(s_b)$ with 3 different values of A_1 , indicating that the effect of A_1 on $f(s_b)$ and hence on t^* is very small. Therefore, the previous curve $f(s_b)$ can be used to compute t^* as an approximation. We study the effect of A_1 on the flux J_1 or the current I at steady state. Figure 16(a) shows the dependence of $-J_1$ on A_1 , indicating that the magnitude of J_1 will slightly decrease with increase of A_1 . Since the final dimensional current also depends on the scaling factor which contains A_1 , Figure 16(b) shows the dependence of the current I on the parameter A_1 , indicating that the current increases with A_1 . Figure 16(b)

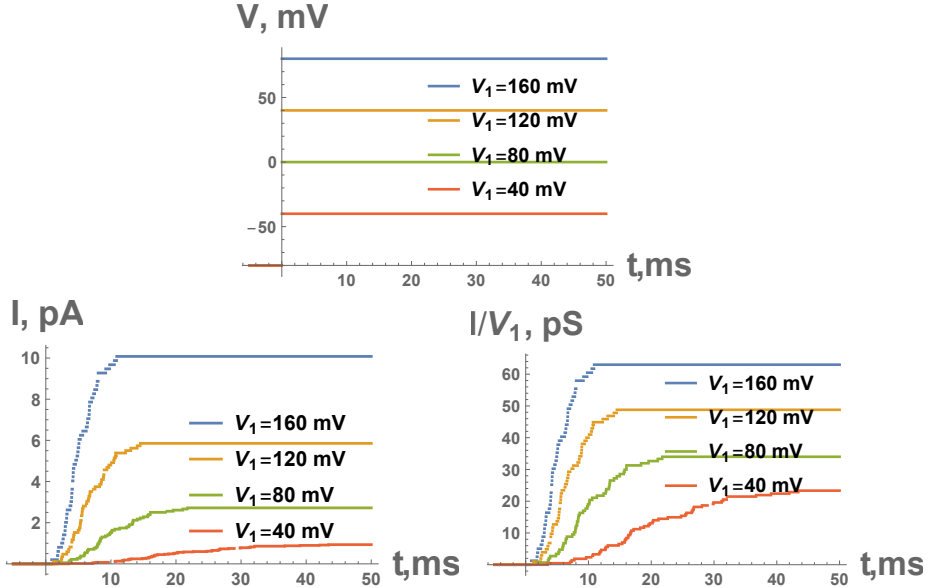


Figure 14: The ensemble curves for the current I and the ratio I/V_1 averaged by 50 random s_b and with 4 different V_1 .

also shows the approximate current $A_1 I(1)$ where $I(1)$ is taken from previous computation with $A_1 = 1$, which is close to the exact curve. Therefore, the main effect of A_1 on the current is due to the scaling factor. We conclude that $A_1 I(1)$ can be used as an approximation for the current in the following figures.

We fix A_1 for each channel during the evolution of the bubble, while allowing it (together with s_b) to vary randomly among 50 channels. The ensemble curves for the current with 50 channels are very similar to those in Figure 14. We also consider the case that A_1 fluctuates randomly when the bubble evolves. We take $A_1(t_i) \sim N(1, \sigma_A^2)$ with $\sigma_A = 0.03$ for each discrete time $t = t_i$ and for each channel. Figure 17 shows the ensemble curve for the current with 50 channels, where $s_b \sim N(0, \sigma^2)$ and $A_1(t_i) \sim N(1, \sigma_A^2)$, with $\sigma = 0.05$, $\sigma_A = 0.03$, and 400 discrete t_i are used for the time interval of 30 ms. Figure 17 shows similar trend and fluctuations with those in experiments, see Figure 2(a,c) in [30] and Figure 3.17 in [4].

To model the Cole-Moore delay [38], we can treat the mean value μ and standard variation σ in (43) as a function of the holding potential V_0 . For

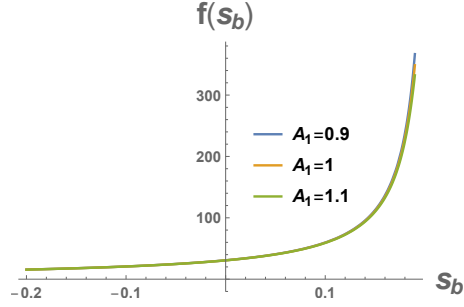


Figure 15: The function $f(s_b)$ with 3 values of the parameter A_1 .

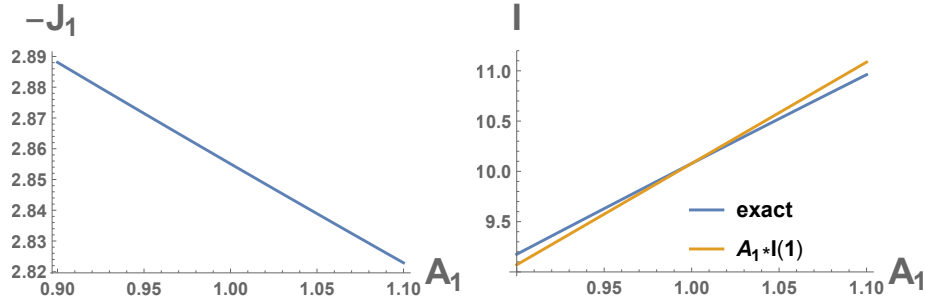


Figure 16: The dependence of the flux $-J_1$ and the current I on the parameter A_1 .

illustration, we take

$$\begin{aligned}
 s_b &\sim N(\mu, \sigma^2), \\
 \mu(V_0) &= s \tanh(k(V_0 - V_0^*)), \quad V_0^* = -80\text{mV}, \quad k = 0.002/\text{mV}, \\
 \sigma(V_0) &= \sigma_0 = 0.05
 \end{aligned} \tag{44}$$

where V_0 is the initial holding potential, and V_0^* is a reference value. Figure 18(a) shows the ensemble curves for the current with 100 channels and $V_1 = 160$ mV, for 7 different holding potential V_0 which are $[-52, -72, -93, -113, -133, -162, -212]$ mV, corresponding to curves from left to right. The ensemble curves show similar features as experimental curves in Figure 18(b), which is reproduced from Figure 5(a) in [38]. Figure 19 shows the ensemble curves for the current with 100 channels and 600 channels and with $V_1 = 160$ mV, for 2 different holding potential $V_0 = -52, -212$ mV. It can be observed from the figures that the delay is longer when holding potential V_0 is smaller.

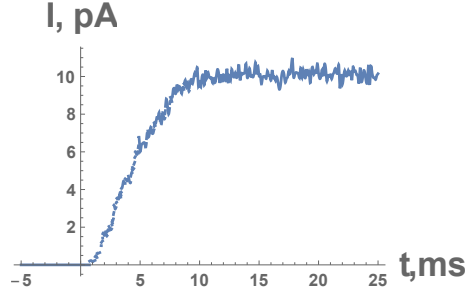


Figure 17: The ensemble curves for the current with 50 channels, where $s_b \sim N(0, \sigma^2)$ and $A_1(t_i) \sim N(1, \sigma_A^2)$, with $\sigma = 0.05, \sigma_A = 0.03$.

Remark 6. We note that the Cole-Moore effect may also arise in the hydrophobic gasket of the voltage sensor region of the channel and show itself as a delay in gating current [41]. The bubble in the voltage sensor itself would not collapse, and the gating current would be given by our equations (B.4-B.6). We speculate that some of the gating current could flow in the adjacent conduction pore, and open it, perhaps by collapsing a bubble in the conduction pore.

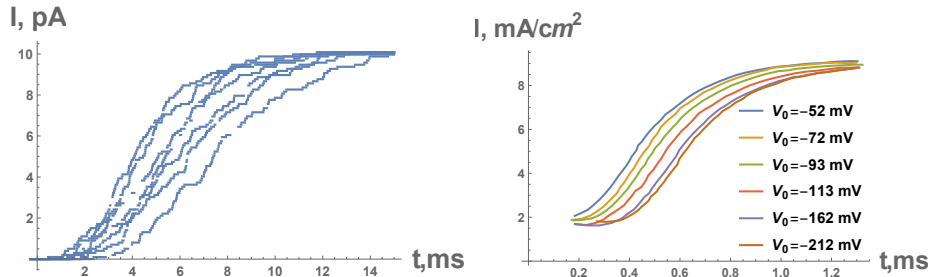


Figure 18: (a) The ensemble curves for the current with 100 channels and $V_1 = 160$ mV, for 7 different holding potentials V_0 , (b) the ensemble curve reproduced based on the experiments in Figure 5(a) of [38].

5. Conclusion

In this paper, we present a macroscopic bubble model for the gating of K_v Channels. The time delay in the opening of a single channel is determined by the motion of the bubble before it collapses. The bubble motion

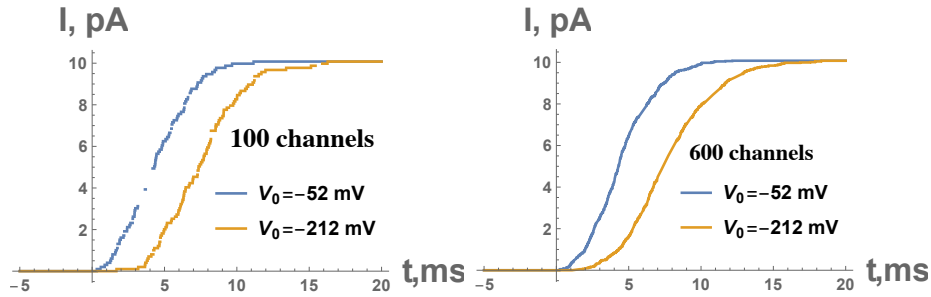


Figure 19: The ensemble curves for the current for $V_1 = 160$ mV and 2 different holding potential V_0 , (a) with 100 channels, and (b) with 600 channels.

is coupled with a Poisson-Nernst-Planck system, which is solved by a full numerical computation as well as a quasi-static approximation method. We also present a stochastic model for the bubble and channel sizes and the ensemble properties of the K_v channel are consistent with experimental observations. Furthermore, the Cole-Moore delay is explored by assuming the dependence of bubble properties on the holding potential.

Although the present simple model captures some key features in the ensemble properties, some parts are oversimplified and there is room for improvement. The permanent charges in the channel are lumped together in the model, and the distinction and effects of charges on bubble and on the channel wall could be examined in the future. The selectivity of channel is not considered in detail here, which depends on the ion sizes (which makes the PNP system very complicated). This is circumvented by assuming small diffusion constants of other ions except K^+ in the present work. The generalization to high-dimensional case is also interesting and nontrivial, since the bubble interface will have a curved shape and specific forces (e.g., some force due to the maxwell stress) can act on the interface.

References

- [1] M. Biel, C. Wahl-Schott, S. Michalakis, X. Zong, Hyperpolarization-activated cation channels: from genes to function, *Physiological reviews* 89 (3) (2009) 847–885.
- [2] M. Ø. Jensen, V. Jogini, D. W. Borhani, A. E. Leffler, R. O. Dror,

- D. E. Shaw, Mechanism of voltage gating in potassium channels, *Science* 336 (6078) (2012) 229–233.
- [3] D. A. Jacobson, F. Mendez, M. Thompson, J. Torres, O. Cochet, L. H. Philipson, Calcium-activated and voltage-gated potassium channels of the pancreatic islet impart distinct and complementary roles during secretagogue induced electrical responses, *The Journal of physiology* 588 (18) (2010) 3525–3537.
- [4] B. Hille, *Ion channels of excitable membranes*, Sinauer Associates, Inc., 2001.
- [5] A. Huxley, *The quantitative analysis of excitation and conduction in nerve. from nobel lectures, physiology or medicine 1963–1970* (1972).
- [6] A. F. Huxley, *Kenneth Stewart Cole 1900-1984. A biographical memoir by Sir Andrew Huxley*, National Academies Press, Washington DC, 1996.
- [7] A. Huxley, From overshoot to voltage clamp, *Trends in Neurosciences* 25 (11) (2002) 553–558.
- [8] A. Hodgkin, *Chance and Design*, Cambridge University Press, New York, 1992.
- [9] S. J. Gould, *The Flamingo’s Smile: Reflections in Natural History*, Norton, New York, 1987.
- [10] A. L. Hodgkin, A. F. Huxley, A quantitative description of membrane current and its application to conduction and excitation in nerve, *The Journal of physiology* 117 (4) (1952) 500.
- [11] R. MacKinnon, Nobel lecture. potassium channels and the atomic basis of selective ion conduction, *Biosci Rep* 24 (2) 75–100.
- [12] E. Neher, *Ion channels for communication between and within cells Nobel Lecture, December 9, 1991*, World Scientific Publishing Co, Singapore, 1997, pp. 10–25.
- [13] D. Boda, W. Nonner, M. Valisko, D. Henderson, B. Eisenberg, D. Gillespie, Steric selectivity in na channels arising from protein polarization and mobile side chains, *Biophys J* 93 (6) (2007) 1960–80.

doi:10.1529/biophysj.107.105478.

URL <http://www.ncbi.nlm.nih.gov/pubmed/17526571>

- [14] T. Dudev, C. Lim, Factors governing the na⁺ vs k⁺ selectivity in sodium ion channels, *Journal of the American Chemical Society* 132 (7) (2010) 2321–2332.
- [15] T. Dudev, C. Lim, Ion selectivity strategies of sodium channel selectivity filters, *Accounts of chemical research* 47 (12) (2014) 3580–3587.
- [16] C. Lim, T. Dudev, Potassium versus sodium selectivity in monovalent ion channel selectivity filters, Springer, 2016, pp. 325–347.
- [17] F. Bezanilla, How membrane proteins sense voltage, *Nat Rev Mol Cell Biol* 9 (4) 323–32. doi:nrm2376 [pii] 10.1038/nrm2376.
- [18] F. Bezanilla, Ion channels: from conductance to structure, *Neuron* 60 (3) 456–68. doi:S0896-6273(08)00900-8 [pii] 10.1016/j.neuron.2008.10.035.
- [19] F. Bezanilla, Gating currents, *The Journal of General Physiology* 150 (7) (2018) 911–932. doi:10.1085/jgp.201812090.
URL <https://doi.org/10.1085/jgp.201812090>
- [20] J. J. Lacroix, H. C. Hyde, F. V. Campos, F. Bezanilla, Moving gating charges through the gating pore in a kv channel voltage sensor, *Proceedings of the National Academy of Sciences* 111 (19) (2014) E1950–E1959.
- [21] L. Catacuzzeno, F. Franciolini, Simulation of gating currents of the shaker k channel using a brownian model of the voltage sensor, *Biophysical journal* 117 (10) (2019) 2005–2019.
- [22] L. Catacuzzeno, L. Sforza, F. Franciolini, Voltage-dependent gating in k channels: experimental results and quantitative models, *Pflügers Archiv-European Journal of Physiology* 472 (1) (2020) 27–47.
- [23] L. Catacuzzeno, L. Sforza, F. Franciolini, R. Eisenberg, Why are voltage gated na channels faster than k channels? one multi-scale hierarchical model, *bioRxiv*. Cold Spring Harbor Laboratory 11.
- [24] C. A. Bassetto, J. L. Carvalho-de Souza, F. Bezanilla, Molecular basis for functional connectivity between the voltage sensor and the selectivity filter gate in shaker k⁺ channels, *Elife* 10 (2021) e63077.

- [25] L. Catacuzzeno, F. Franciolini, F. Bezanilla, R. S. Eisenberg, Gating current noise produced by brownian models of a voltage sensor, *Biophysical Journal* 120 (September 21, 2021) (2021) 1–19. doi:10.1016/j.bpj.2021.08.015.
URL <https://dx.doi.org/10.1016/j.bpj.2021.08.015>
- [26] L. Catacuzzeno, L. Sforza, F. Franciolini, R. S. Eisenberg, Multiscale modeling shows that dielectric differences make nav channels faster than kv channels, *Journal of General Physiology* 153 (2).
- [27] T.-L. Horng, R. S. Eisenberg, C. Liu, F. Bezanilla, Gating current models computed with consistent interactions, *Biophysical Journal* 110 (3) (2016) 102a–103a.
- [28] T.-L. Horng, R. S. Eisenberg, C. Liu, F. Bezanilla, Continuum gating current models computed with consistent interactions, *Biophysical journal* 116 (2) (2019) 270–282.
- [29] I. Llano, R. J. Bookman, Ionic conductances of squid giant fiber lobe neurons., *The Journal of general physiology* 88 (4) (1986) 543–569.
- [30] I. Llano, C. K. Webb, F. Bezanilla, Potassium conductance of the squid giant axon. single-channel studies., *The Journal of general physiology* 92 (2) (1988) 179–196.
- [31] I. Kim, A. Warshel, Coarse-grained simulations of the gating current in the voltage-activated kv1. 2 channel, *Proceedings of the National Academy of Sciences* 111 (6) (2014) 2128–2133.
- [32] F. Bezanilla, Voltage sensor movements, *The Journal of general physiology* 120 (4) (2002) 465–473.
- [33] A. Hodgkin, A. Huxley, B. Katz, Ionic currents underlying activity in the giant axon of the squid, *Arch. Sci. physiol.* 3 (1949) 129–150.
- [34] B. Sakmann, E. Neher, *Single Channel Recording.*, 2nd Edition, Plenum, New York, 1995.
- [35] J. Zheng, M. C. Trudeau, *Handbook of ion channels*, CRC Press, 2015.

- [36] O. P. Hamill, A. Marty, E. Neher, B. Sakmann, F. J. Sigworth, Improved patch-clamp techniques for high-resolution current recording from cells and cell-free membrane patches, *Pflügers Archiv* 391 (2) (1981) 85–100.
- [37] D. Werry, J. Eldstrom, Z. Wang, D. Fedida, Single-channel basis for the slow activation of the repolarizing cardiac potassium current, *iks*, *Proceedings of the National Academy of Sciences* 110 (11) (2013) E996–E1005.
- [38] K. S. Cole, J. W. Moore, Potassium ion current in the squid giant axon: dynamic characteristic, *Biophysical Journal* 1 (1) (1960) 1–14.
- [39] J. W. Moore, K. S. Cole, Resting and action potentials of the squid giant axon in vivo, *The journal of general physiology* 43 (5) (1960) 961–970.
- [40] R. E. Taylor, J. W. Moore, K. S. Cole, Analysis of certain errors in squid axon voltage clamp measurements, *Biophysical journal* 1 (2) (1960) 161–202.
- [41] M. F. Priest, E. E. Lee, F. Bezanilla, Tracking the movement of discrete gating charges in a voltage-gated potassium channel, *Elife* 10. doi:10.7554/eLife.58148.
URL <https://www.ncbi.nlm.nih.gov/pubmed/34779404>
- [42] P. S. Langan, V. G. Vandavasi, W. Kopec, B. Sullivan, P. V. Afonne, K. L. Weiss, B. L. de Groot, L. Coates, The structure of a potassium-selective ion channel reveals a hydrophobic gate regulating ion permeation, *IUCrJ* 7 (5) (2020) 835–843.
- [43] N. Schoppa, F. Sigworth, Activation of shaker potassium channels: I. characterization of voltage-dependent transitions, *The Journal of general physiology* 111 (2) (1998) 271–294.
- [44] F. Bezanilla, E. Perozo, E. Stefani, Gating of shaker k⁺ channels: II. the components of gating currents and a model of channel activation, *Biophysical journal* 66 (4) (1994) 1011–1021.
- [45] J. Tytgat, P. Hess, Evidence for cooperative interactions in potassium channel gating, *Nature* 359 (6394) (1992) 420–423.

- [46] L. Delemotte, M. Tarek, M. L. Klein, C. Amaral, W. Treptow, Intermediate states of the kv1. 2 voltage sensor from atomistic molecular dynamics simulations, *Proceedings of the National Academy of Sciences* 108 (15) (2011) 6109–6114.
- [47] L. Delemotte, M. A. Kasimova, D. Sigg, M. L. Klein, V. Carnevale, M. Tarek, Exploring the complex dynamics of an ion channel voltage sensor domain via computation, *BioRxiv* (2017) 108217.
- [48] A. Peyser, W. Nonner, Voltage sensing in ion channels: Mesoscale simulations of biological devices, *Physical Review E* 86 (1) (2012) 011910.
- [49] A. Dryga, S. Chakrabarty, S. Vicatos, A. Warshel, Coarse grained model for exploring voltage dependent ion channels, *Biochimica et Biophysica Acta (BBA)-Biomembranes* 1818 (2) (2012) 303–317.
- [50] Z. Song, X. Cao, T.-L. Horng, H. Huang, Electric discharge of electrocytes: Modelling, analysis and simulation, *Journal of Theoretical Biology* 498 (2020) 110294.
- [51] Z. Song, X. Cao, T.-L. Horng, H. Huang, Selectivity of the kcsa potassium channel: Analysis and computation, *Physical Review E* 100 (2) (2019) 022406.
- [52] X. Cao, Z. Song, T.-L. Horng, H. Huang, Electric potential generation of electrocytes: Modelling, analysis, and computation, *Journal of Theoretical Biology* 487 (2020) 110107.
- [53] Z. Song, X. Cao, H. Huang, Electroneutral models for a multidimensional dynamic poisson-nernst-planck system, *Physical Review E* 98 (3) (2018) 032404.
- [54] B. Eisenberg, W. Liu, Poisson–nernst–planck systems for ion channels with permanent charges, *SIAM Journal on Mathematical Analysis* 38 (6) (2007) 1932–1966.
- [55] L. Zhang, W. Liu, Effects of large permanent charges on ionic flows via poisson–nernst–planck models, *SIAM Journal on Applied Dynamical Systems* 19 (3) (2020) 1993–2029.

- [56] D. Colquhoun, A. Hawkes, On the stochastic properties of single ion channels, *Proceedings of the Royal Society of London. Series B. Biological Sciences* 211 (1183) (1981) 205–235.
- [57] D. Colquhoun, A. G. Hawkes, The principles of the stochastic interpretation of ion-channel mechanisms, in: *Single-channel recording*, Springer, 1995, pp. 397–482.
- [58] B. Eisenberg, X. Oriols, D. Ferry, Dynamics of current, charge and mass, *Computational and Mathematical Biophysics* 5 (1) (2017) 78–115.
- [59] B. Eisenberg, N. Gold, Z. Song, H. Huang, What current flows through a resistor?, *arXiv preprint arXiv:1805.04814*.
- [60] H. Miedema, M. Vrouenraets, J. Wierenga, W. Meijberg, G. Robillard, B. Eisenberg, A biological porin engineered into a molecular, nanofluidic diode, *Nano letters* 7 (9) (2007) 2886–2891.

Appendix A. Parameter values

We adopt the following values for the physical parameters [29, 30]

$$\begin{aligned}
k_B &= 1.38 \times 10^{-23} \text{J/K}, & e_0 &= 1.602 \times 10^{-19} \text{C}, & \epsilon_0 &= 8.854 \times 10^{-12} \text{C}/(\text{V} \cdot \text{m}), \\
T &= 292.15 \text{K}, & k_B T / e_0 &\approx 25.17 \text{mV}, & \epsilon_{r0} &= 2, & \epsilon_{r1} &= 40, \\
L &= 0.75 \text{nm}, & s &= 0.15 \text{nm}, & A &= (0.7 \text{nm})^2, & c_0 &= 560 \text{ mM} \approx 3.37 \times 10^{26} / \text{m}^3, \\
c_1^L &= 10 \text{mM}, & c_2^L &= 550 \text{mM}, & c_3^L &= 560 \text{mM}, \\
c_1^R &= 400 \text{mM}, & c_2^R &= 160 \text{mM}, & c_3^R &= 560 \text{mM}, \\
D_0 = D_1 &= 10^{-10} \text{m}^2/\text{s}, & D_2 = D_3 &= 10^{-12} \text{m}^2/\text{s}, & D_b &= 10^{-19} \text{m}^2/\text{s}, \\
AJ_0 &= AD_0 c_0 / L \approx 2.2 \times 10^7 / \text{s}, & e_0 AJ_0 &\approx 3.53 \text{ pA}, \\
t_0 &= \frac{L^2}{D_0} = 5.625 \times 10^{-9} \text{s}, & V_0 &= -80 \text{mV}, & V_1 &= 160 \text{mV}.
\end{aligned}
\tag{A.1}$$

The dimensionless quantities are

$$\begin{aligned}
\epsilon &= \frac{\epsilon_0 k_B T}{e_0^2 c_0 L^2} \approx 7.3 \times 10^{-3}, & \beta &= L A c_0 \approx 0.12, \\
c_1^L &\approx 0.018, & c_2^L &\approx 0.982, & c_3^L &= 1, \\
c_1^R &\approx 0.71, & c_2^R &\approx 0.29, & c_3^R &= 1, \\
D_1 &= 1, & D_2 &= D_3 = 0.01, & D_b &= 10^{-9}, \\
V_0 &= -3.18, & V_1 &= 6.36.
\end{aligned} \tag{A.2}$$

Appendix B. Continuity of the total current

Appendix B.1. The continuous system

The total current consists of three different types of current in different regions

- (i) the current from the change of electric field (for the whole interval/channel)
- (ii) the current from the ionic fluxes (outside of the bubble)
- (iii) the current from the motion of the bubble charge (in the bubble)

We will illustrate the continuity of the total current by the dimensional system in Section 2.1. For the region outside of the bubble ($-L < x < s_b, s < x < L$), we define the total current (per unit cross-sectional area) as I_{total}^{pnp}

$$I_{total}^{pnp}(x, t) = \epsilon_0 \epsilon_r \partial_t E + \sum_{i=1}^3 e_0 z_i J_i = -\epsilon_0 \epsilon_r \partial_{tx} \phi + e_0 (J_1 + J_2 - J_3). \tag{B.1}$$

Taking the time derivative of (1)₁ and using (1)₂, we get

$$\partial_x I_{total}^{pnp} = 0, \tag{B.2}$$

which implies the continuity of current outside of the bubble.

In the bubble, we define the total current (per unit cross-sectional area) as

$$I_{total}^{bubble}(x, t) = \epsilon_0 \epsilon_r \partial_t E + \partial_t Q_b = -\epsilon_0 \epsilon_r \partial_{tx} \phi + \partial_t Q_b, \tag{B.3}$$

where Q_b is the total bubble charge (per unit area) stored in the interval $[s_b, x]$ (it is the magnitude of total negative charge)

$$Q_b = \int_{s_b}^x \frac{q_b}{V_b} dx = \frac{q_b(x - s_b)}{A(s - s_b)}. \tag{B.4}$$

If Q_b increases, that means some positive current of the bubble charge goes across the interface at x . Another interpretation is based on the velocity of the cross sectional surface at x

$$v(x) = \frac{(s-x) ds_b}{(s-s_b) dt}, \quad (\text{B.5})$$

and one can easily verify that

$$\partial_t Q_b = J_b = -\frac{q_b}{V_b} v(x). \quad (\text{B.6})$$

Taking the time derivative of (3), we get the continuity of the total current in the bubble

$$\partial_x I_{total}^{bubble} = 0. \quad (\text{B.7})$$

Appendix B.2. The discrete numerical scheme

The quantities q_k^{n+1} and $\epsilon_{r,k+1/2}$ are defined as

$$q_k^{n+1} = \int_{x_{k-1/2}}^{x_{k+1/2}} \frac{1}{\beta} \frac{q_b}{(s-s_b)} dx, \quad (\text{B.8})$$

and

$$\epsilon_{r,k+1/2} = \frac{h}{\frac{h_1}{40} + \frac{h_2}{2}}, \quad h_1 = s_b - x_k, \quad h_2 = x_{k+1} - s_b, \quad \text{if } s_b \in [x_k, x_{k+1}]. \quad (\text{B.9})$$

Next we show the continuity of the total current in the discrete scheme. The equation of ϕ can be written as

$$\begin{aligned} J_{\phi,k+1/2}^{n+1} - J_{\phi,k-1/2}^{n+1} &= hc_{1,k}^{n+1} + hc_{2,k}^{n+1} - hc_{3,k}^{n+1} - hq_k^{n+1}, \\ J_{\phi,k+1/2}^{n+1} &= -\epsilon \epsilon_{r,k+1/2} \frac{\phi_{k+1}^{n+1} - \phi_k^{n+1}}{h}. \end{aligned} \quad (\text{B.10})$$

Summing over $k = 1, \dots, N$ gives

$$J_{\phi,N+1/2}^{n+1} - J_{\phi,1/2}^{n+1} = h \sum_{k=1}^N c_{1,k}^{n+1} + \sum_{k=1}^N hc_{2,k}^{n+1} - \sum_{k=1}^N hc_{3,k}^{n+1} - \sum_{k=1}^N hq_k^{n+1}. \quad (\text{B.11})$$

Repeat it for J^n with the time step t_n , take the difference, divide it by Δt , and then we get

$$\begin{aligned}
& \frac{J_{\phi, N+1/2}^{n+1} - J_{\phi, N+1/2}^n}{\Delta t} - \frac{J_{\phi, 1/2}^{n+1} - J_{\phi, 1/2}^n}{\Delta t} \\
&= h \sum_{k=1}^N \frac{c_{1,k}^{n+1} - c_{1,k}^n}{\Delta t} + h \sum_{k=1}^N \frac{c_{2,k}^{n+1} - c_{2,k}^n}{\Delta t} - h \sum_{k=1}^N \frac{c_{3,k}^{n+1} - c_{3,k}^n}{\Delta t} \\
&\quad - \frac{h}{\Delta t} \left(\sum_{k=1}^N q_k^{n+1} - \sum_{k=1}^N q_k^n \right) \tag{B.12} \\
&= - \left(J_{1, N+1/2}^{n+1} - J_{1, 1/2}^{n+1} \right) - \left(J_{2, N+1/2}^{n+1} - J_{2, 1/2}^{n+1} \right) + \left(J_{3, N+1/2}^{n+1} - J_{3, 1/2}^{n+1} \right) \\
&\quad - \frac{h}{\Delta t} (Q_b^{n+1} - Q_b^n).
\end{aligned}$$

Rearranging the terms leads to

$$\begin{aligned}
& \frac{J_{\phi, N+1/2}^{n+1} - J_{\phi, N+1/2}^n}{\Delta t} + \left(J_{1, N+1/2}^{n+1} + J_{2, N+1/2}^{n+1} - J_{3, N+1/2}^{n+1} \right) + \frac{h}{\Delta t} (Q_b^{n+1} - Q_b^n) \\
&= \frac{J_{\phi, 1/2}^{n+1} - J_{\phi, 1/2}^n}{\Delta t} + J_{1, 1/2}^{n+1} + J_{2, 1/2}^{n+1} - J_{3, 1/2}^{n+1}, \tag{B.13}
\end{aligned}$$

where the three terms on the left hand side are the discrete version of the three types of currents defined in (i), (ii), (iii) in the previous subsection. If the sum is over the entire interval (i.e., $N + 1/2$ is the right end), the term $Q_b^{n+1} - Q_b^n$ disappears since the total bubble charge Q_b^n is conserved by definition, and the total current is conserved at the two ends.

Appendix C. Derivation for quasi-static state and steady state

Appendix C.1. The quasi-static state

For the quasi-static state, we ignore the dipole and V_0 (equivalently the ϕ is shifted up by a constant V_0 and continuity condition of ϕ will be used at interface). We first consider the right part $s < x < 1$. We get

$$\begin{aligned}
c_1 &= c_1^R e^{-(\phi - V_1)}, \quad c_2 = c_2^R e^{-(\phi - V_1)}, \quad c_3 = e^{\phi - V_1}, \\
\epsilon \epsilon_{r1} \phi'' &= e^{\phi - V_1} - e^{-(\phi - V_1)}, \tag{C.1}
\end{aligned}$$

where $c_3^R = c_1^R + c_2^R = 1$ have been used. Integrating once gives

$$\frac{1}{2}\epsilon\epsilon_{r1}[(\phi'(x))^2 - (\phi'(s+))^2] = e^{\phi-V_1} + e^{-(\phi-V_1)} - B_2, \quad (\text{C.2})$$

where

$$B_2 = e^{\phi_s-V_1} + e^{-(\phi_s-V_1)}, \quad \phi'(s+) = \frac{\epsilon_{r0}}{\epsilon_{r1}}\phi'(s-) = \frac{\epsilon_{r0}}{\epsilon_{r1}}\tilde{\phi}_s. \quad (\text{C.3})$$

Then, we obtain

$$(\phi'(x))^2 = G_1(\phi; \phi_s, \tilde{\phi}_s) = \left(\frac{\epsilon_{r0}}{\epsilon_{r1}}\tilde{\phi}_s\right)^2 + \frac{2}{\epsilon\epsilon_{r1}}[e^{\phi-V_1} + e^{-(\phi-V_1)} - B_2] \quad (\text{C.4})$$

and

$$x = \int_{\phi_s}^{\phi} \frac{1}{\sqrt{G_1(\phi; \phi_s, \tilde{\phi}_s)}} d\phi + s. \quad (\text{C.5})$$

For the left part $-1 < x < s_b$, we get

$$\begin{aligned} \epsilon\epsilon_{r1}\phi'' &= e^{\phi} - e^{-\phi}, \\ \frac{1}{2}\epsilon\epsilon_{r1}[(\phi'(x))^2 - (\phi'(s_b-))^2] &= e^{\phi} + e^{-\phi} - B_3, \end{aligned} \quad (\text{C.6})$$

with

$$\begin{aligned} B_3 &= e^{\phi_{s_b}} + e^{-\phi_{s_b}}, \quad \phi_{s_b} = B_1(s_b - s)^2 + \tilde{\phi}_s(s_b - s) + \phi_s \\ \phi'(s_b-) &= \frac{\epsilon_{r0}}{\epsilon_{r1}}\phi'(s_b+) = \frac{\epsilon_{r0}}{\epsilon_{r1}}[\tilde{\phi}_s + 2B_1(s_b - s)], \end{aligned} \quad (\text{C.7})$$

where B_1 is given in (35). Then, we get

$$(\phi'(x))^2 = G_2(\phi; \phi_s, \tilde{\phi}_s) = (\phi'(s_b-))^2 + \frac{2}{\epsilon\epsilon_{r1}}[e^{\phi} + e^{-\phi} - B_3] \quad (\text{C.8})$$

and

$$x = - \int_{\phi_{s_b}}^{\phi} \frac{1}{\sqrt{G_2(\phi; \phi_s, \tilde{\phi}_s)}} d\phi + s_b. \quad (\text{C.9})$$

Appendix C.2. The steady state

Now we consider the steady state. Define

$$p = c_1 + c_2, \quad J_p = J_1 + \frac{J_2}{D_2}, \quad (\text{C.10})$$

then the two equations for c_1 and c_2 lead to

$$-J_p = p'(x) + p\phi'(x). \quad (\text{C.11})$$

Let $V = V_0 + V_1$. For the right part $x > s$, we get

$$c_3 = c_3^R e^{\phi-V} = e^{\phi-V}. \quad (\text{C.12})$$

Multiplying ϕ' in the equation of ϕ (i.e., equation (40)₁, and the delta function is put into the jump conditions) gives

$$-\epsilon\epsilon_{r1}\phi''(x)\phi'(x) = p\phi' - c_3\phi' = -J_p - p' - c_3', \quad (\text{C.13})$$

and integrating gives

$$p = \frac{1}{2}\epsilon\epsilon_{r1} [(\phi'(x))^2 - (\phi'(1))^2] - J_p(x-1) - c_3 + 2, \quad (\text{C.14})$$

where the boundary conditions at $x = 1$ have been used. Substituting into (40)₁, we get

$$-\epsilon\epsilon_{r1}\phi''(x) = \frac{1}{2}\epsilon\epsilon_{r1} [(\phi'(x))^2 - (\phi'(1))^2] - J_p(x-1) - 2(e^{\phi-V} - 1), \quad (\text{C.15})$$

for $x > s$. Similarly for the left part $x < s$, we have

$$\begin{aligned} c_3 &= c_3^L e^\phi, \quad c_1 = \frac{1}{2}\epsilon\epsilon_{r1} [(\phi'(x))^2 - (\phi'(-1))^2] - J_p(x+1) - c_3 + 2, \\ -\epsilon\epsilon_{r1}\phi''(x) &= \frac{1}{2}\epsilon\epsilon_{r1} [(\phi'(x))^2 - (\phi'(-1))^2] - J_p(x+1) - 2(e^\phi - 1). \end{aligned} \quad (\text{C.16})$$